

# Reconstructing Neural Sources of Activity from SEEG Recordings

(All models are wrong, but  
some are useful)

The University of Texas  
Health Science Center at Houston

*Prof. John C. Mosher*

*Texas Institute for Restorative Neurotechnologies (TIRN)  
Department of Neurology*

# Outline

**All models are wrong, but some are useful.**

*-George Box*

- Physiological basis of the **Current Column**
- Modeling of the cortical surface
- Invasive Source Modeling

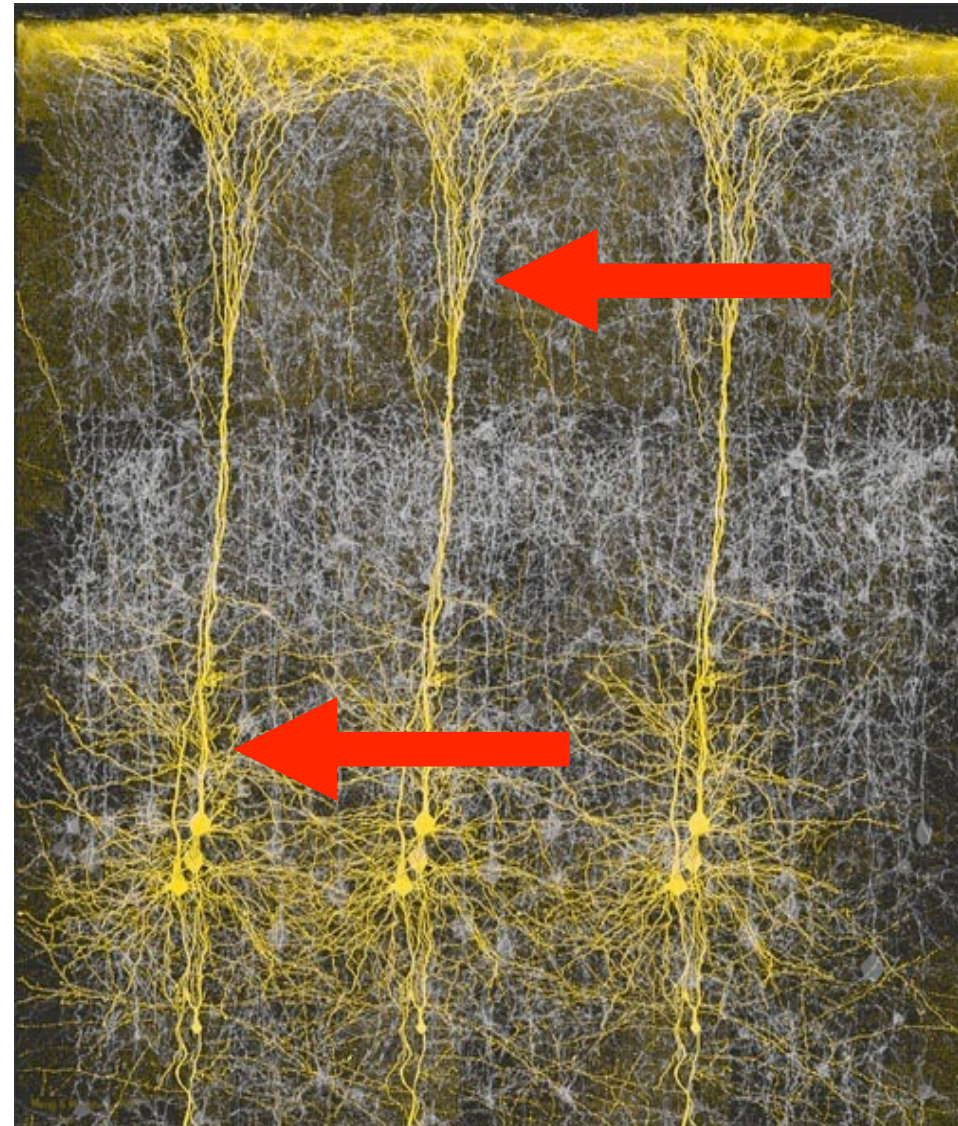
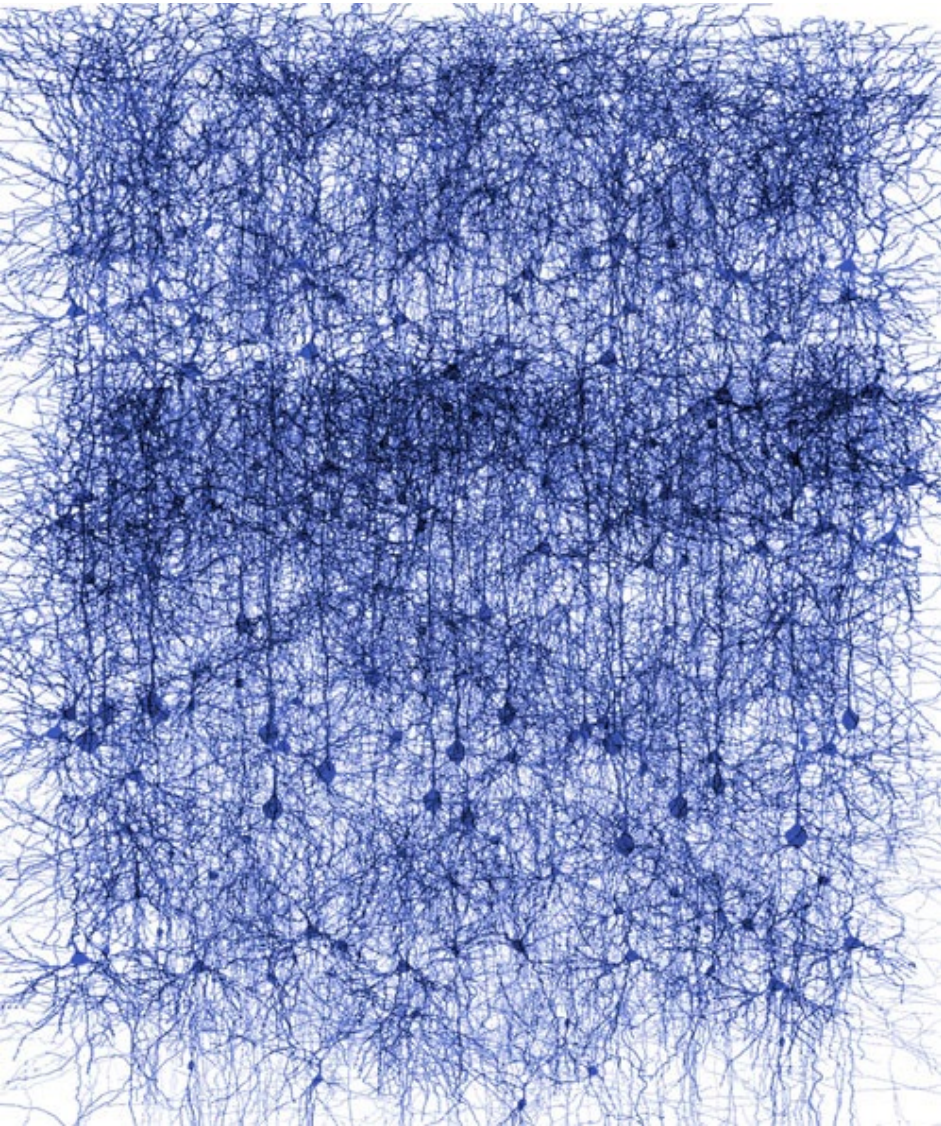
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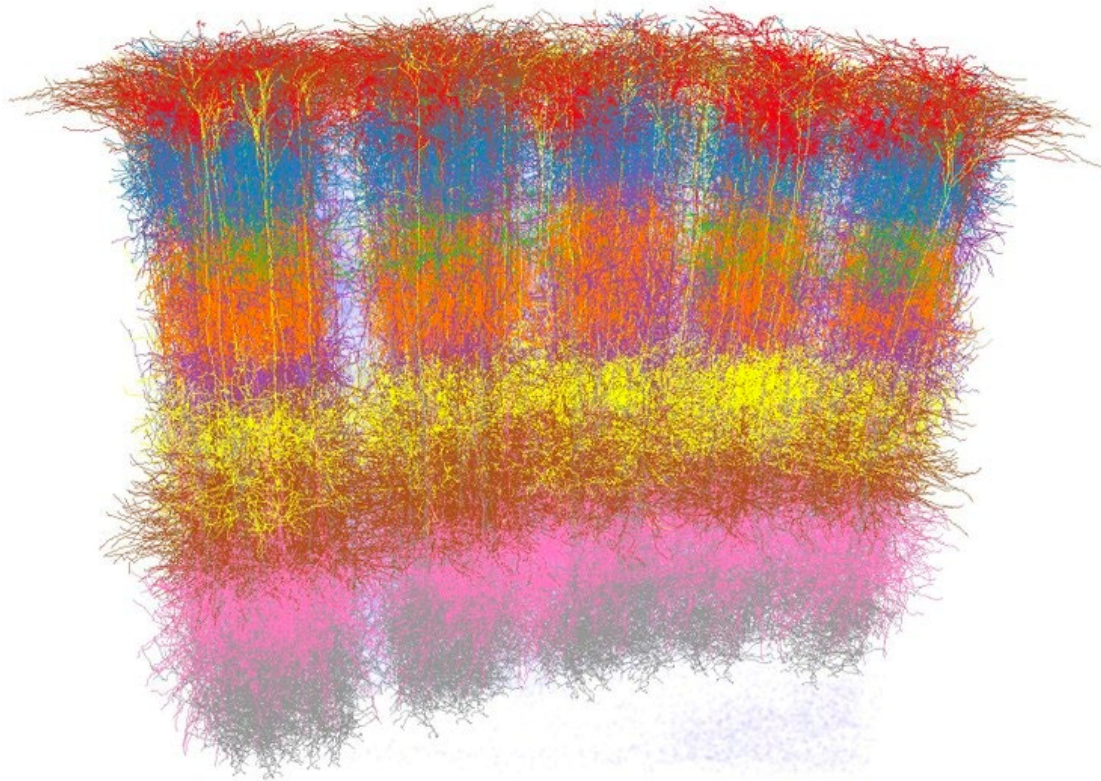
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# A Forest of Neurons in Gray Matter



# “Cortical Columns”



*Cell-type-specific 3D reconstruction of five neighboring barrel columns in rat vibrissal cortex (credit: Marcel Oberlaender et al.)*

- Model the 3D multilayer cortex as columns.
- Emphasize the 2D cortical surface in units of square mm
- This “wrong” model ignores the complexity of the column and the transverse connections.

# Excitatory vs Inhibitory PSP

- Ambiguous whether excitatory in upper layers or inhibitory in lower layers.

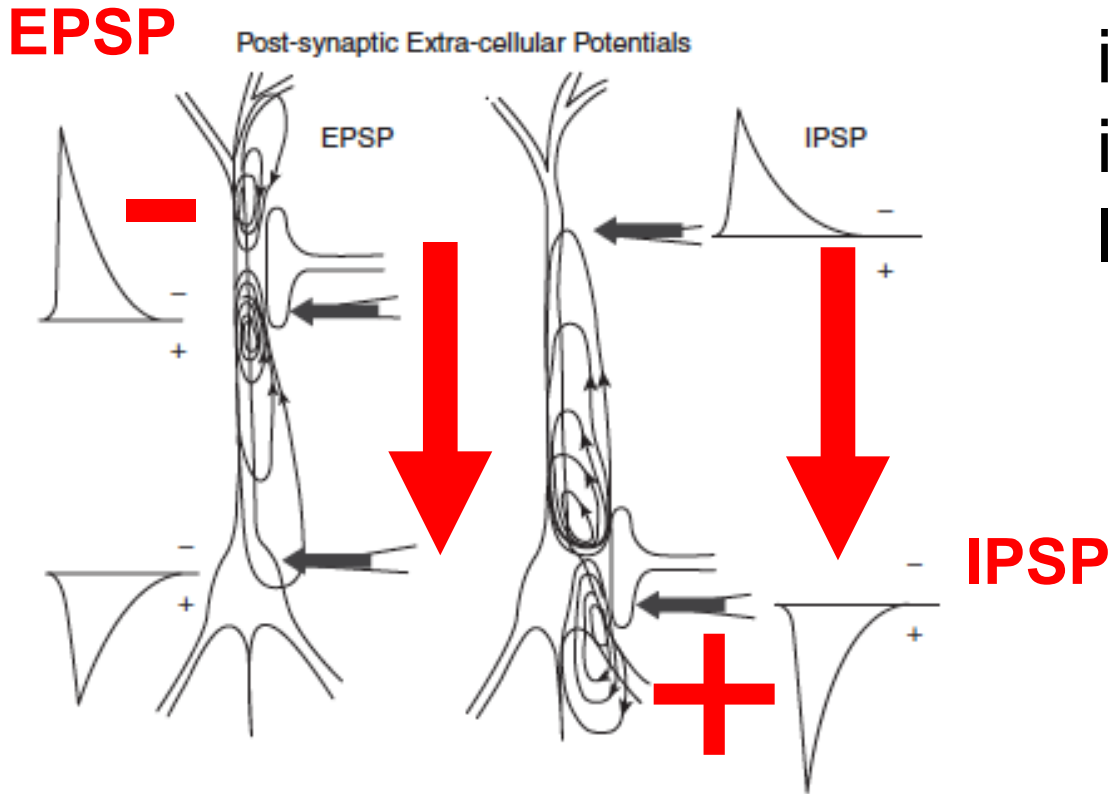
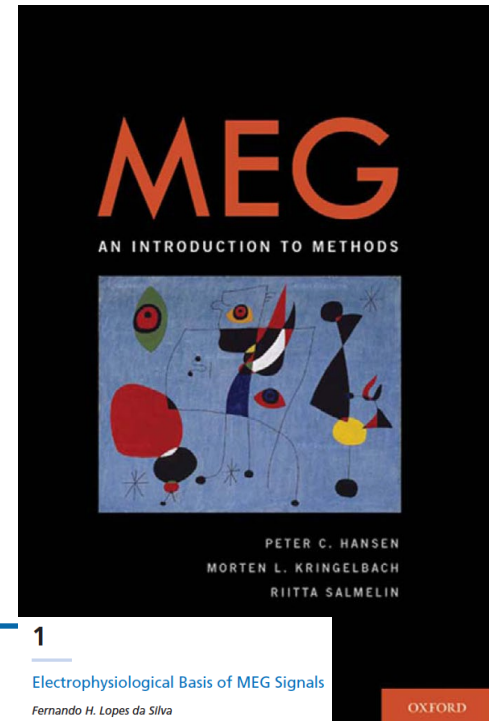
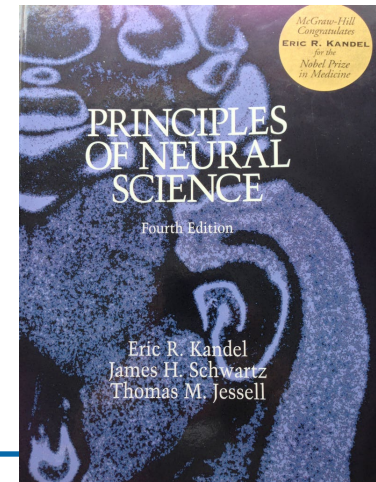
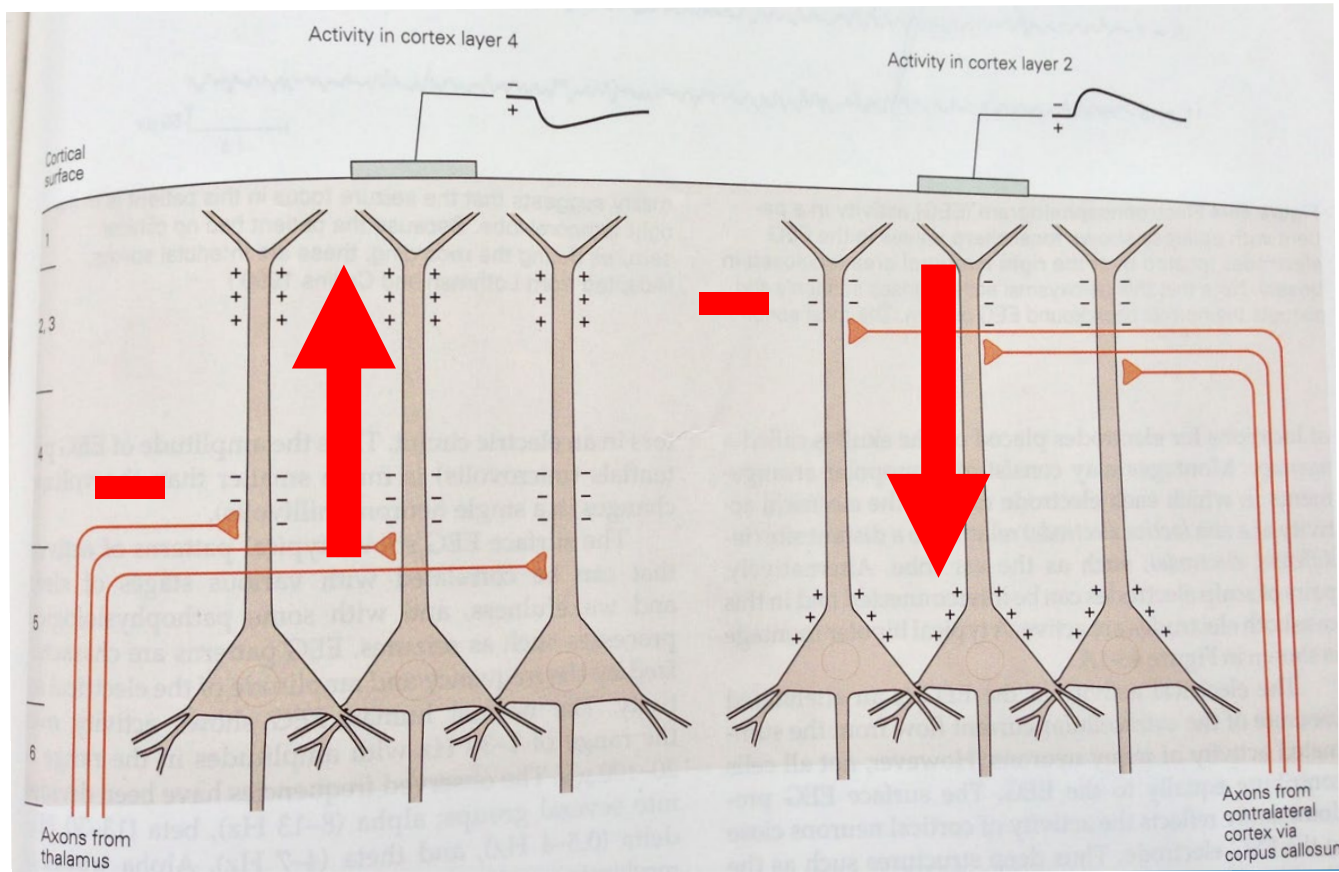


Figure 1-1. Intra- and extracellular current flow in an idealized pyramidal neuron due to different types of synaptic activation. EPSP: excitatory



# EPSP Distal vs Proximal

- Thalamo-cortical into Layer 4 -> **Upwards**
- Contralateral-cortical into Layer 2,3 -> **Downwards**



# Cortex is NOT Columnar EVERYWHERE

(But good enough for now)

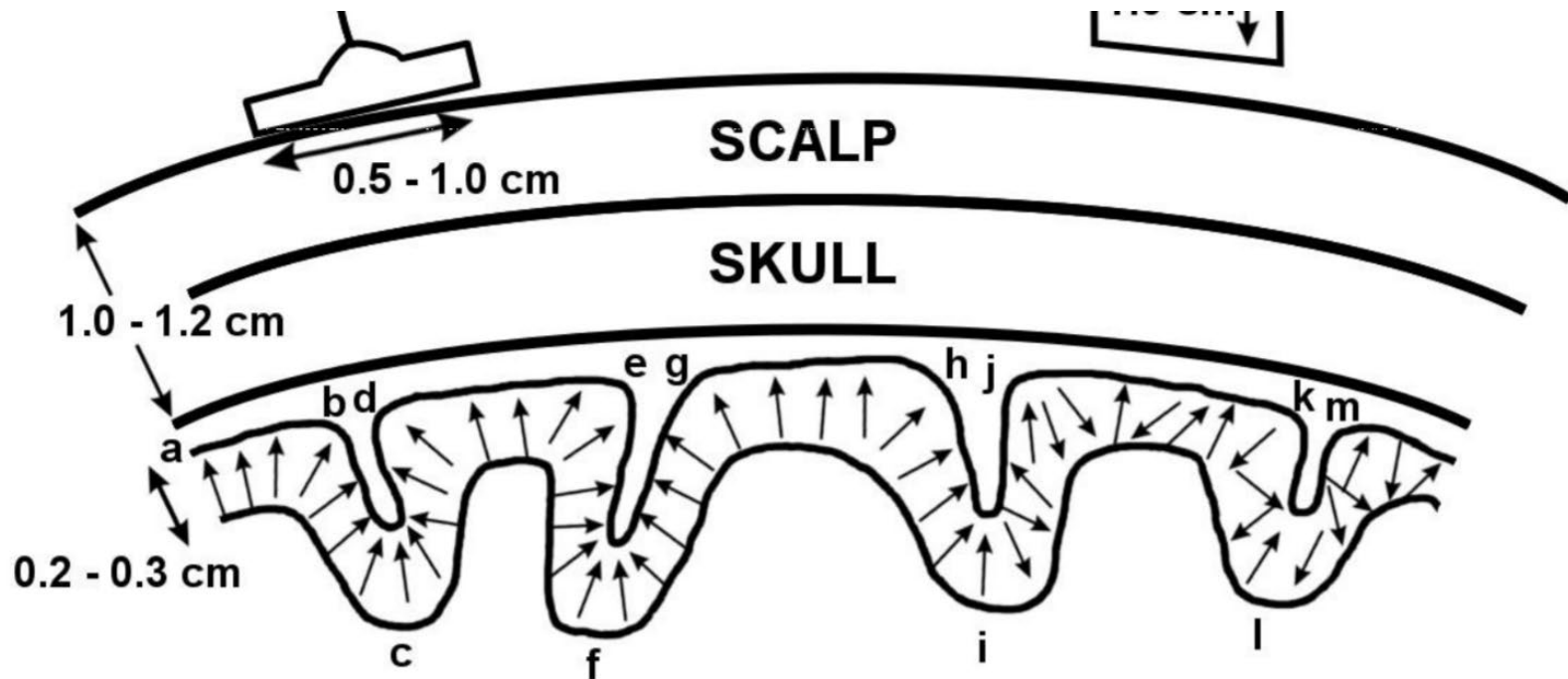


Figure 4. Cortical dipole layers. The arrows represent a snapshot of the macro source function  $\mathbf{P}(\mathbf{r}, t)$ , which is here assumed to be synchronous and directed perpendicular to the local cortical surface over the extended region a-i. In contrast,  $\mathbf{P}(\mathbf{r}, t)$  has random directions in regions i-m.



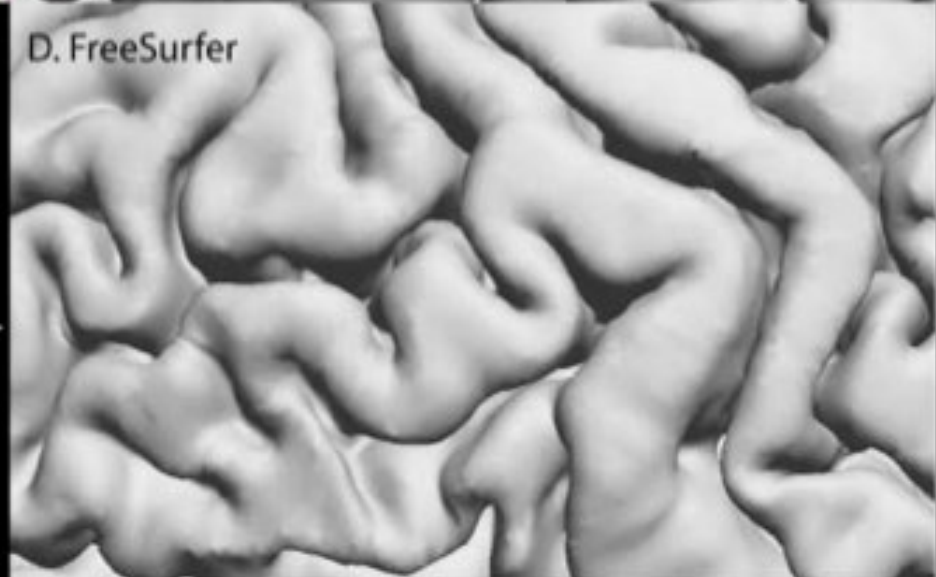
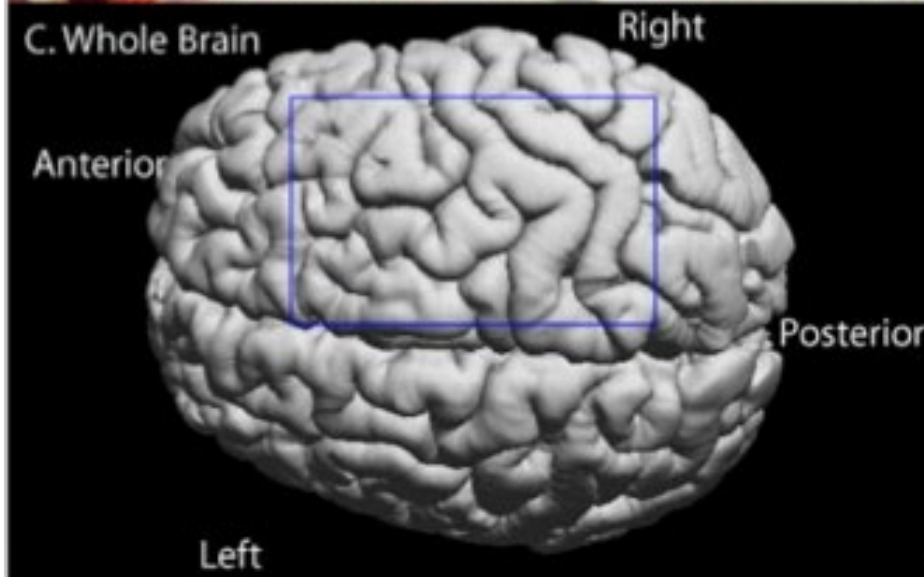
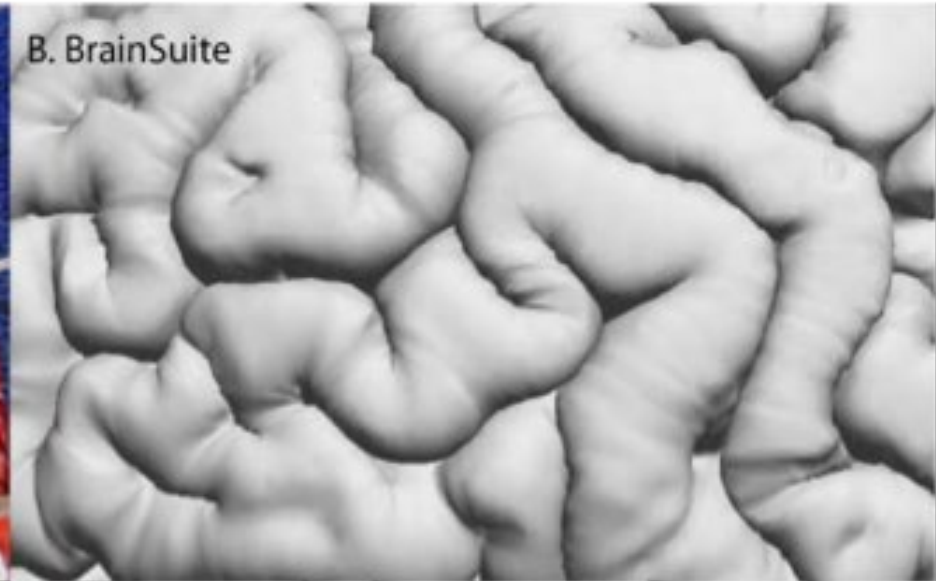
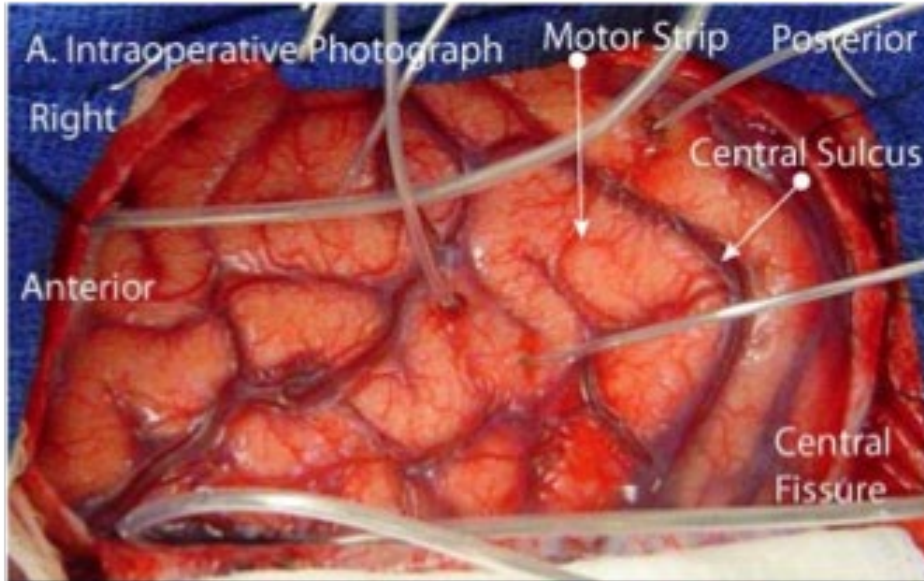
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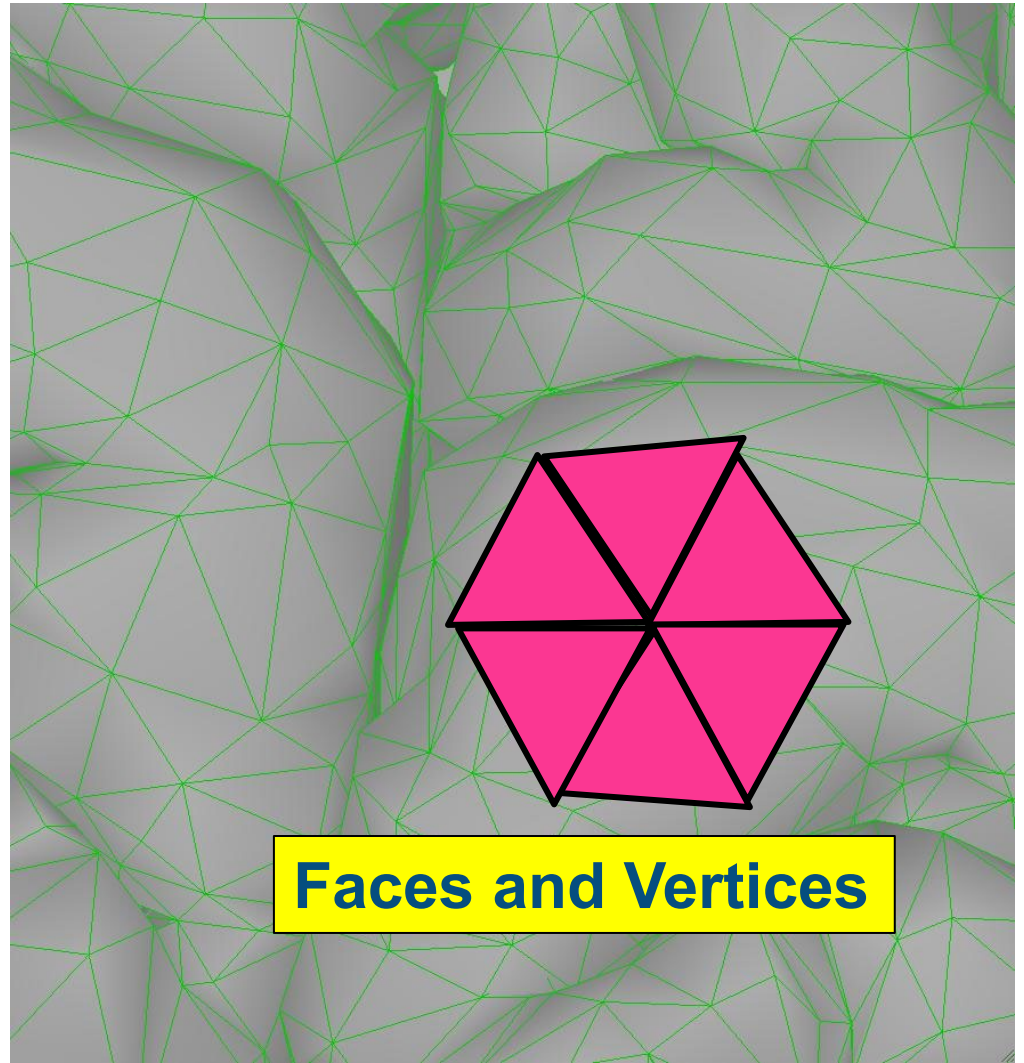
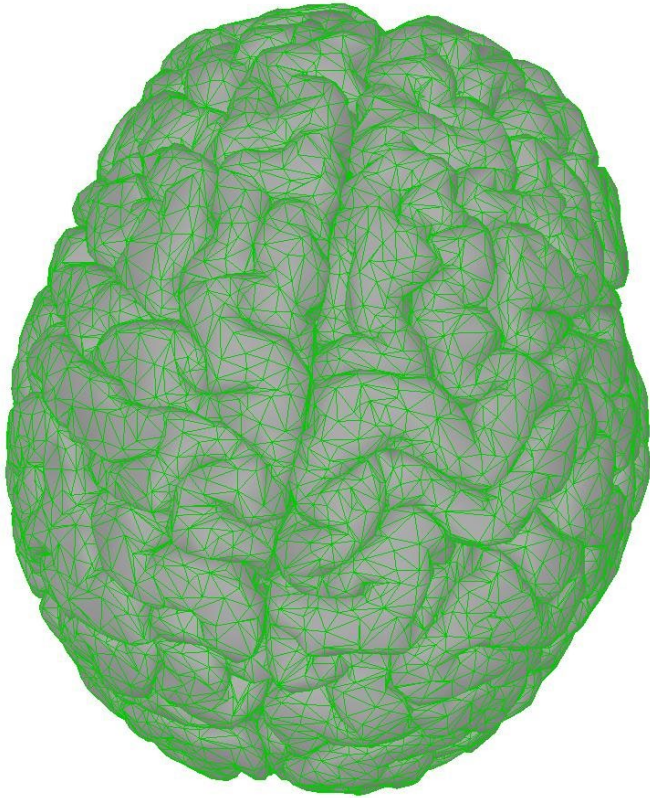
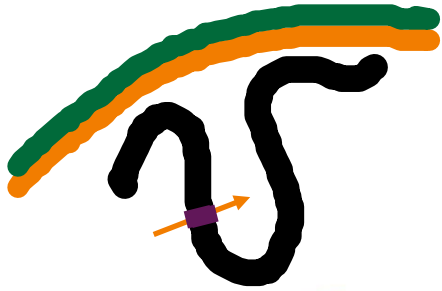
*-George Box*

- Physiological basis of the **Current Column**
- **Modeling of the cortical surface**
- Invasive Source Modeling

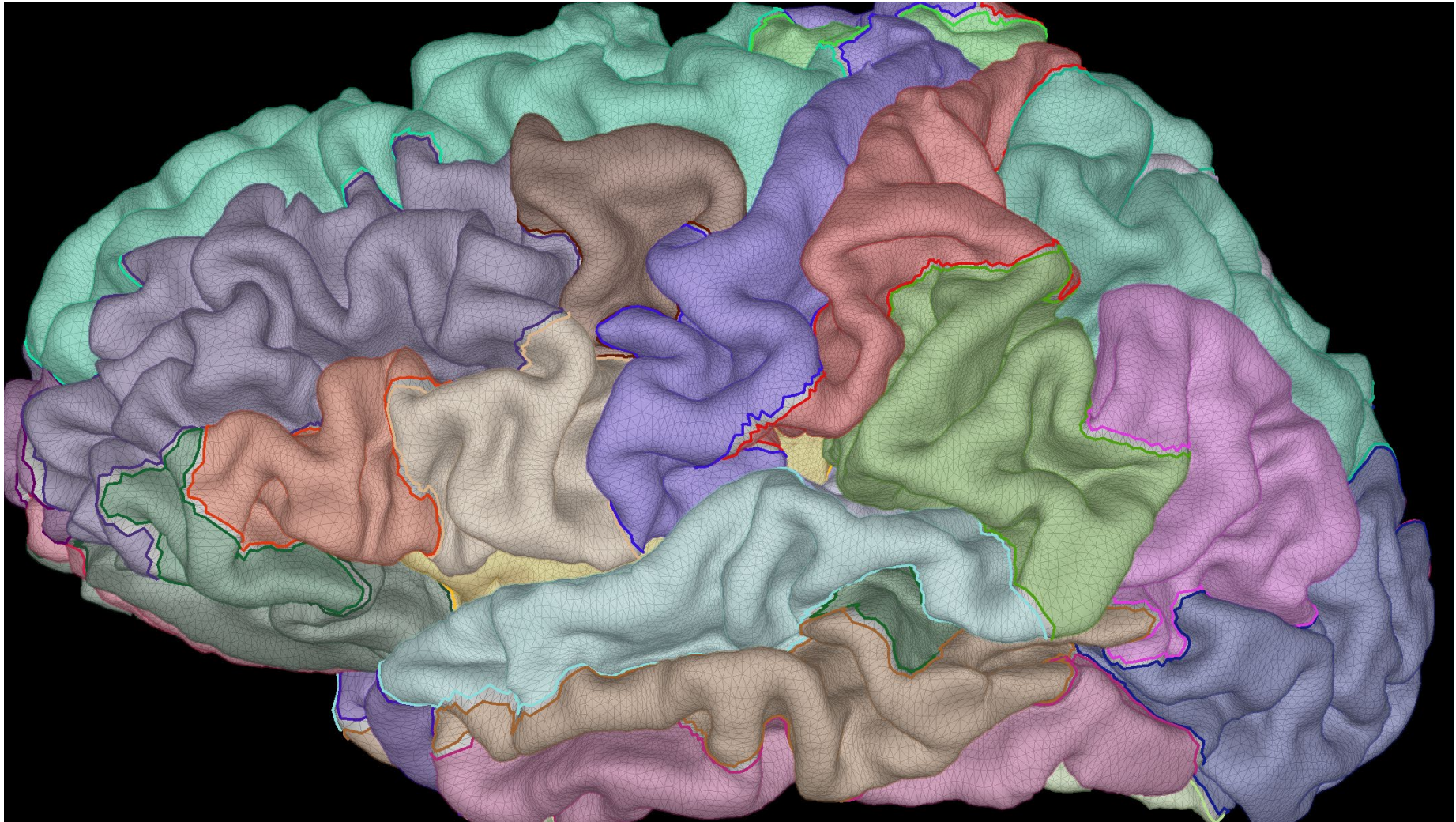
# Cortical Surface



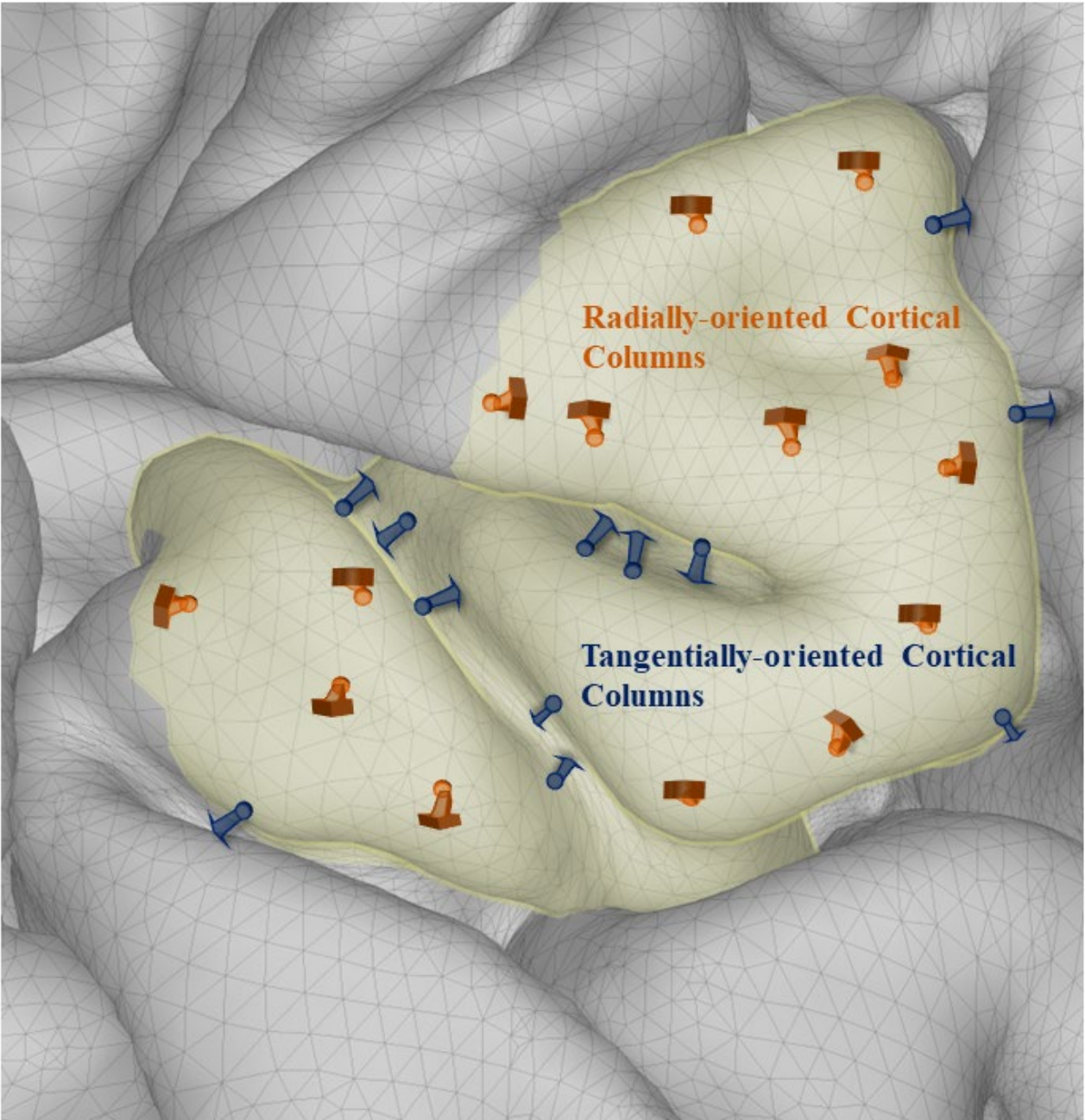
# Cortical Modeling of Sources – Many Thousands of Triangles



Even Denser, Hundreds of Thousands of Triangles  
- 252,224 **labeled** vertices, spanning 192,152 square mm

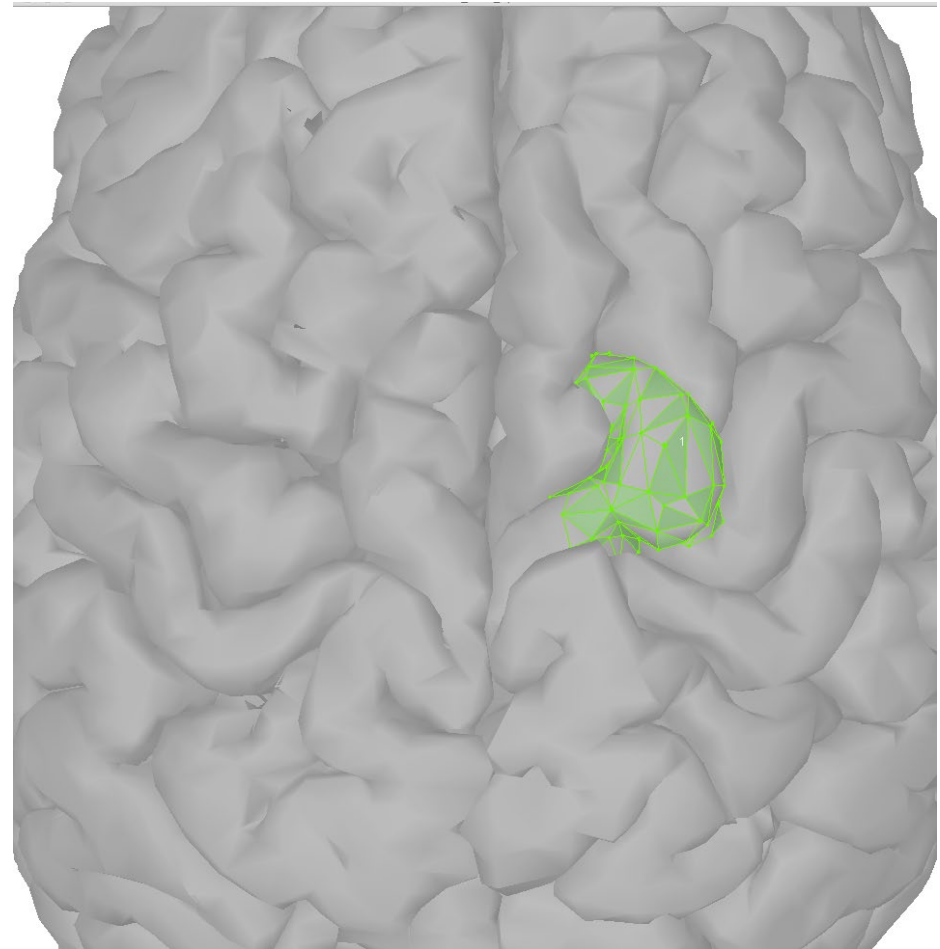


Each vertex models  
an area of about  
**1 square mm**  
of a Cortical Column

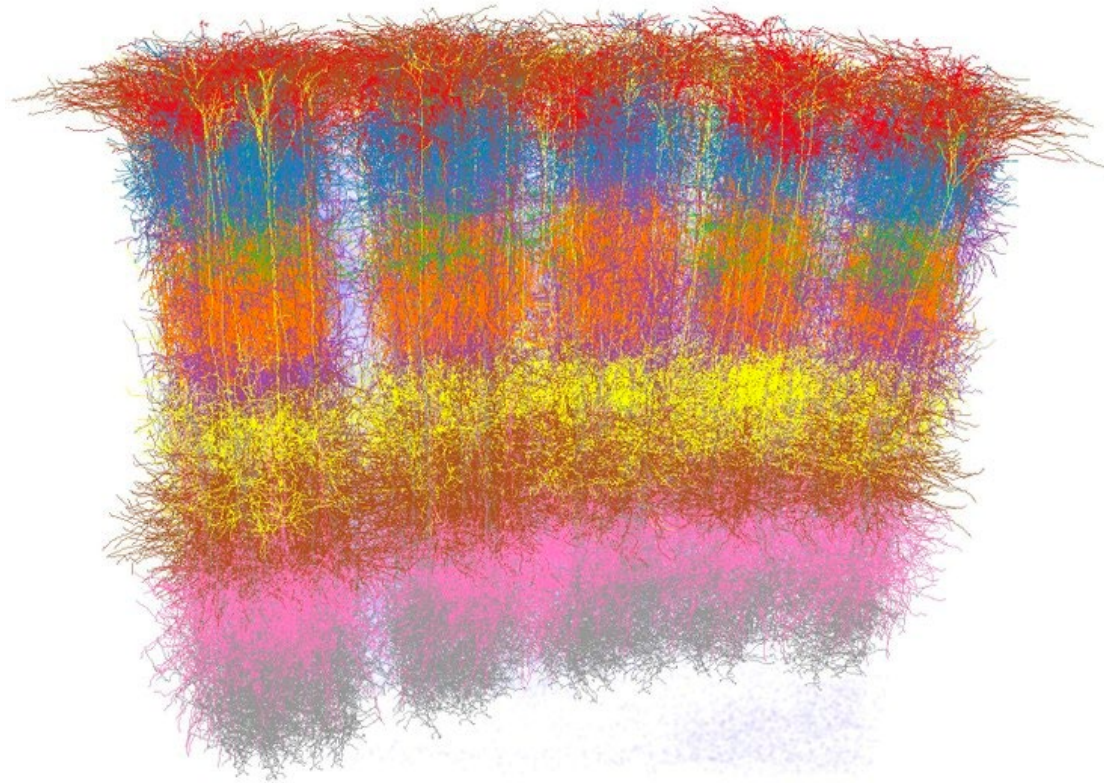


# Patches on the Cortex

- Patch models are a collection of vertices, rather than a single dipole per vertex.
- Incorporates the intuitive and physiologic concept of a “distributed” source.



# “Cortical Columns”

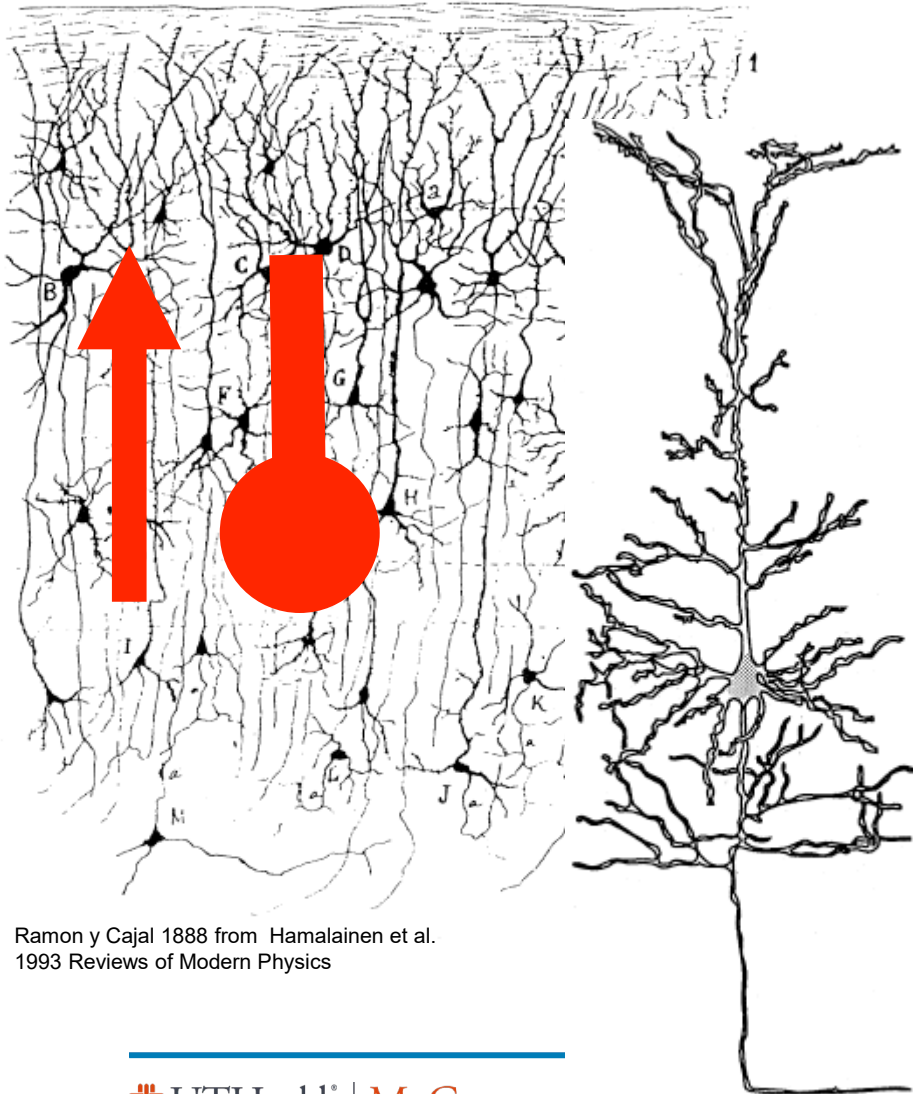


- Back to our “wrong” model: We ask the modeling question:

How much current can one square mm generate?

*Cell-type-specific 3D reconstruction of five neighboring barrel columns in rat vibrissal cortex (credit: Marcel Oberlaender et al.)*

# Current Dipole Moment of Neurons



Ramon y Cajal 1888 from Hamalainen et al.  
1993 Reviews of Modern Physics

- Post-synaptic Potentials along the length of the pyramidal cells, effective conductor length of about **2mm** (very arguable)
- Each pyramidal cell generates about  
**20 fA-m = 20 pA-mm**  
or **10 pA flowing along 2 mm.**
- Therefore, **one million cells** is  
**20 nA-m = 20μA-mm**,  
about that of an evoked response.
- Epilepsy Spike is about  
**200 nA-m = 200μA-mm**
- Compare functional stimulation:  
4mA bipolar into 5mm contact separation  
= 20 mA-mm  
  
-> **20,000 nA-m!**



# “Okada Constant” for Current Density

NeuroImage 111 (2015) 49–58



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NeuroImage

journal homepage: [www.elsevier.com/locate/ynimg](http://www.elsevier.com/locate/ynimg)

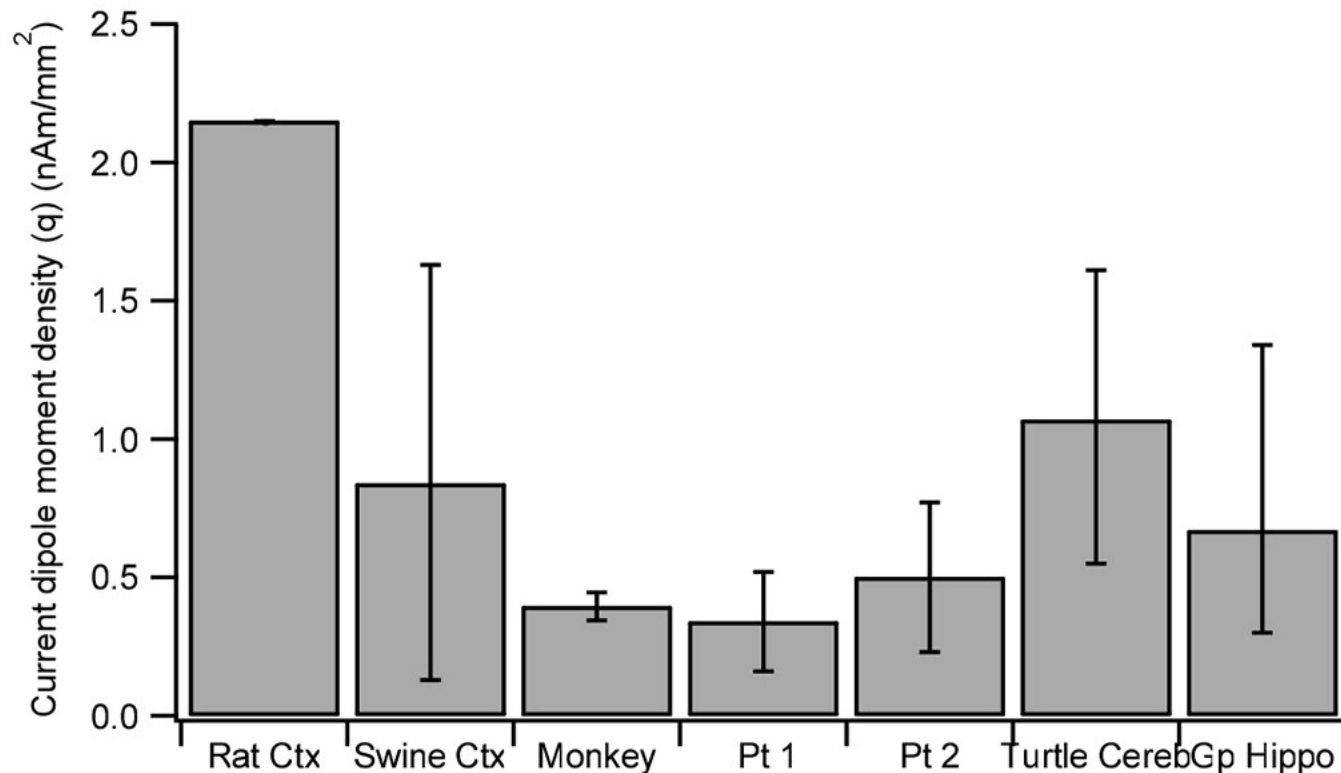
Invariance in current dipole moment density across brain structures and species: Physiological constraint for neuroimaging

Shingo Murakami <sup>a</sup>, Yoshio Okada <sup>b,\*</sup>

2015 Neuroimage, Vol 111, 49-58

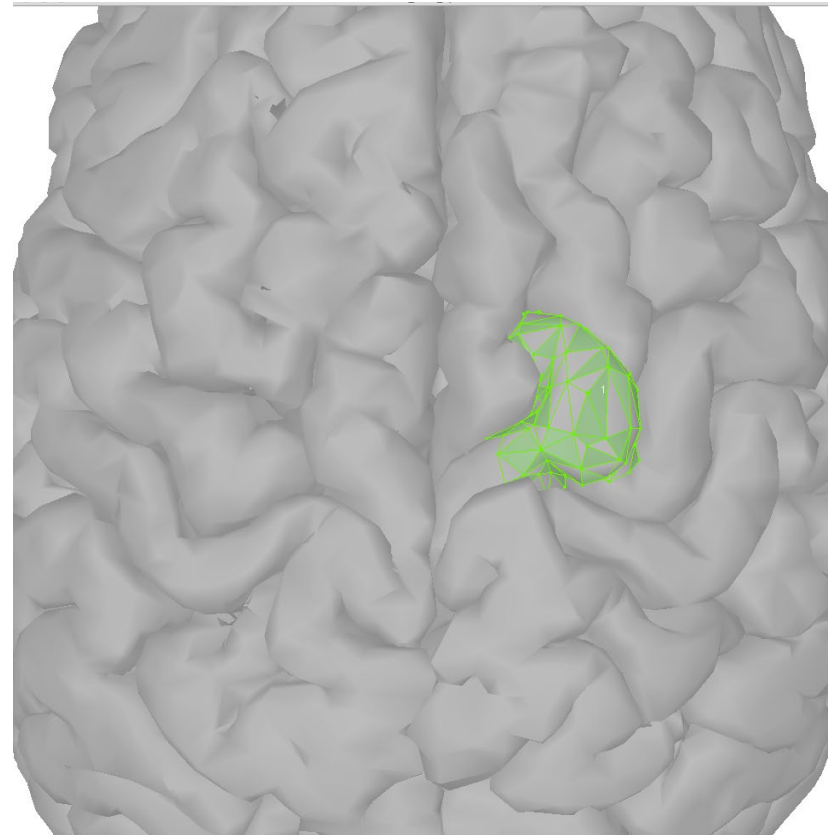
## Invariance Across Species – “About” 1 nA-m / mm<sup>2</sup>

- Units of nA-m per square mm
- Convenient for immediately scaling cortical area



# The Equivalent Current Dipole Models a Patch on the Cortex

- Using “Okada Constant”:
  - 20 nA-m is a **minimum** of 20 mm<sup>2</sup> of activated cortex
  - 200 nA-m is **minimum** of 200 mm<sup>2</sup>
- Simply varying the current density over the range of 0.1 to 1 nA-m/mm<sup>2</sup> easily changes these extents by a **factor of 10**.



# Outline

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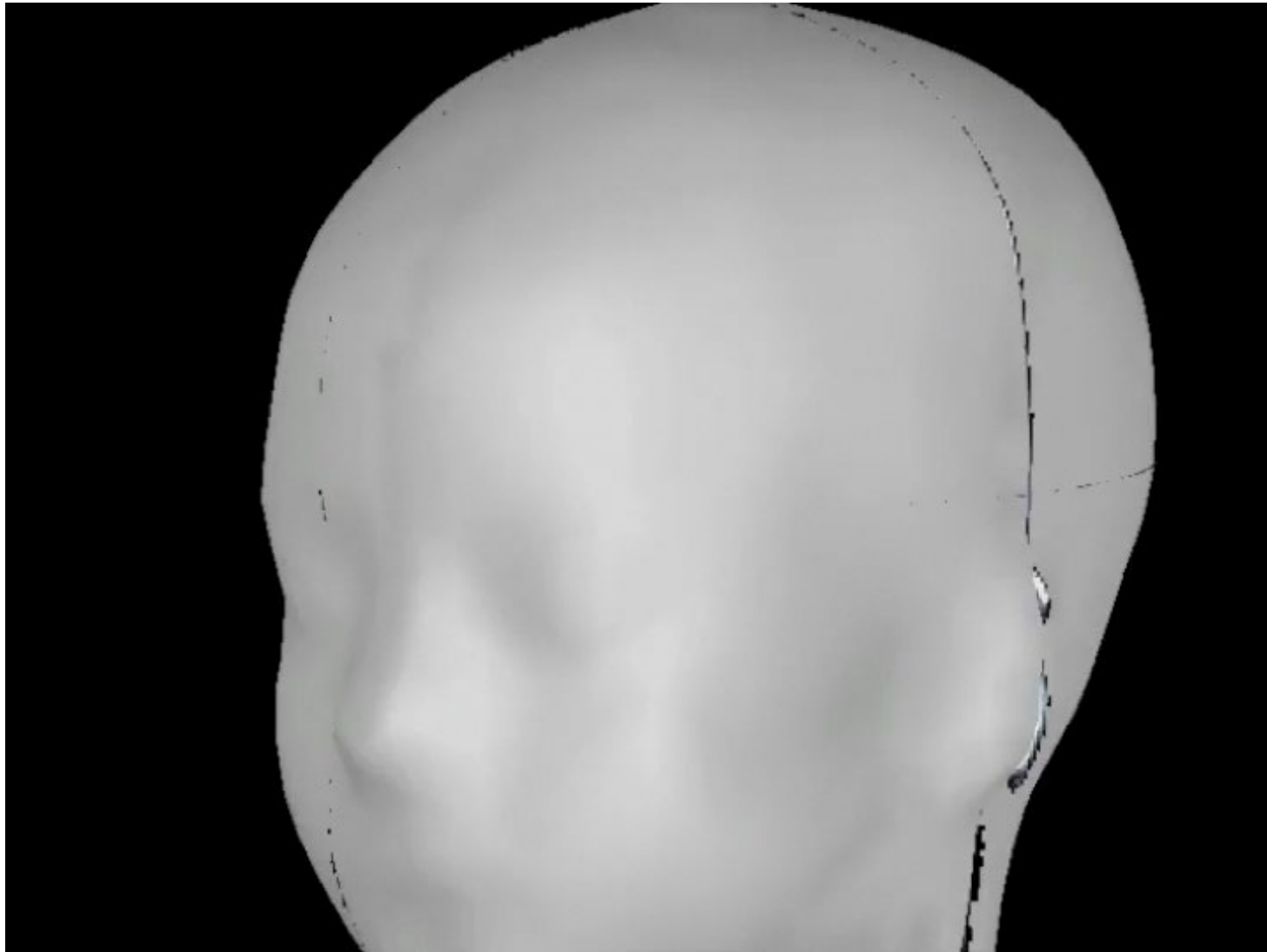
- Physiological basis of the **Current Column**
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# Brainstorm SEEG

- SEEG Contacts are registered to the PT anatomy
- Contacts are visualized life-size
- Brainstorm tutorial on how to do in your facility



# Brainstorm SEEG Processing



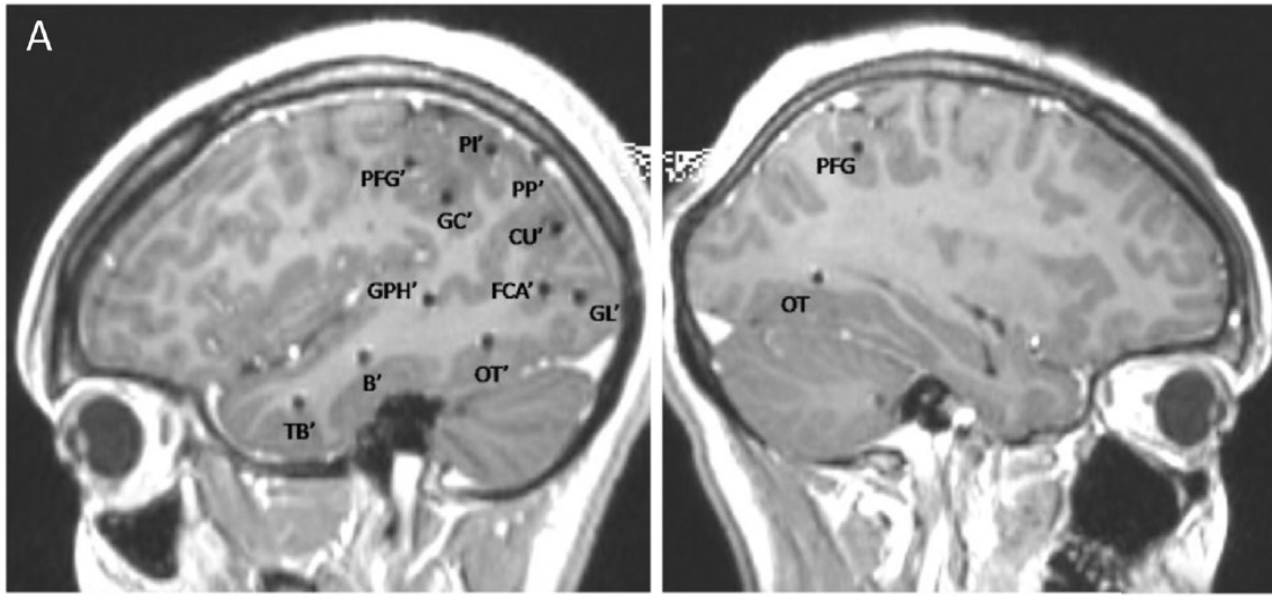


# Good Coverage is Important!

Short communication

Simultaneous SEEG-MEG-EEG recordings Overcome the SEEG limited spatial sampling

Martine Gavaret<sup>a,b</sup>, Anne-Sophie Dubarry<sup>a,c</sup>, Romain Carron<sup>a,d</sup>, Fabrice Bartolomei<sup>a,b</sup>,  
Agnès Trébuchon<sup>a,b,1</sup>, Christian-George Bénar<sup>a,\*,1</sup>



# MEG Localized



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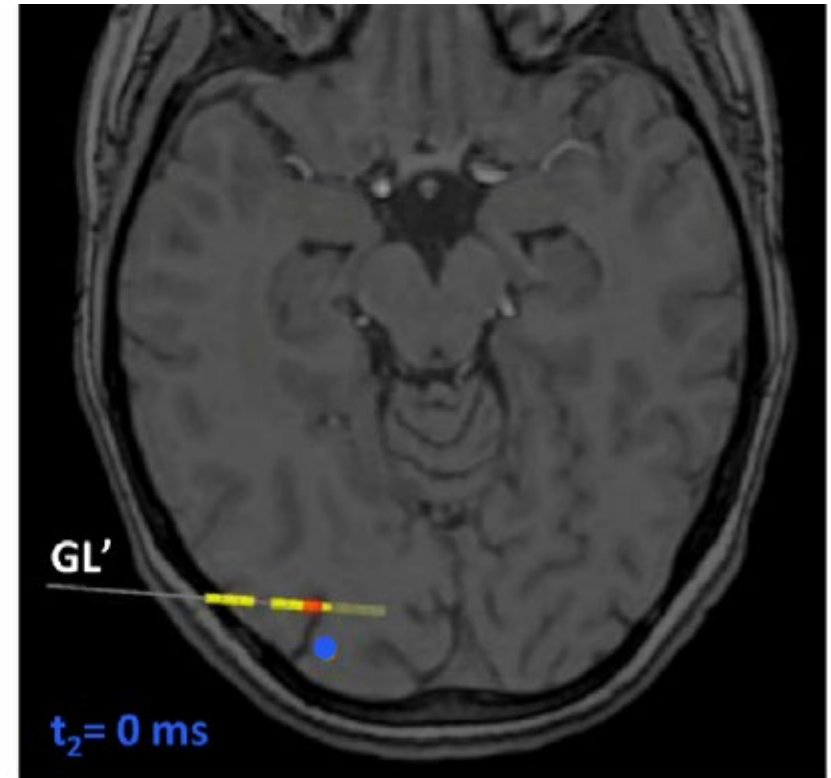
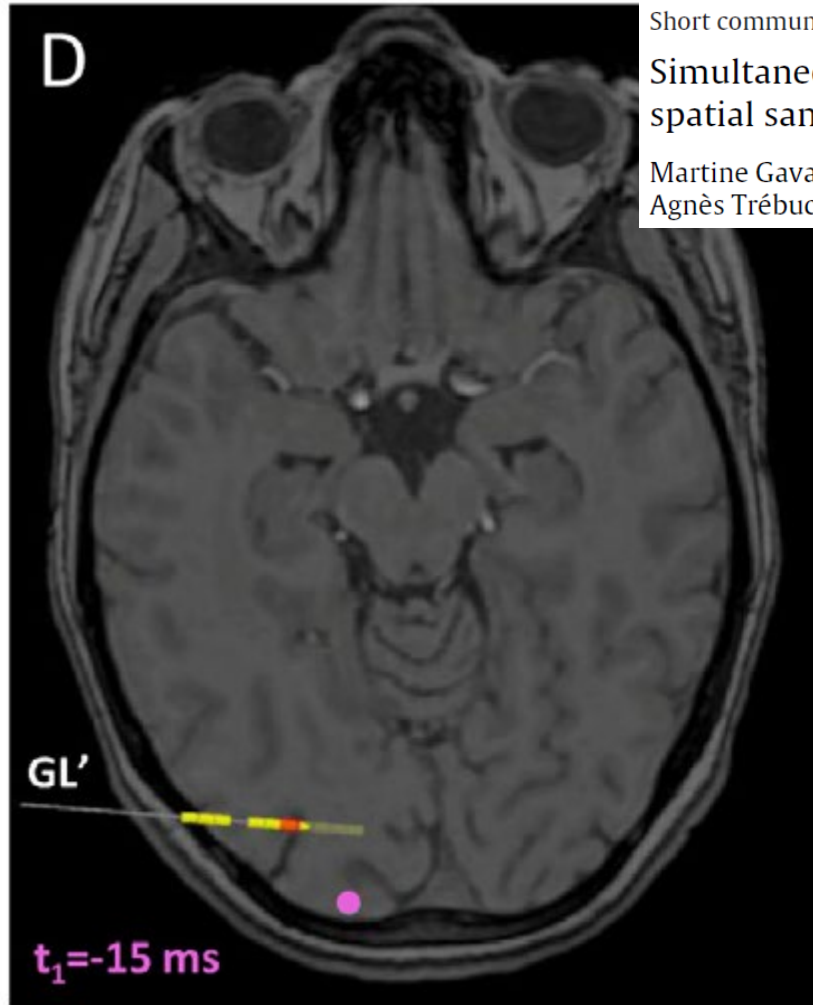
Epilepsy Research

journal homepage: [www.elsevier.com/locate/epilepsyres](http://www.elsevier.com/locate/epilepsyres)

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# Excellent Reference Paper on Good Practices

NeuroImage 260 (2022) 119438



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## Advances in human intracranial electroencephalography research, guidelines and good practices



Manuel R. Mercier<sup>a,\*</sup>, Anne-Sophie Dubarry<sup>b</sup>, François Tadel<sup>c</sup>, Pietro Avanzini<sup>d</sup>, Nikolai Axmacher<sup>e,f</sup>, Dillan Cellier<sup>g</sup>, Maria Del Vecchio<sup>d</sup>, Liberty S. Hamilton<sup>h,i,j</sup>, Dora Hermes<sup>k</sup>, Michael J. Kahana<sup>l</sup>, Robert T. Knight<sup>m</sup>, Anais Llorens<sup>n</sup>, Pierre Megevand<sup>o</sup>, Lucia Melloni<sup>p,q</sup>, Kai J. Miller<sup>r</sup>, Vitória Piai<sup>s,t</sup>, Aina Puce<sup>u</sup>, Nick F Ramsey<sup>v</sup>, Caspar M. Schwiedrzik<sup>w,x</sup>, Sydney E. Smith<sup>y</sup>, Arjen Stolk<sup>s,z</sup>, Nicole C. Swann<sup>aa</sup>, Mariska J Vansteensel<sup>v</sup>, Bradley Voytek<sup>g,y,ab,ac</sup>, Liang Wang<sup>ad,ae</sup>, Jean-Philippe Lachaux<sup>af,1</sup>, Robert Oostenveld<sup>s,ag,1</sup>

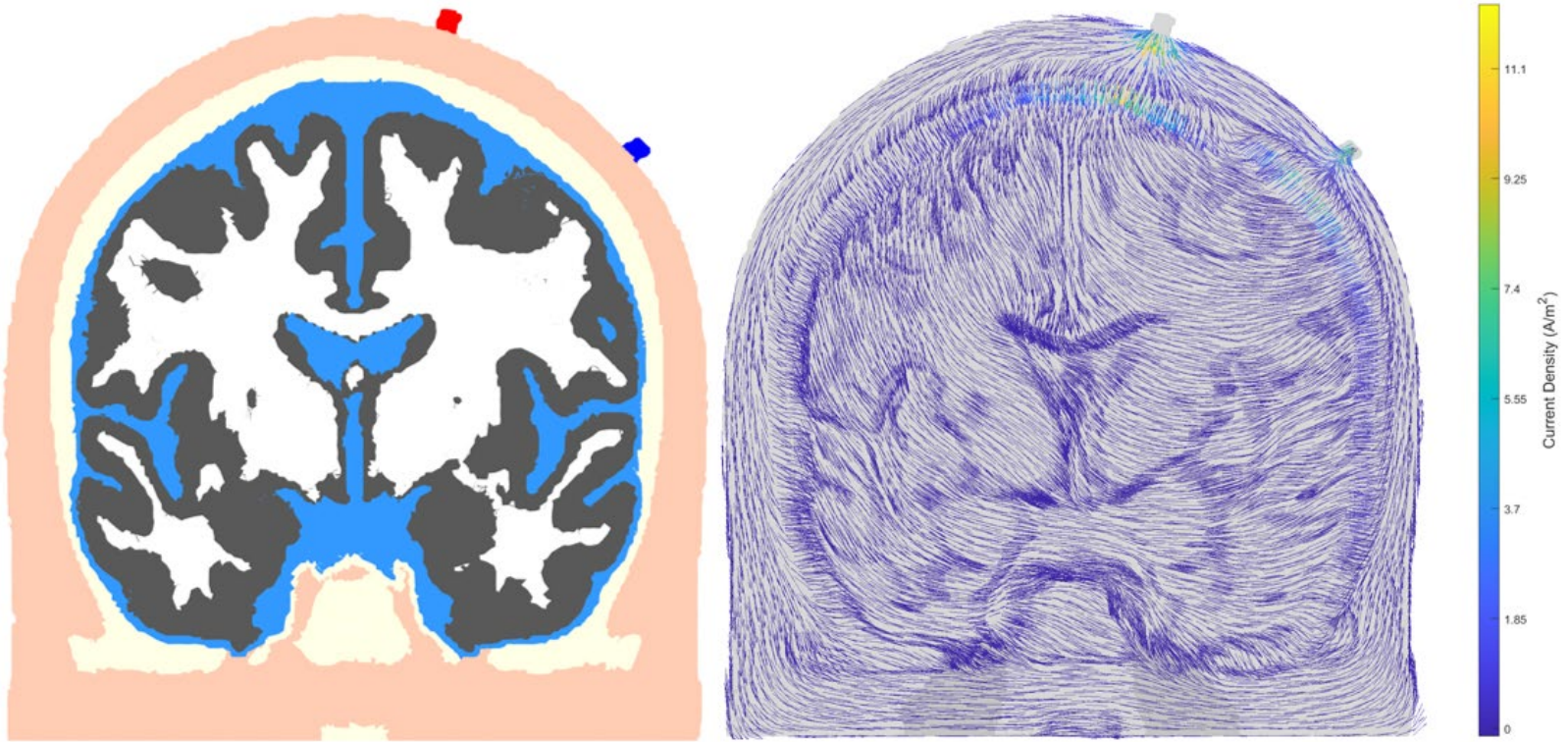
# Example Case Study

- PT has PMG (polymicrogyria) in the right peri-rolandic region
  - suspected seizure onset site
- 17 devices (‘electrodes’) implanted, comprising about 250 electrodes (‘channels,’ ‘contacts’).
- Surface modeling of the “mid” surface between pial and gray/white boundaries.
- (VLC Movie: Viewing the Implantation)

## Leadfield Analyses

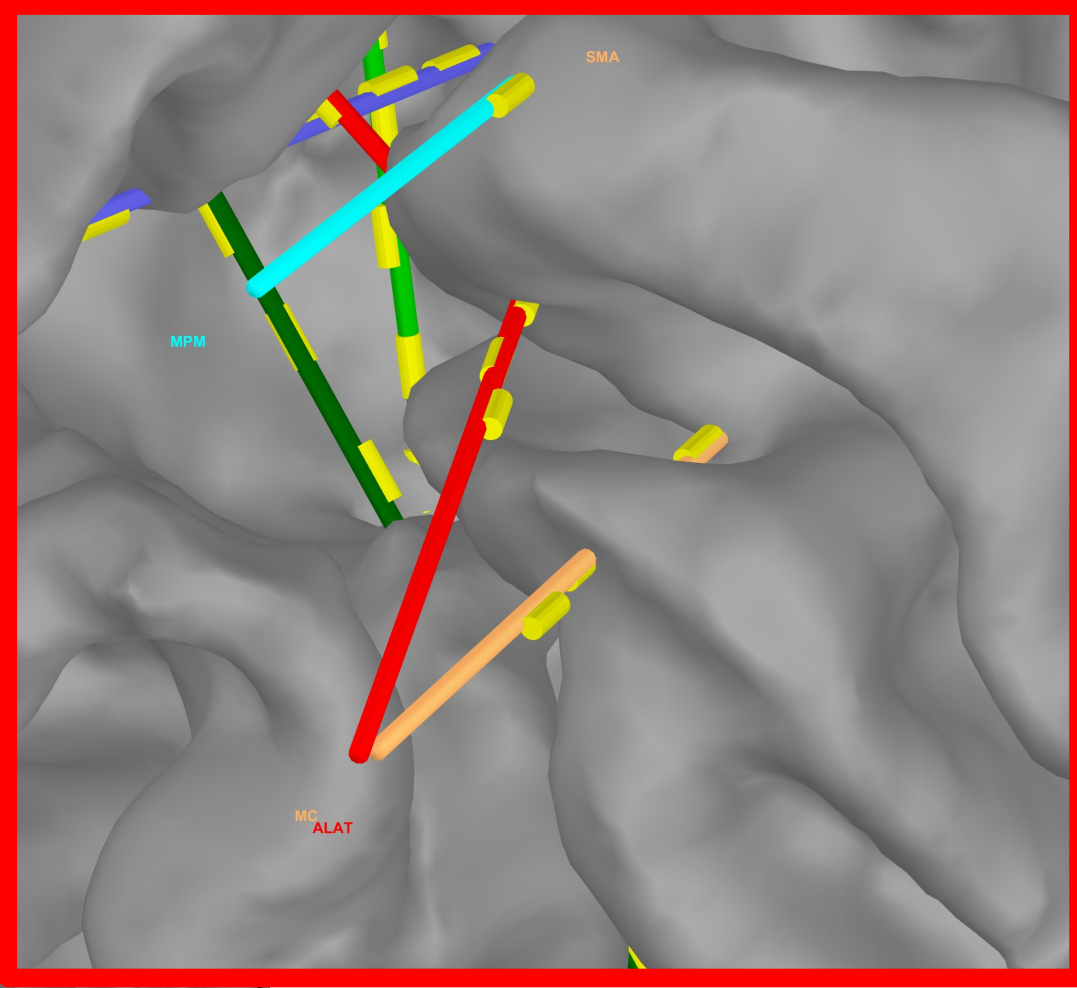
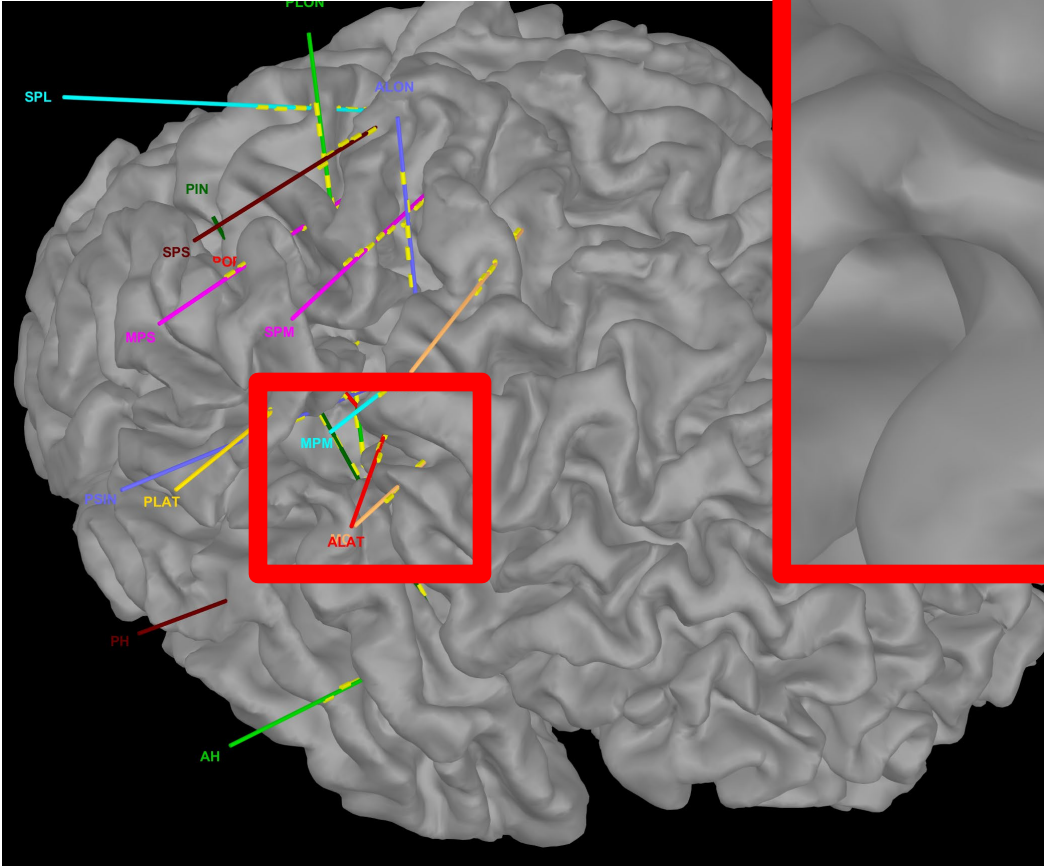
- In this example, the cortical surface comprises ~270,000 vertices, and we have ~250 SEEG contacts.
- For each of the vertices, we calculate the forward model to all contacts.
  - OpenMEEG or DuneNEURO
  - Forward model calculated in x, y, and z directions.
  - Forward matrix is 250 x 3 for each vertex.
- The result is a matrix of size 250 x 810,000.
  - Only a few GB at single precision.
- By reciprocity, each ROW of this matrix represents samples of the leadfields for that contact.

# FEM Lead-Fields in a Five Compartment Model

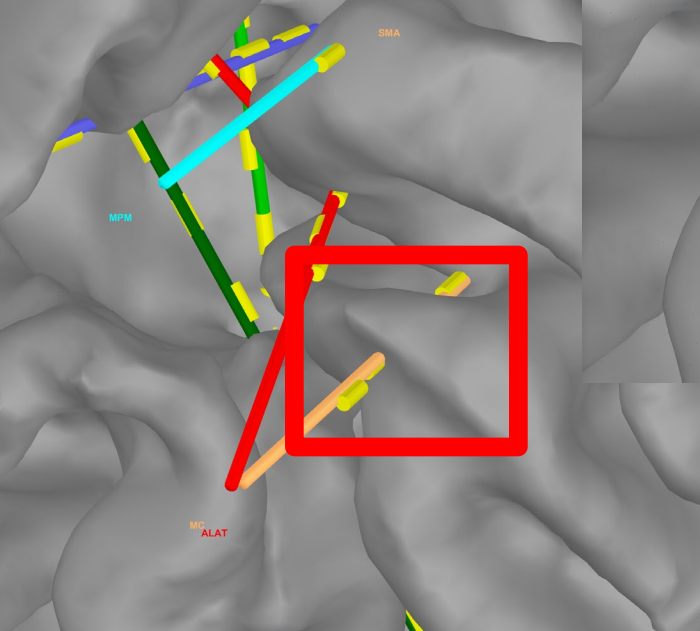
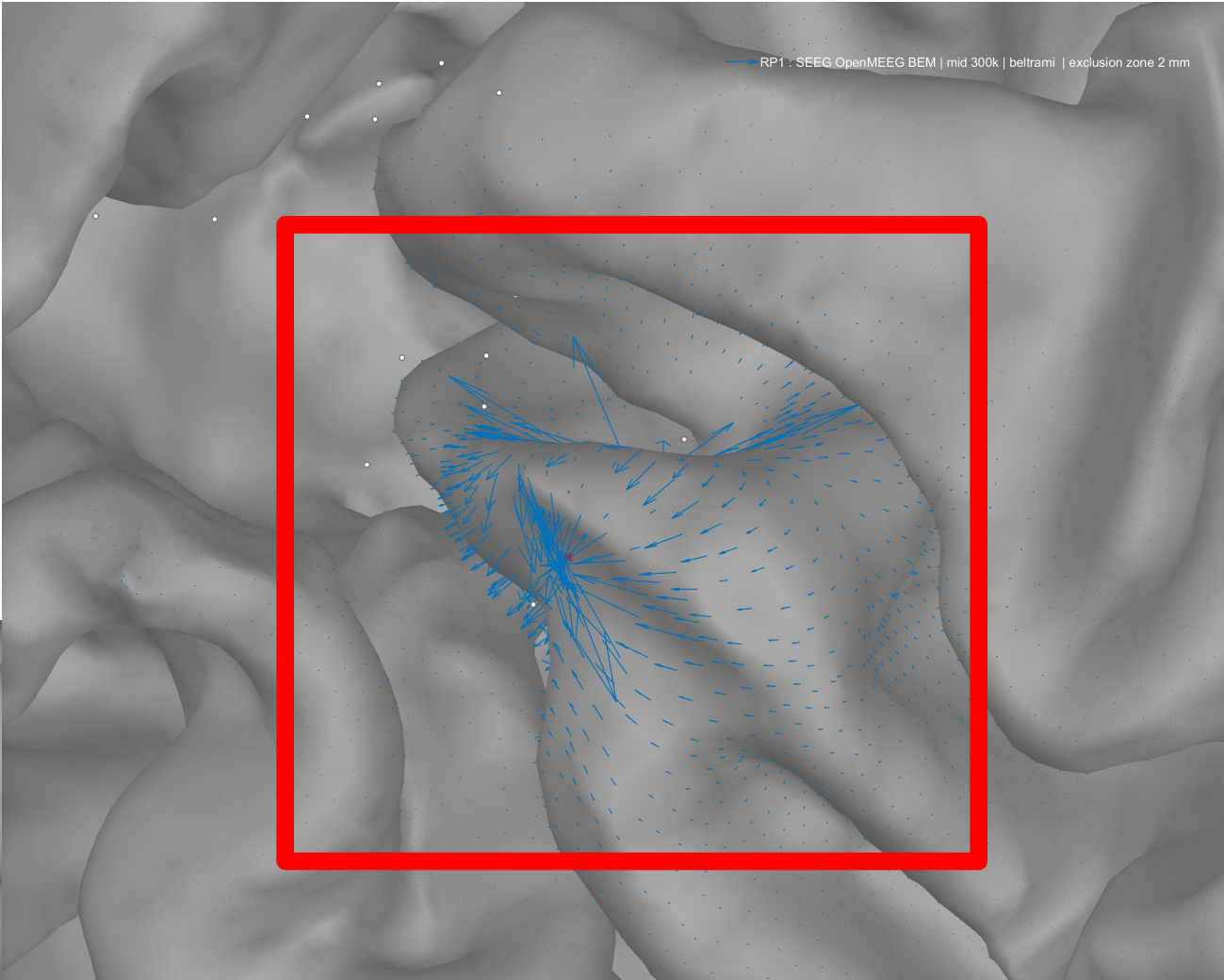


- DUNEuro – Brainstorm implementation.
  - Duneuro is based on the DUNE library (distributed and unified numerics environment)
  - Brainstorm provides a Matlab interface to duneuro
  - Example here is the lead fields through a five isotropic compartment
  - REF: [Duneuro.org](http://Duneuro.org) and [neuroimage.usc.edu/brainstorm](http://neuroimage.usc.edu/brainstorm)

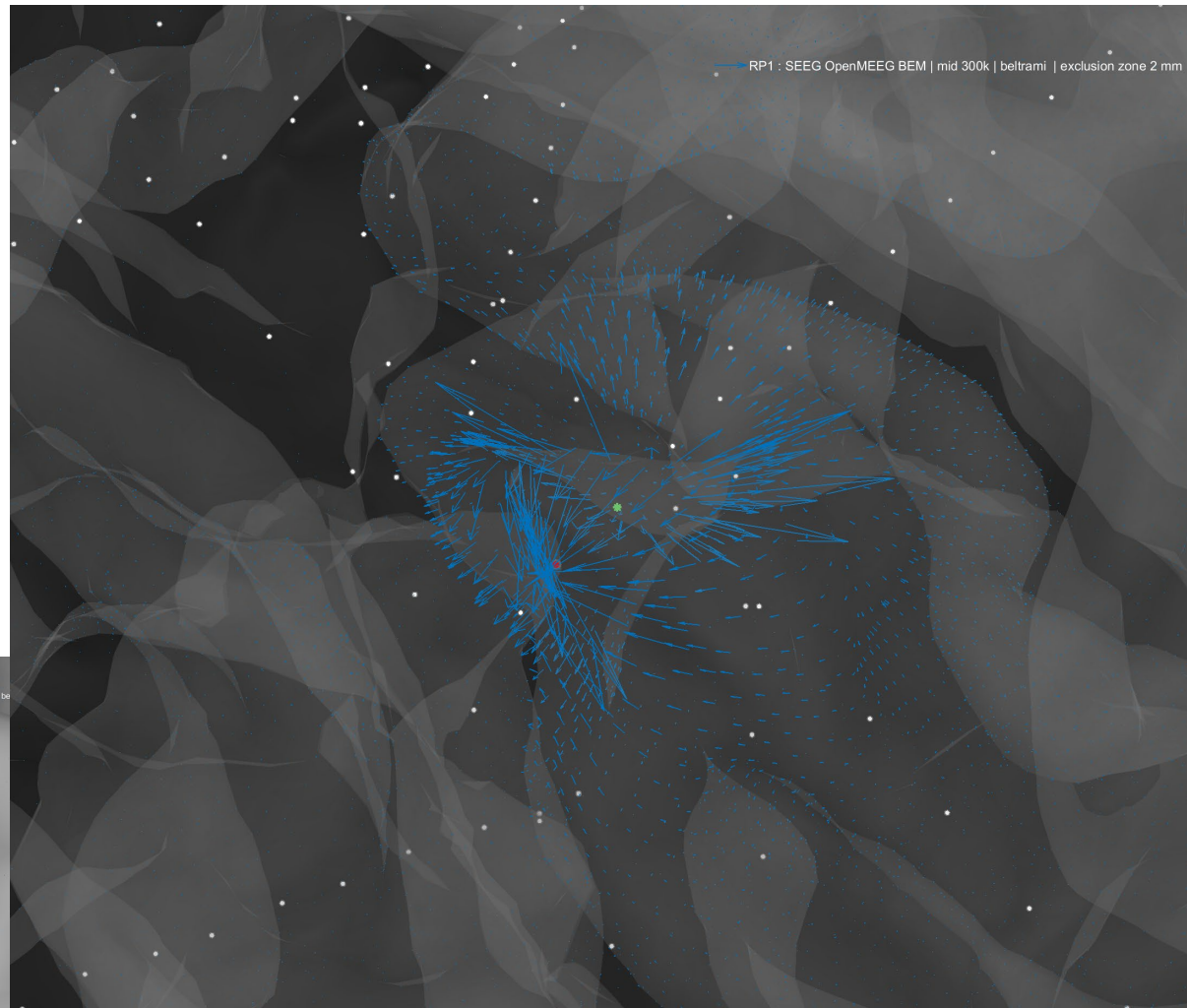
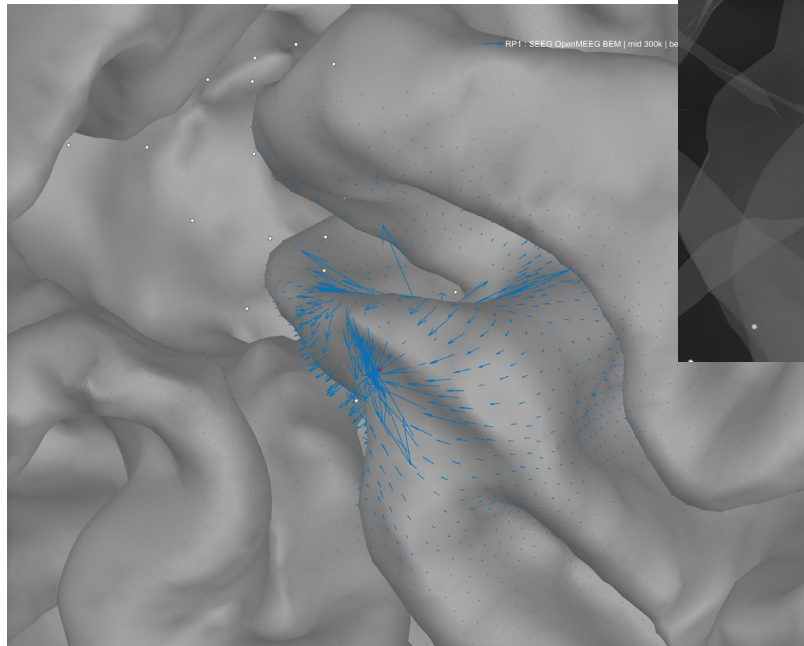
# Leadfields



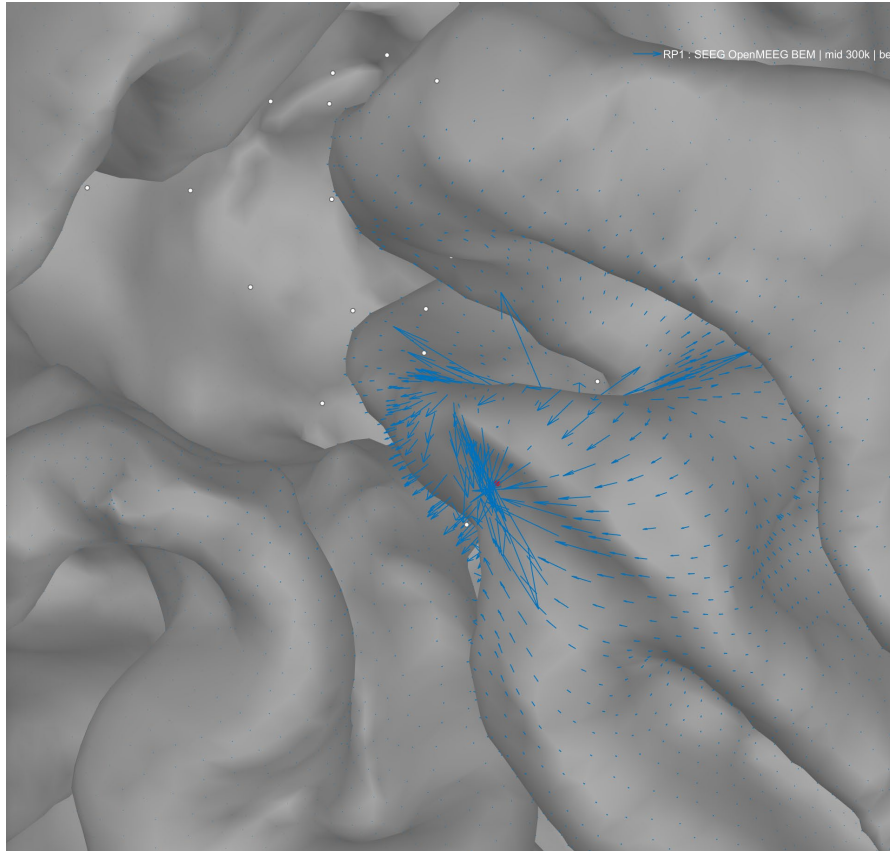
# Leadfields



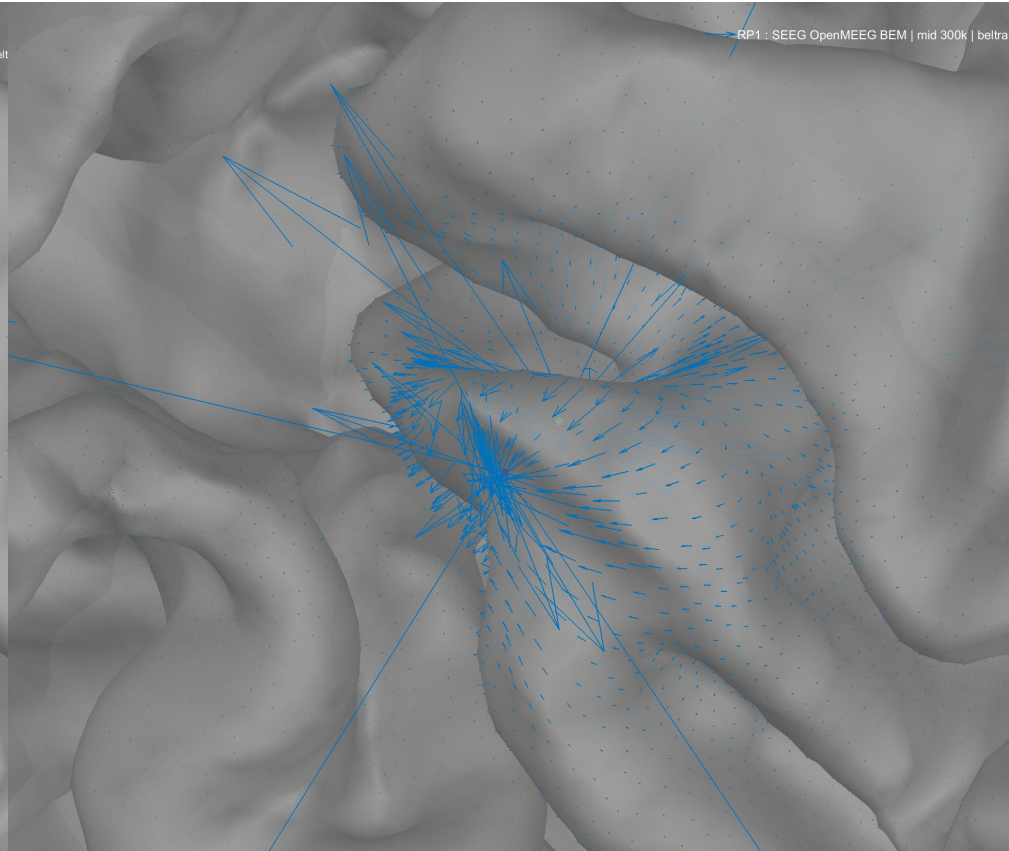
# Leadfields



# Numeric Instabilities Need Trimming



**2mm Exclusion Zone**

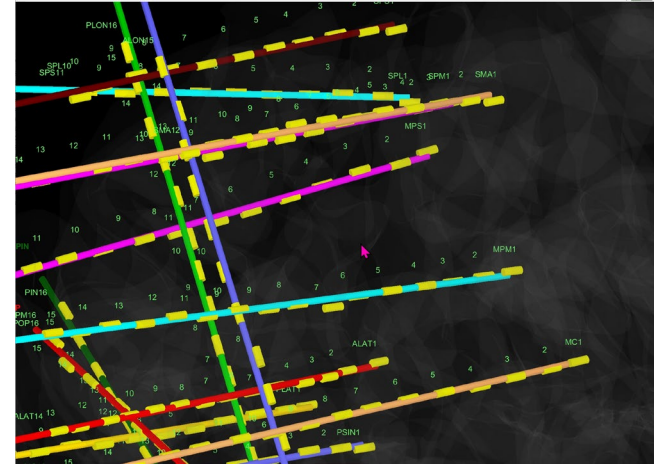


**No Exclusion Zone**



# Stepping through Leadfields

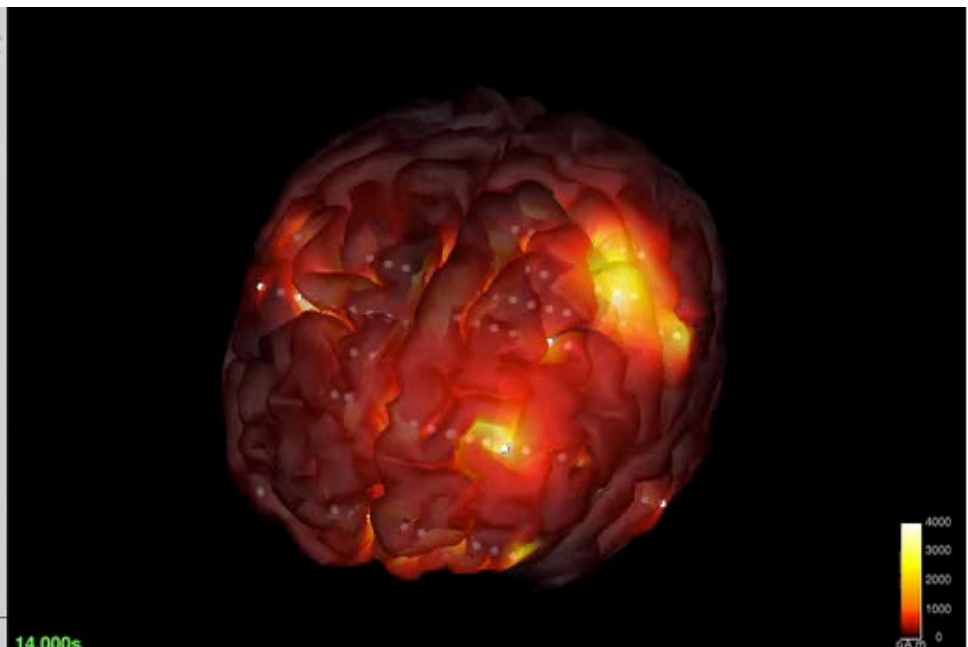
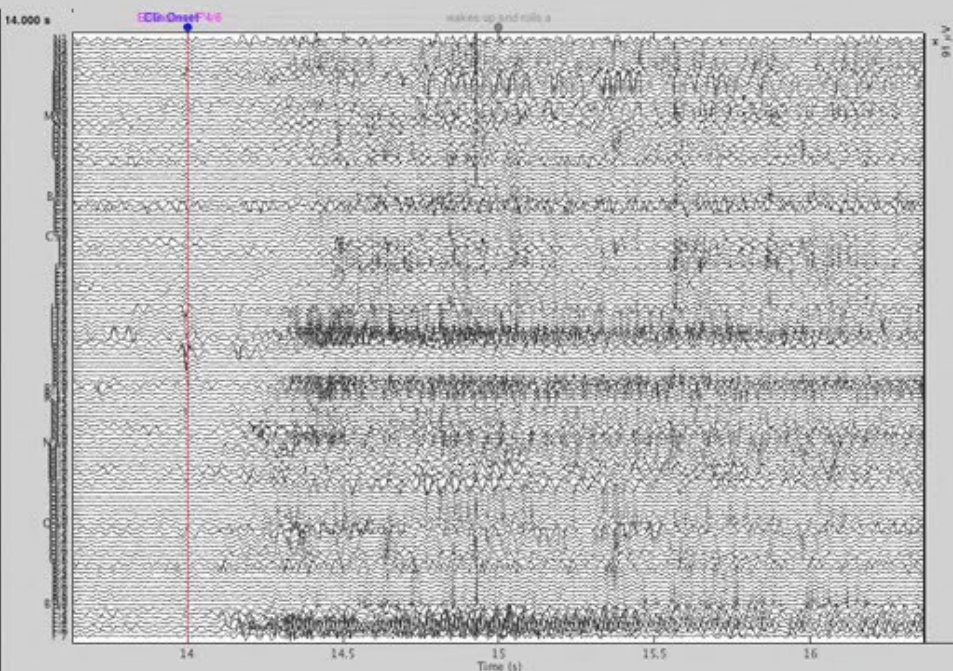
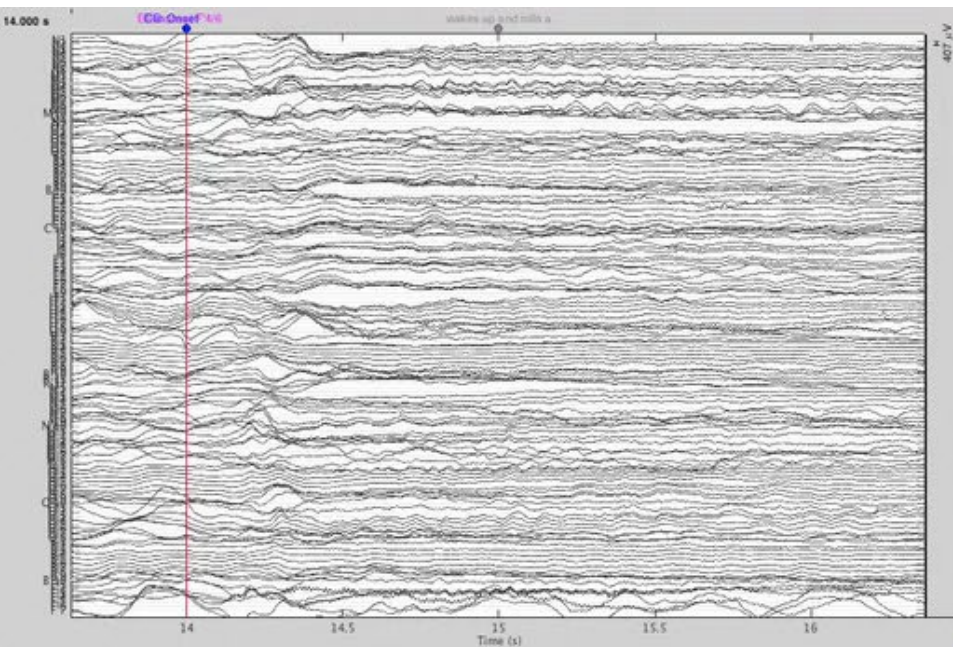
- (VLC Movie: Stepping Through)



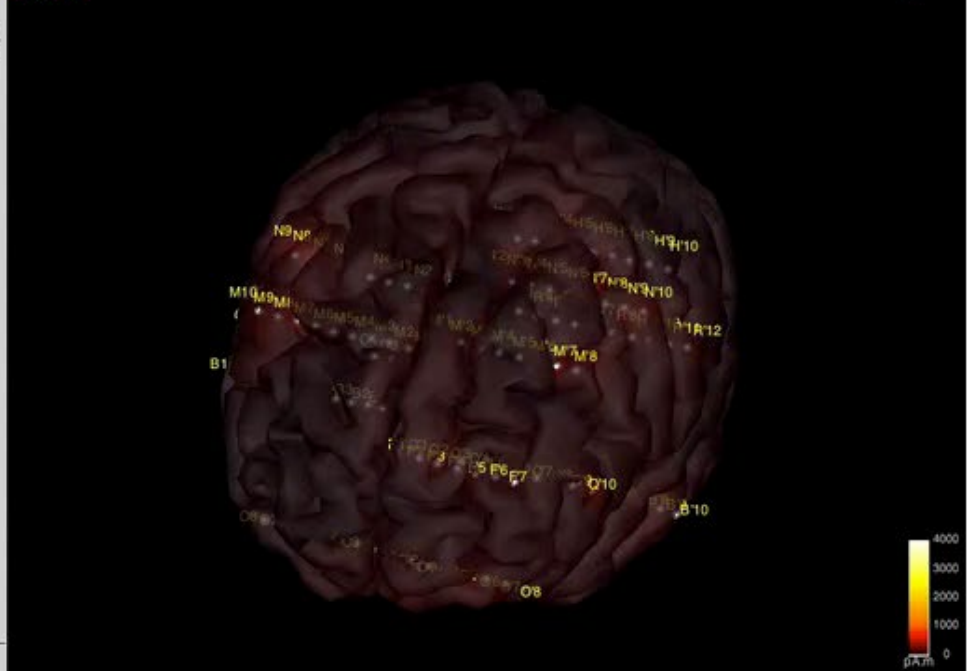
# Source Imaging and Modeling

- Lead fields must be inspected for consistency
- With lead fields approved, minimum norm and its standardizations (sLORETA, dSPM, z-score) provide dynamic “heat maps”
- With good coverage (interpolation), some sources can be localized – dipole models

# SZ - 1/10 speed - 2 seconds - two bands

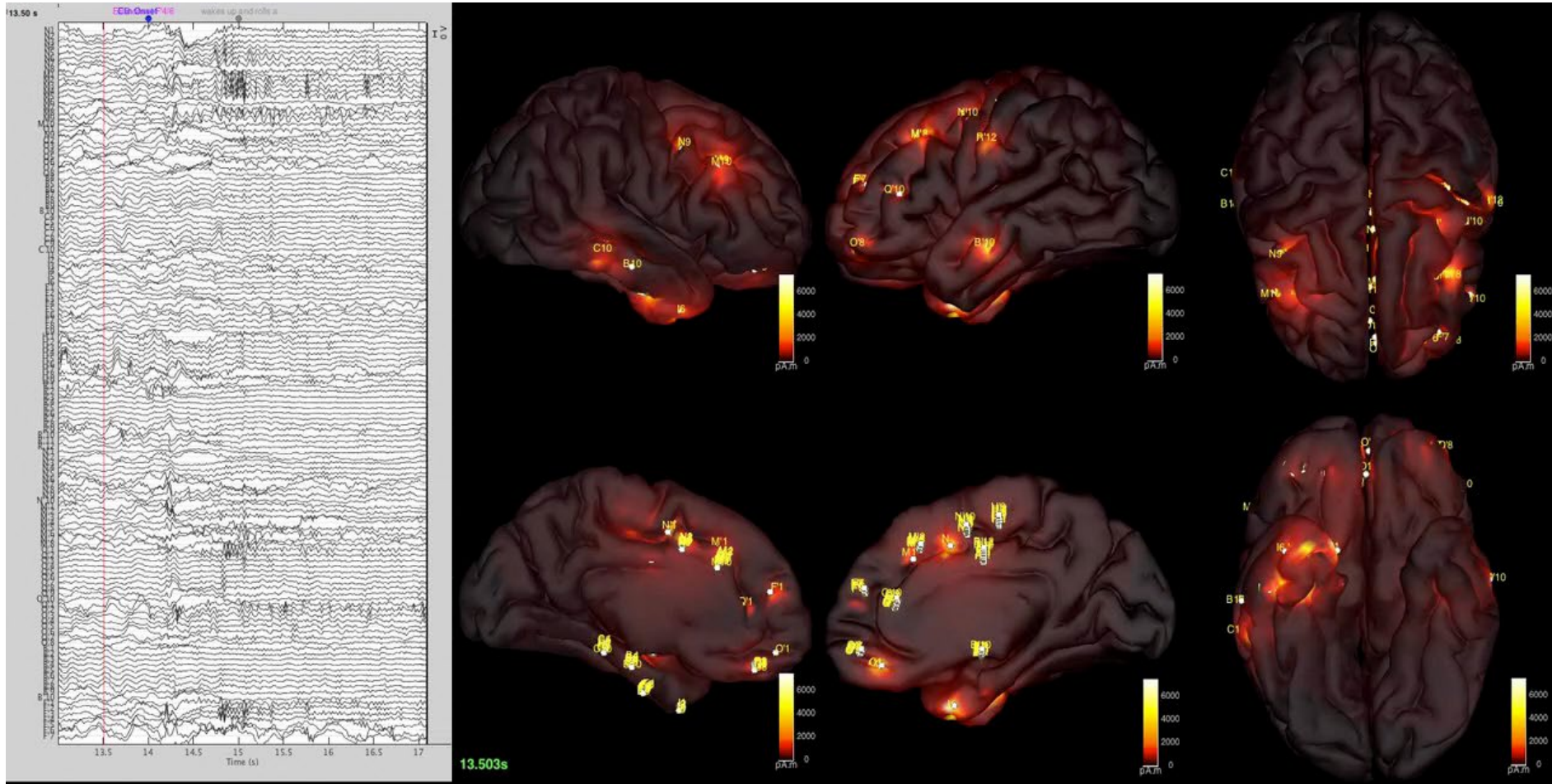


14.000s

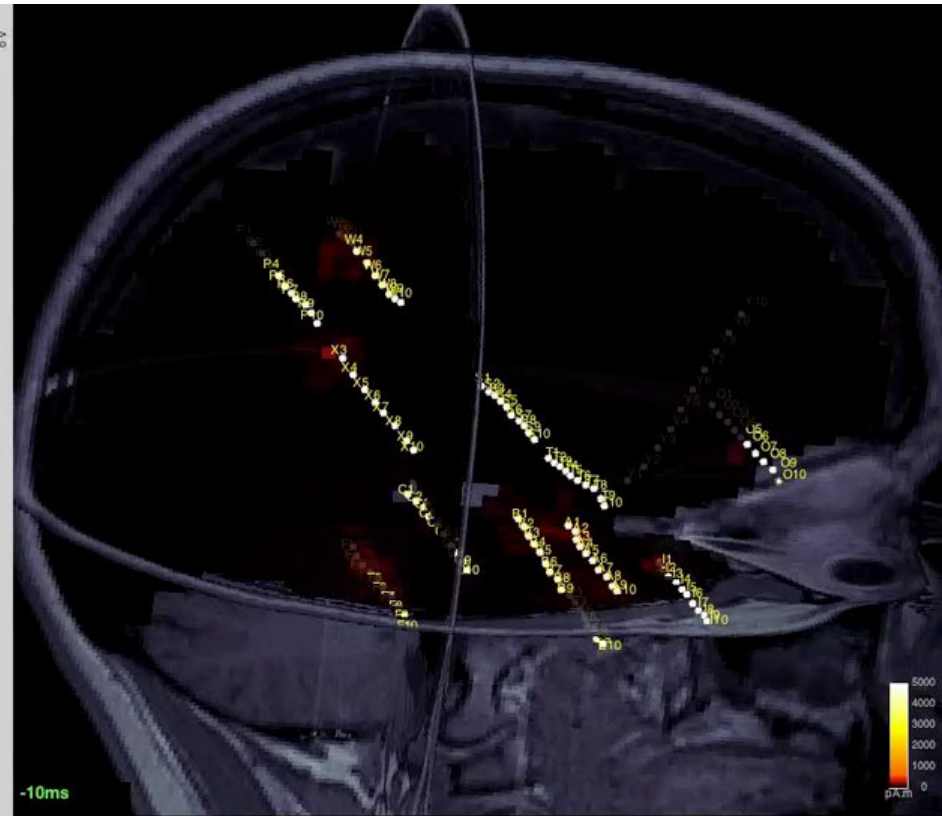
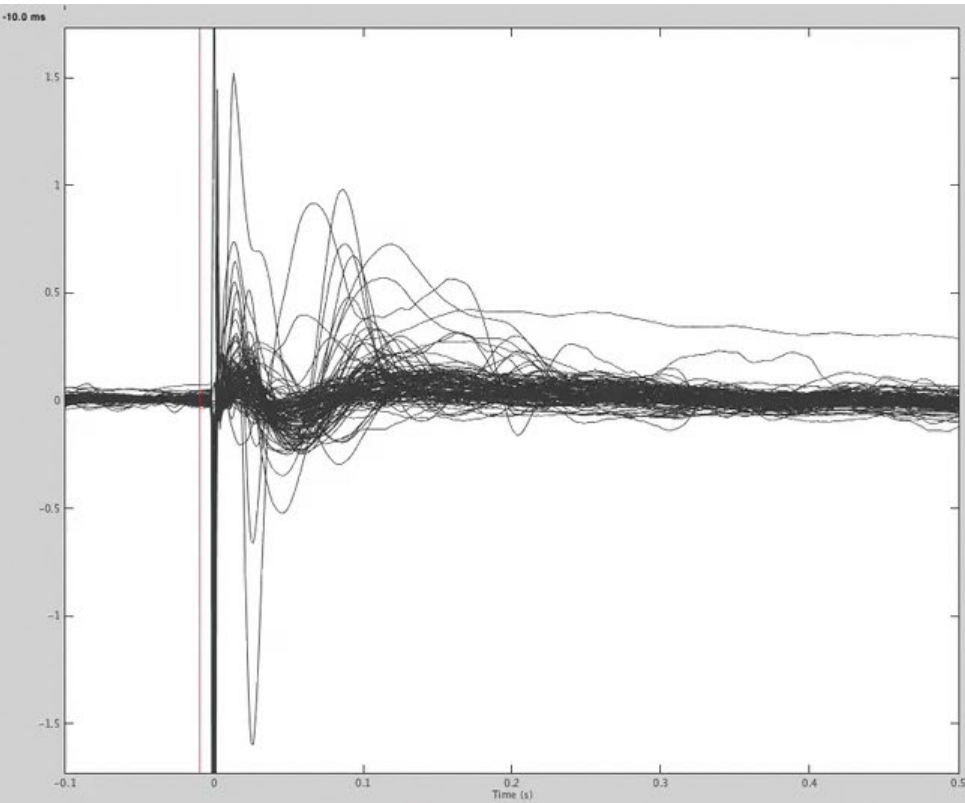


# SZ Onset - Four Seconds Real-Time

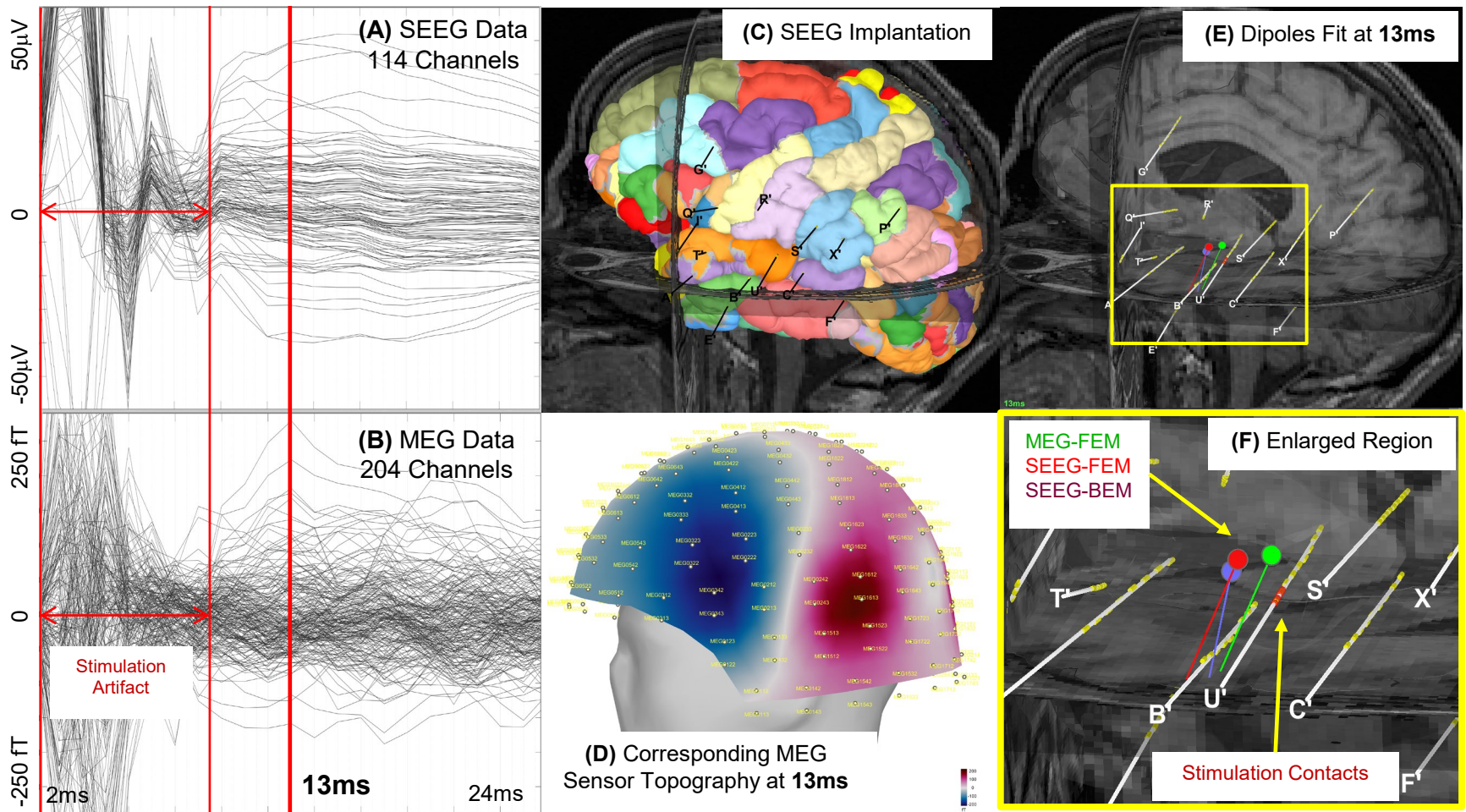
- Simultaneous different views



# CCEPS - 1/10th real-time



# MEG vs SEEG, BEM vs FEM for Dipole Localization



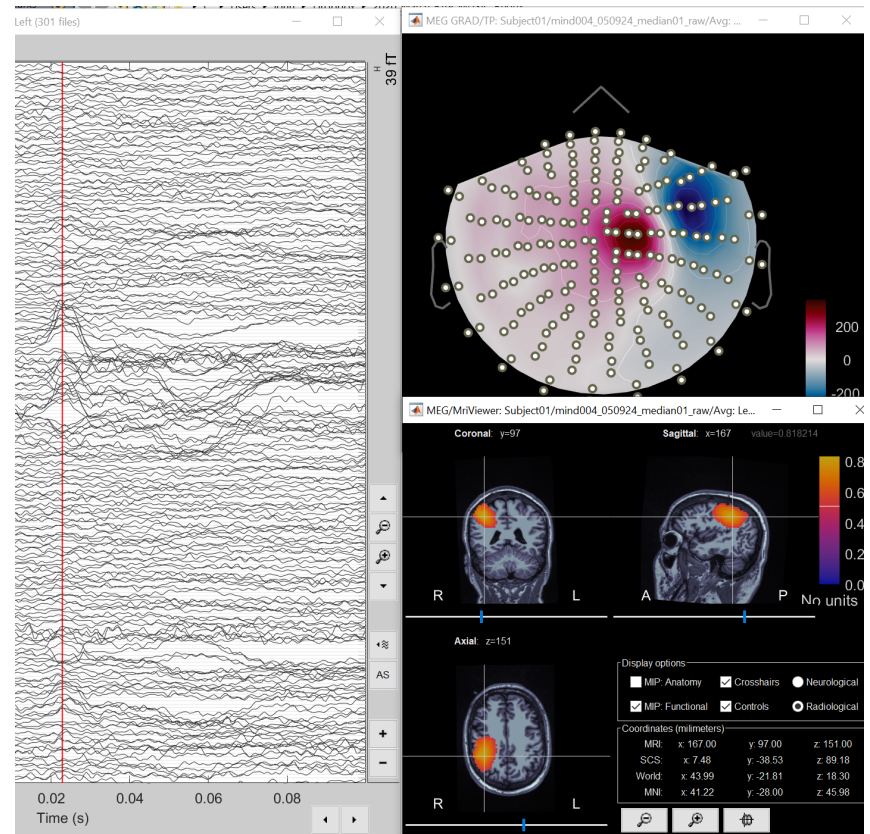
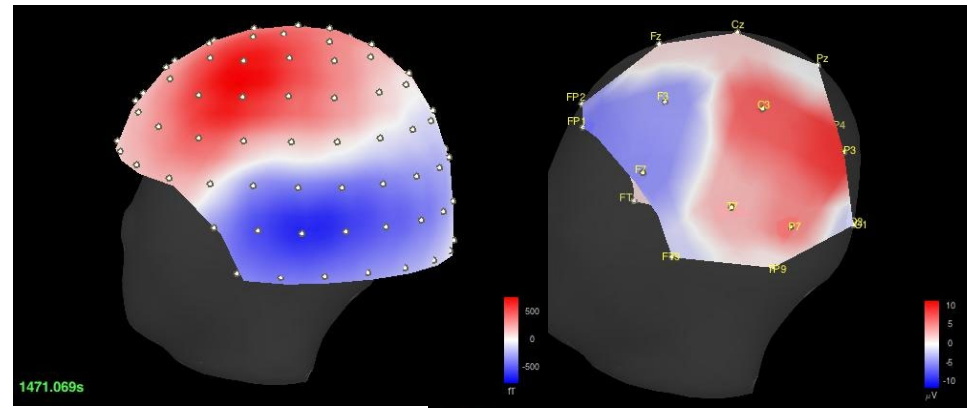
- Bipolar current stimulation at a pair of SEEG contacts produces focal early stimulus artifact and later propagating evoked response, here recorded simultaneously in (A) SEEG and (B) MEG arrays. (C) SEEG electrode locations (black) relative to the USC brain atlas coregistered to individual anatomy. (D) MEG sensor topography of the evoked response at 13ms. (E) Brain locations of dipole models: using SEEG-BEM (blue), SEEG-FEM (red) and MEG-FEM (green). (F) Enlarged view.

# Dipole Interpretation Summary

- The Cortical Column represents a useful model of the gray matter, with EPSPs and IPSPs flowing up and down the column.
- Vertices from the tessellation of the cortex easily represent these cortical columns. In turn, these tessellations are easily joined to form patches of cortex.
- These extended sources nonetheless compress to models of point **equivalent** current dipoles (not shown today, see Jerbi 2004).
- We can directly **estimate** the location, orientation, and dipolar strength of these equivalent current dipoles.
- The true extent of the source can be **inferred** through the **Okada Constant** for source densities, about 1 nA-m per square mm.
- Minor variations in the assumed current density dramatically change this source extent, from 0.1 – 1.0 nA-m/mm<sup>2</sup>.
- Any more sophisticated models of source extent should explicitly clarify this assumption of density.

# Overall Summary

- Lead field modeling reveal how currents flow through our assumed head model and allows us to spot errors.
- Head models range from the simple sphere, overlapping spheres, boundary elements, and finite elements.
- OpenMEEG and DuneNEURO easily interfaced from within Brainstorm
- Visualization and pruning very important due to sources and sensors lying in the same space.
- Min norm “heat maps” are particularly useful in SEEG, showing dynamics effectively
- Source imaging via sLORETA standardization of the min norm effective in coming “off” the contacts and into the volume
- Source modeling such as current dipoles possible when coverage is adequate





# Brainstorm Contributors

## Investigators



Sylvain Baillet  
*MNI*



Richard Leahy  
*USC*

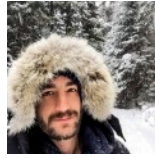


John Mosher  
*UT Houston*



Dimitrios Pantazis  
*MIT*

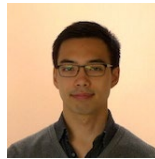
## MEG @ McGill



Konstantinos Nasiotis  
*PhD student*



Soheila Samiee  
*PhD student*



Jeremy Moreau  
*PhD student*

## Key collaborators



Elizabeth Bock  
*MEGIN, Chicago*



Guiomar Niso  
*Politécnica Madrid*



Juan Garcia-Prieto  
*Martinos, Boston*

## Geeks



François Tadel  
*Software, Grenoble*



Raymundo Cassani  
*Software, MNI*



Marc Lalancette  
*MEG manager, MNI*

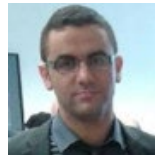
## SIPI @ USC



Anand Joshi  
*RA Professor*



Hossein Shahabi  
*Research assistant*

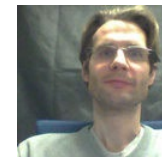


Takfarinas Medani  
*Research assistant*

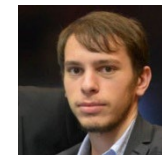
## NIRSTORM



Christophe Grova  
*Concordia*



Thomas Vincent  
*Montreal Heart Inst*



Edouard Delaire  
*Concordia*