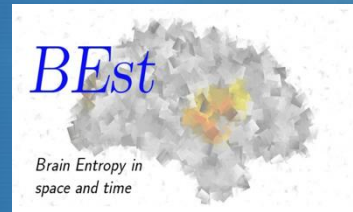


Presentation of two Brainstorm plugins:
(1) Brain Entropy in space and time (BEst) for Maximum Entropy on the Mean source imaging
(2) NIRSTORM plugin dedicated for fNIRS analysis

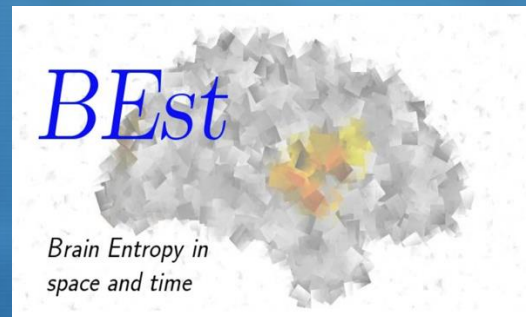


Christophe Grova

Physics Dpt, PERFORM centre, Concordia University
Biomedical Engineering Dpt, McGill University
Montreal Neurological Institute
Centre de Recherches Mathématiques, Montréal
Canada

christophe.grova@concordia.ca

Part 1: EEG/MEG source imaging using Maximum Entropy on the Mean (MEM)

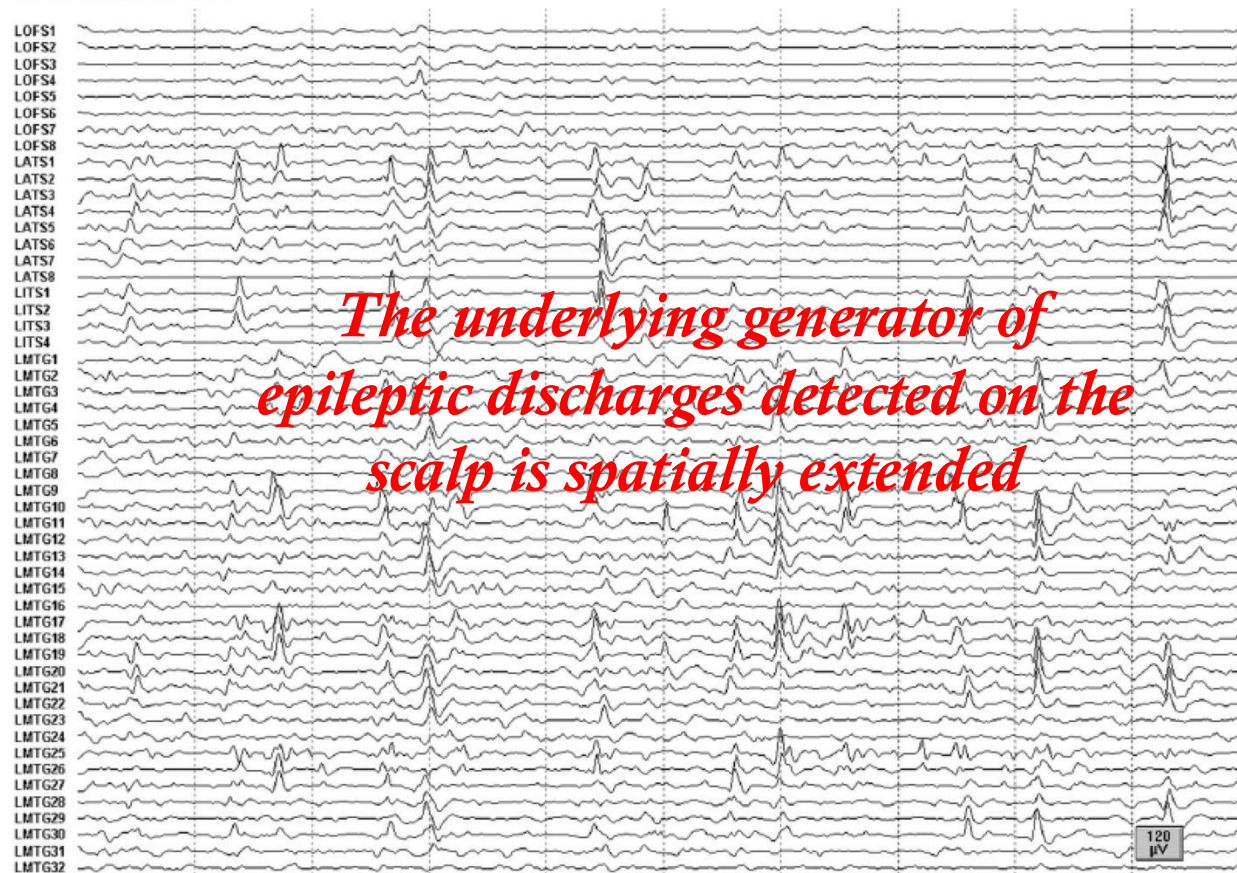


<http://neuroimage.usc.edu/brainstorm/Tutorials/TutBEst>



EEG recording of epileptic discharges

Intracranial EEG



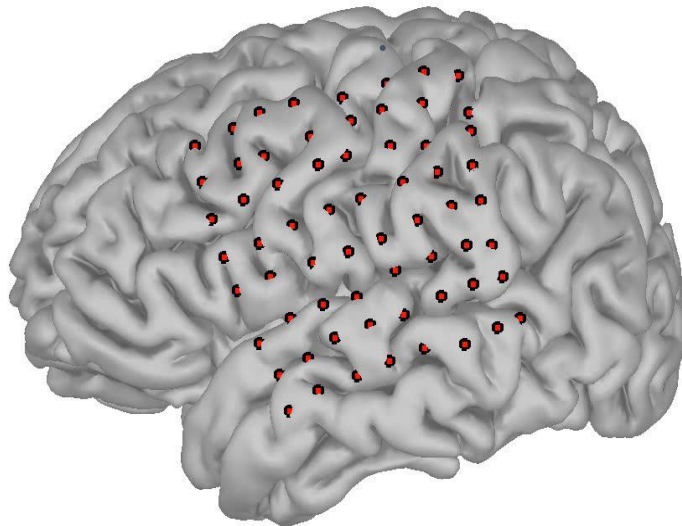
Should we have spatially extended generators to detect epileptic discharges from the scalp. What is the true underlying extent ?

Spike generators of 4 to 8 cm² can generate scalp EEG signals with good SNR

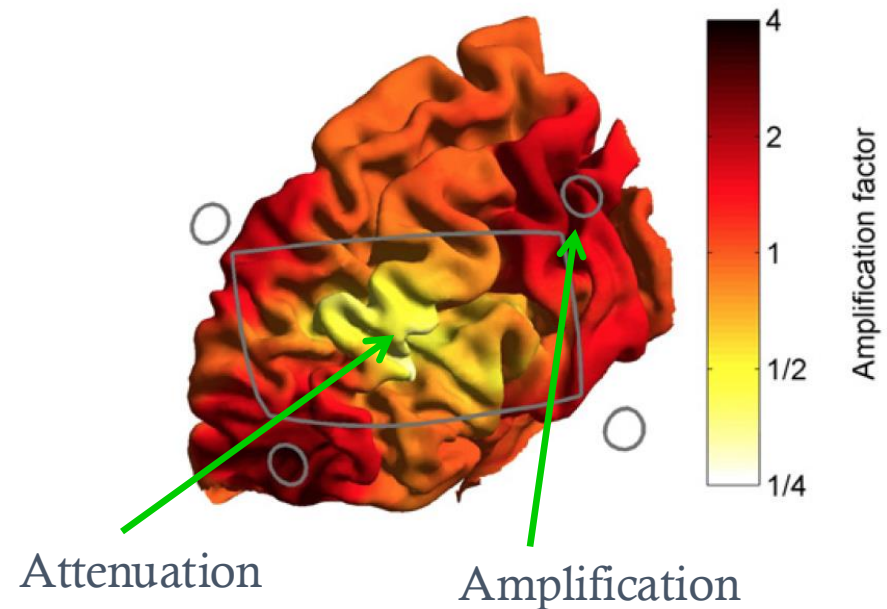
A minimum of 3-4 cm² can generate MEG signals with good SNR

(Oishi et al Epilepsia 2002)

An ECoG grid is not covering the whole underlying surface



An ECoG grid is influencing local signal to noise ratio (SNR)



Courtesy of T. Hedrich

Von Ellenrieder Neuroimage 2014

*EEG/MEG source imaging and estimation of
the underlying spatial extent of the generators*

*EEG/MEG Source
localization using
Maximum Entropy on the
Mean (MEM)*

*Recover the spatial extent
of the source with good
accuracy*

Brainstorm

<http://neuroimage.uroc.edu/brainstorm>

MEM plugin available in
Brainstorm software

- MEM in the time domain: interesting spatial properties and the ability to recover the **spatial extent of the underlying sources**
- Wavelet based MEM (wMEM): MEM localization after time-frequency decomposition of the data using discrete wavelets. **Ideal to localize oscillations.**
- Ridge MEM (rMEM): localization of **synchronous** sources

**Co-Developer /
Main Collaborator**

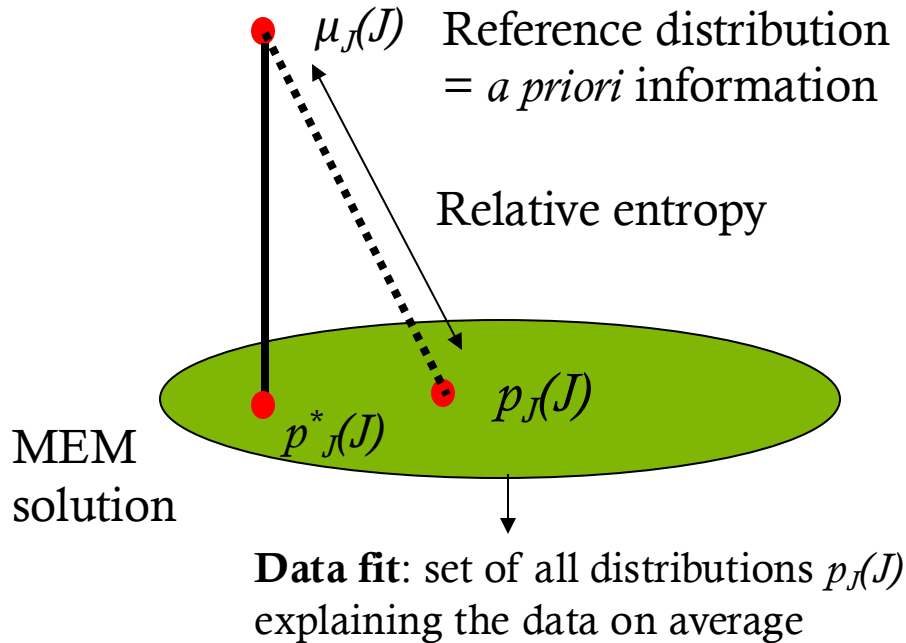
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Jean-Marc Lina, PhD

Solving the EEG/MEG inverse problem: Maximum Entropy on the Mean (MEM) model

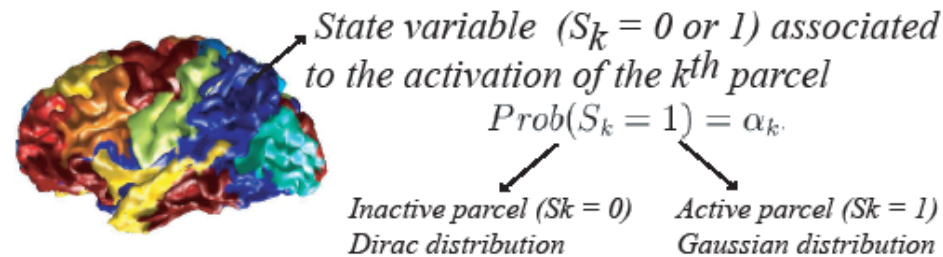
Maximum Entropy on the Mean (MEM)



Prior information on J: Brain activity distributed over K cortical patches

$$d\mu(\mathbf{j}) = \prod_{k=1}^K [(1 - \alpha_k)\delta(\mathbf{j}_k) + \alpha_k \mathcal{N}(\mu_k, \Sigma_k)(\mathbf{j}_k)] d\mathbf{j}$$

Parcelling of the cortical surface in K parcels:



Grova et al, Neuroimage. 2006;29(3)

Amblard et al, IEEE BME. 2004;51(3)

Chowdhury et al, Neuroimage 2016; 43:175-195

Point Spread Function of an extended source Resolution matrix study



Tanguy Hedrich

MEG

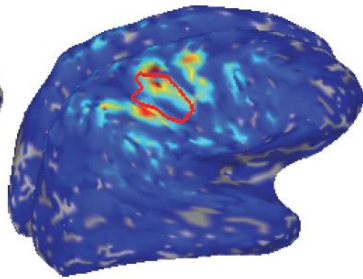
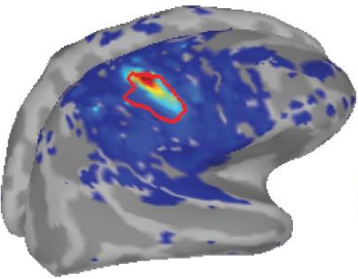
hdEEG

cMEM

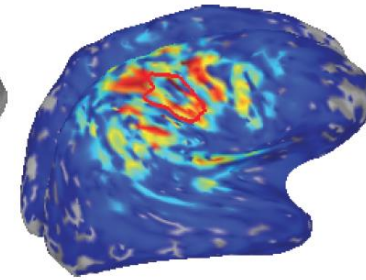
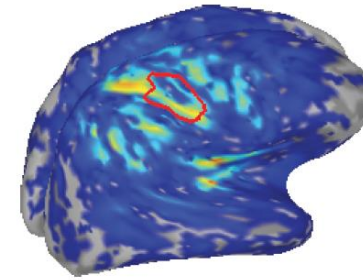
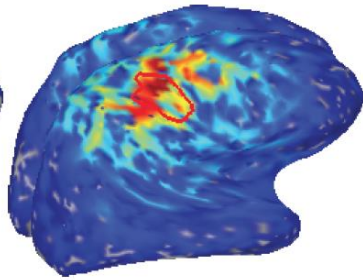
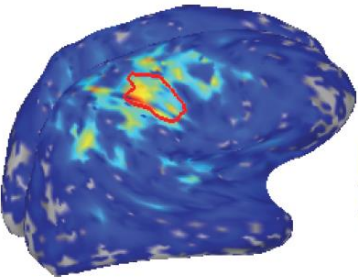
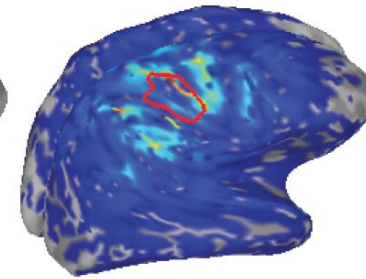
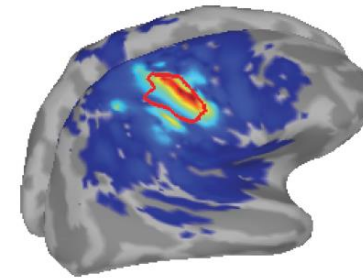
MNE

cMEM

MNE



source



dSPM

sLORETA

dSPM

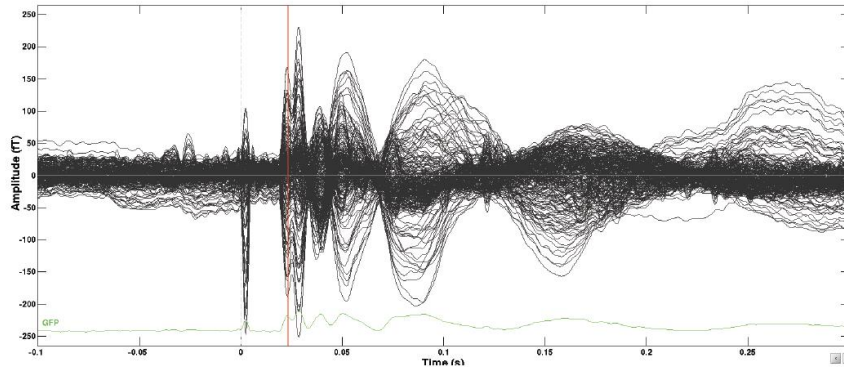
sLORETA

Electrical median nerve stimulation in 5 healthy controls in MEG

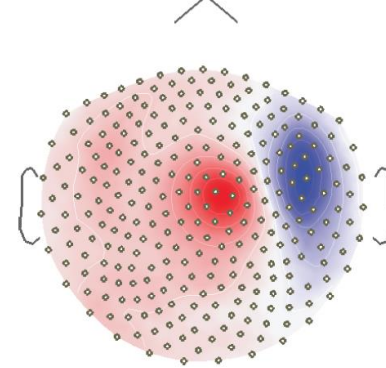


Tanguy Hedrich

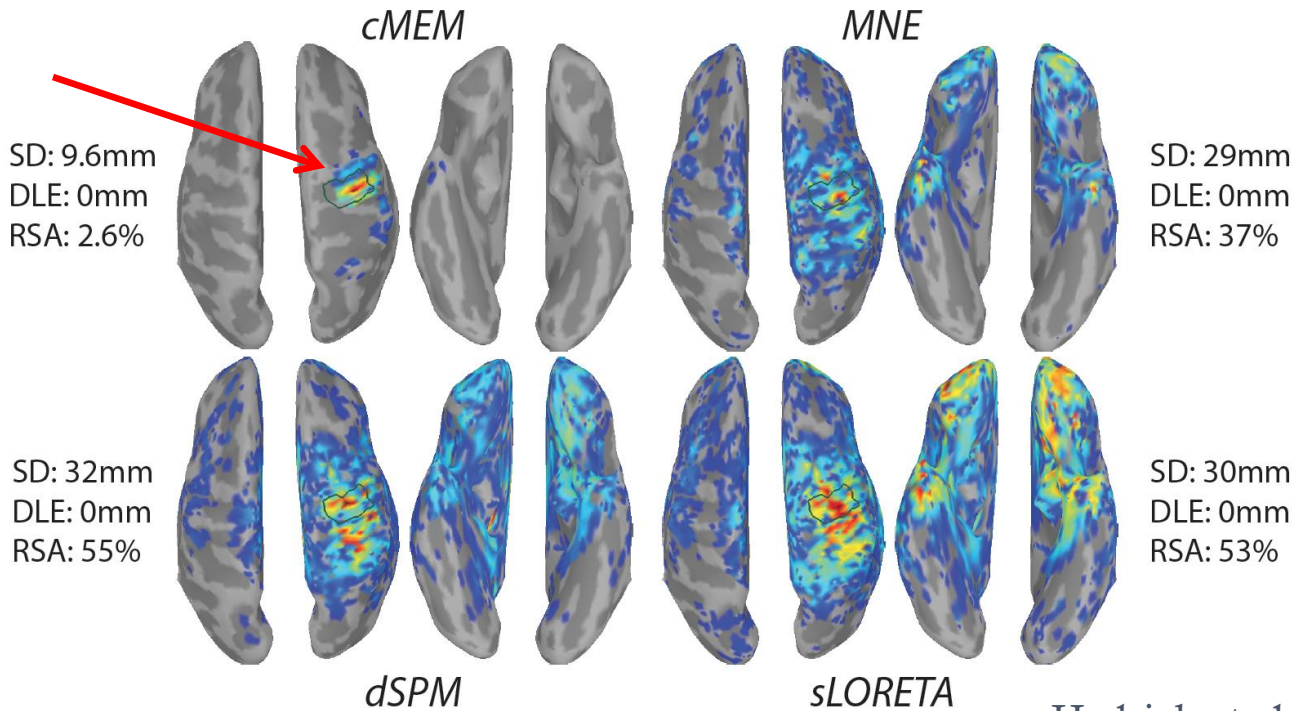
MEG butterfly plot



MEG topographic plot at 20ms



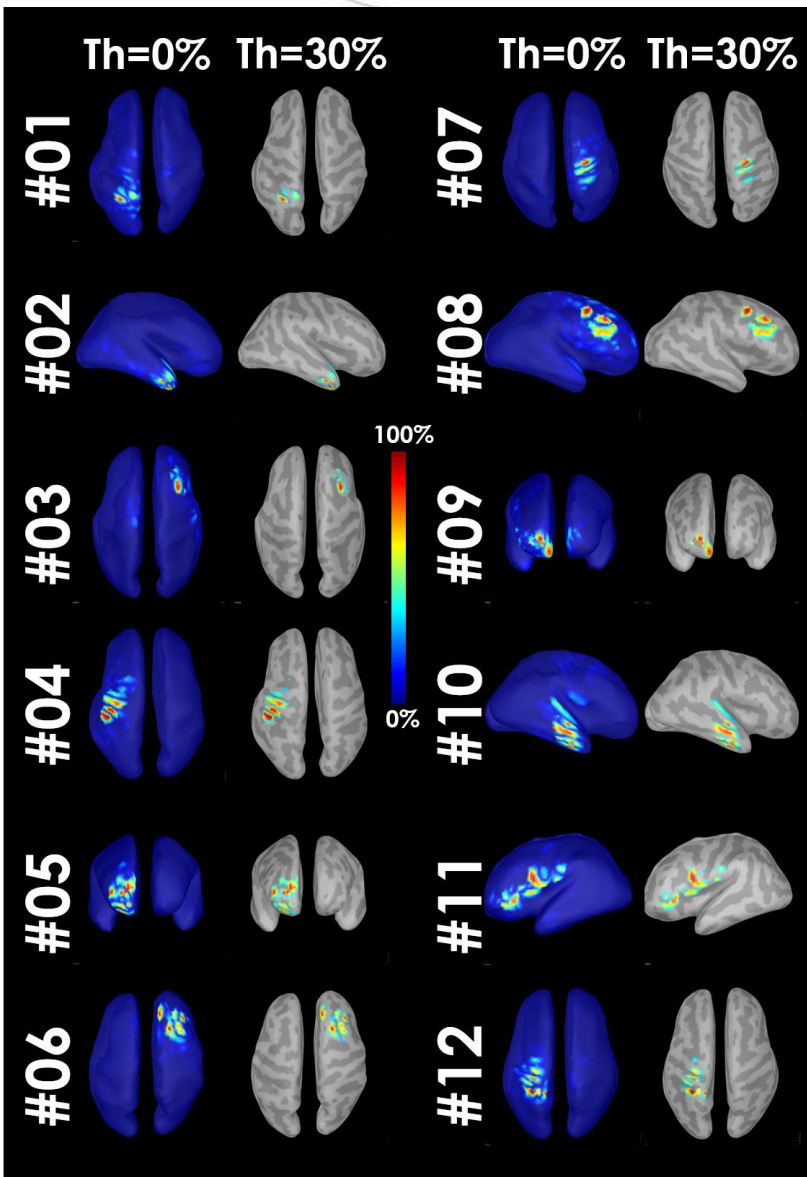
Reference:
Anatomical
Landmark
of S1



Clinical yield of MEG source localization using cMEM in epilepsy in 340 studies (49 patients)



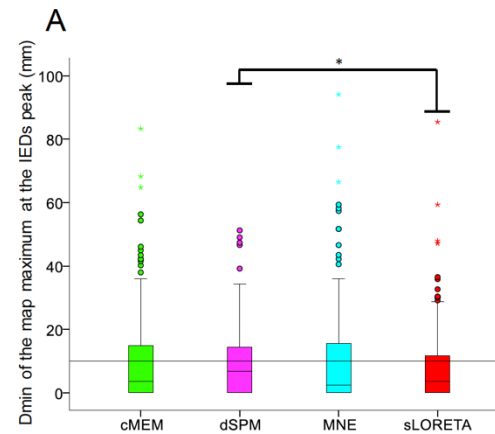
Giovanni Pellegrino



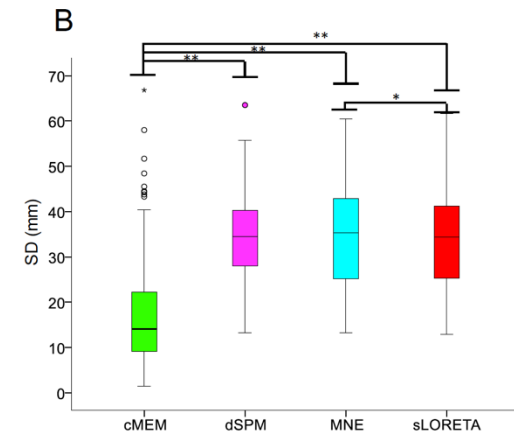
Comparison of several distributed sources

Localization methods:

MEM, MNE, dSPM, sLORETA



Distance to the focus



Spatial spread around the focus

Outline

- ◆ Basic principle of source localization and imaging in EEG/MEG
- ◆ **Validation of EEG/MEG source imaging with intracranial EEG**
- ◆ EEG/MEG source imaging of oscillatory patterns
- ◆ EEG/MEG source imaging of deep activity
- ◆ EEG/MEG source imaging of resting state

Clinical Yield of Electromagnetic Source Imaging and Hemodynamic Responses in Epilepsy

Validation With Intracerebral Data

Chifaou Abdallah, MD, Tanguy Hedrich, PhD, Andreas Koupparis, MD, PhD, Jawata Afnan, MSc, Jeffrey Alan Hall, MD, PhD, Jean Gotman, PhD, Francois Dubeau, MD, Nicolas von Ellenrieder, PhD, Birgit Frauscher, MD, PD, Eliane Kobayashi, MD, PhD, and Christophe Grova, PhD

Correspondence

Dr. Abdallah
chifaou.abdallah@mcgill.ca

Neurology® 2022;98:1-13. doi:10.1212/WNL.0000000000200337

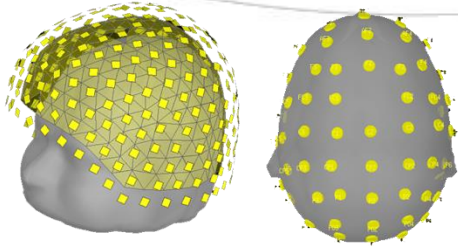


Chifaou Abdallah

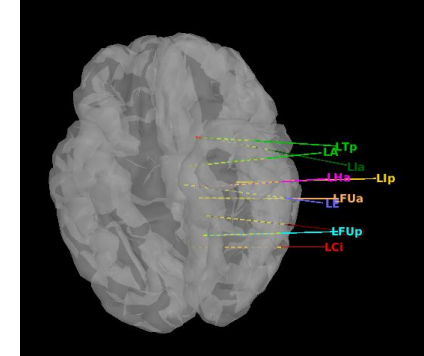
*Quantitative comparison between
EEG/MEG fusion using MEM,
EEG/fMRI and intracranial EEG*



Clinical yield of electromagnetic source imaging and hemodynamic responses in epilepsy: validation with intracerebral data



brainproducts.com



MEG+EEG: ~300 MEG sensors ,
60 EEG electrodes

Sampling Rate: at least **1200Hz**,
About 1h recording, divided in **6 min runs**



**Simultaneous EEG/fMRI
+ Anatomical MRI (3T)**

Head model, Hemodynamic
response to epileptic spikes



**Intracranial EEG
(iEEG)**

Gold Standard

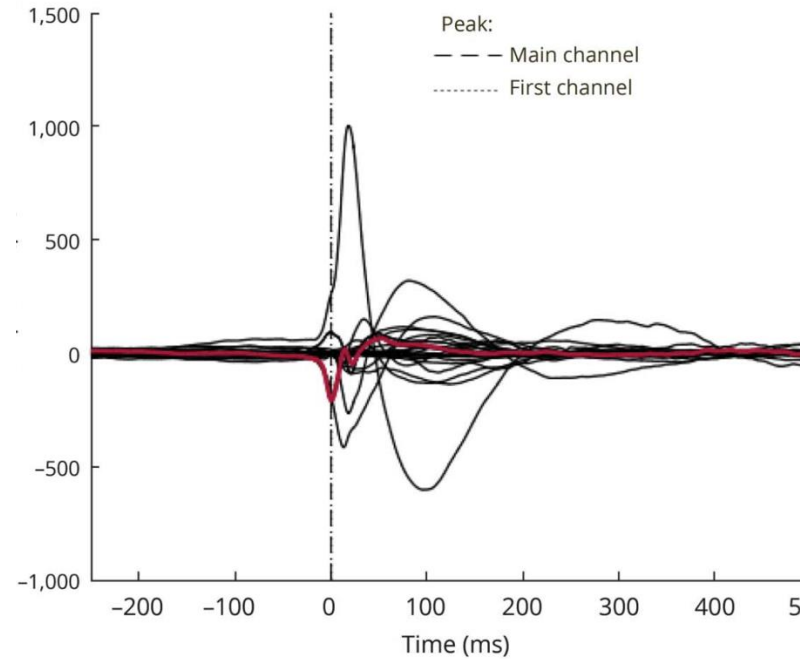
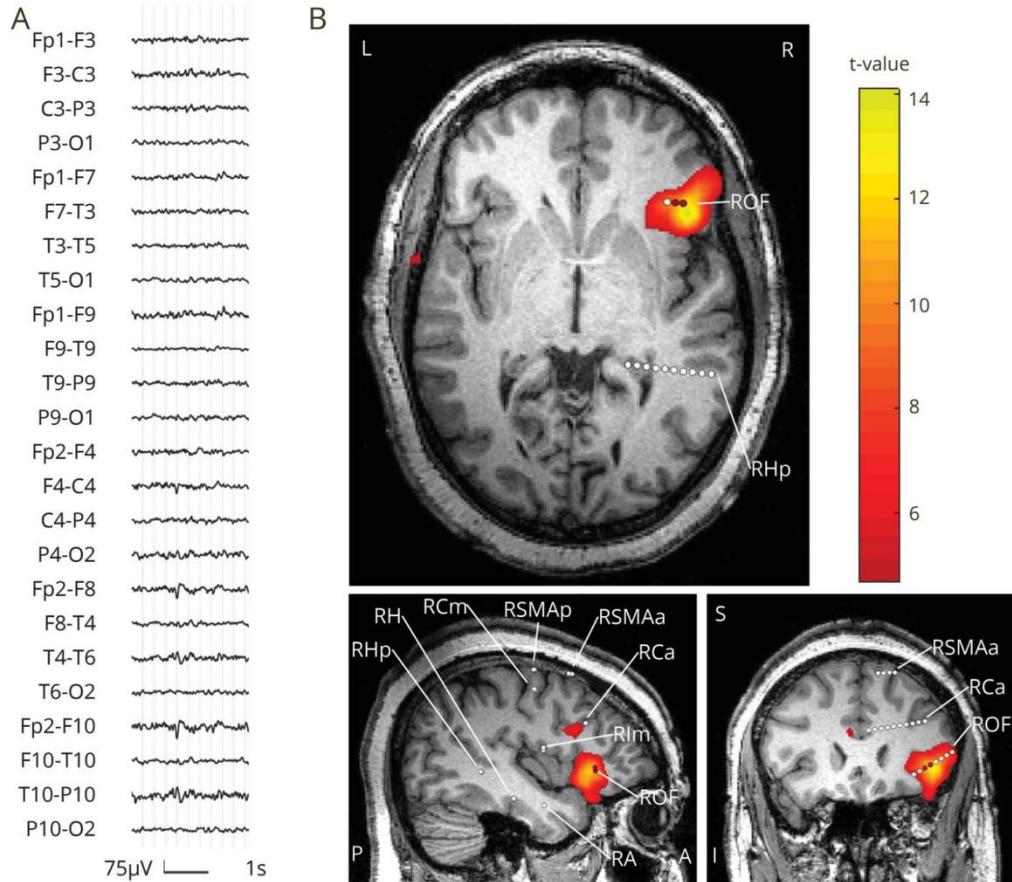
17 Patients who underwent EEG/MEG, EEG/fMRI and subsequent iEEG were included

EEG/MEG fusion using MEM (Chowdhury et al HBM 2018) and **fMRI BOLD response** (Khoo et al Neurology 2018) to similar EEG epileptic spikes

Identification of the reference **SOZ** and **Primary Irritative Zone (PIZ)** from iEEG data

Quantitative analysis within the iEEG space: spatial overlap (ROC analysis) and distances

Simultaneous EEG-fMRI: The most significant BOLD response localizing the spike onset

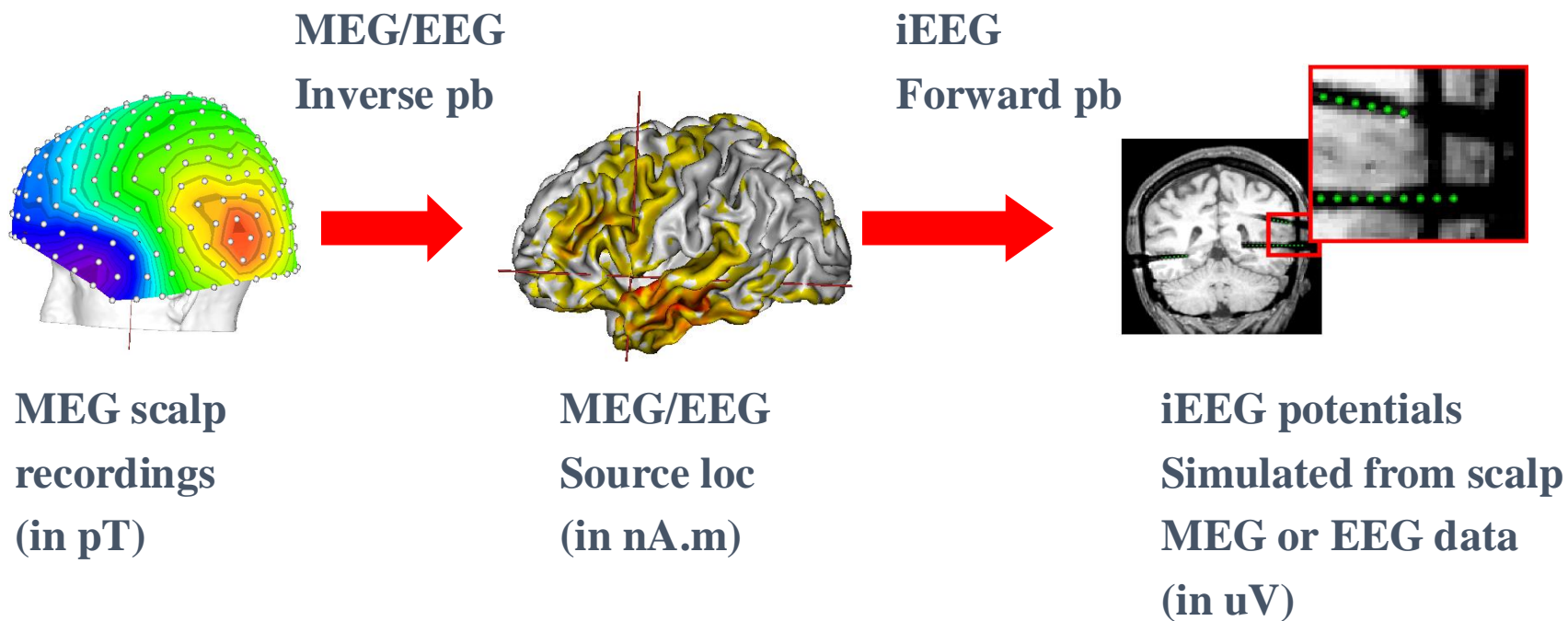


Averaged interictal spike in SEEG

The most significant fMRI BOLD response (pos. or neg.) to interictal discharges delineates a subset of the irritative zone in concordance with the seizure onset zone

→ Spike onset zone

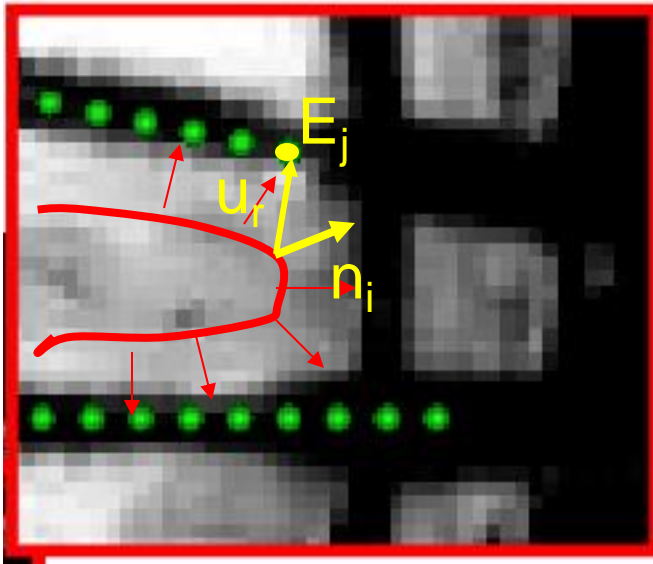
Quantitative correlation between EEG/MEG sources and iEEG



- ◆ One can compare **virtual MEG-estimated iEEG potentials** with **real iEEG potentials**
- ◆ Same physical entities: electrical potentials in V
- ◆ Spatial relationship between the cortical surface and iEEG contact: **iEEG forward model**

iEEG forward model: infinite volume conductor model

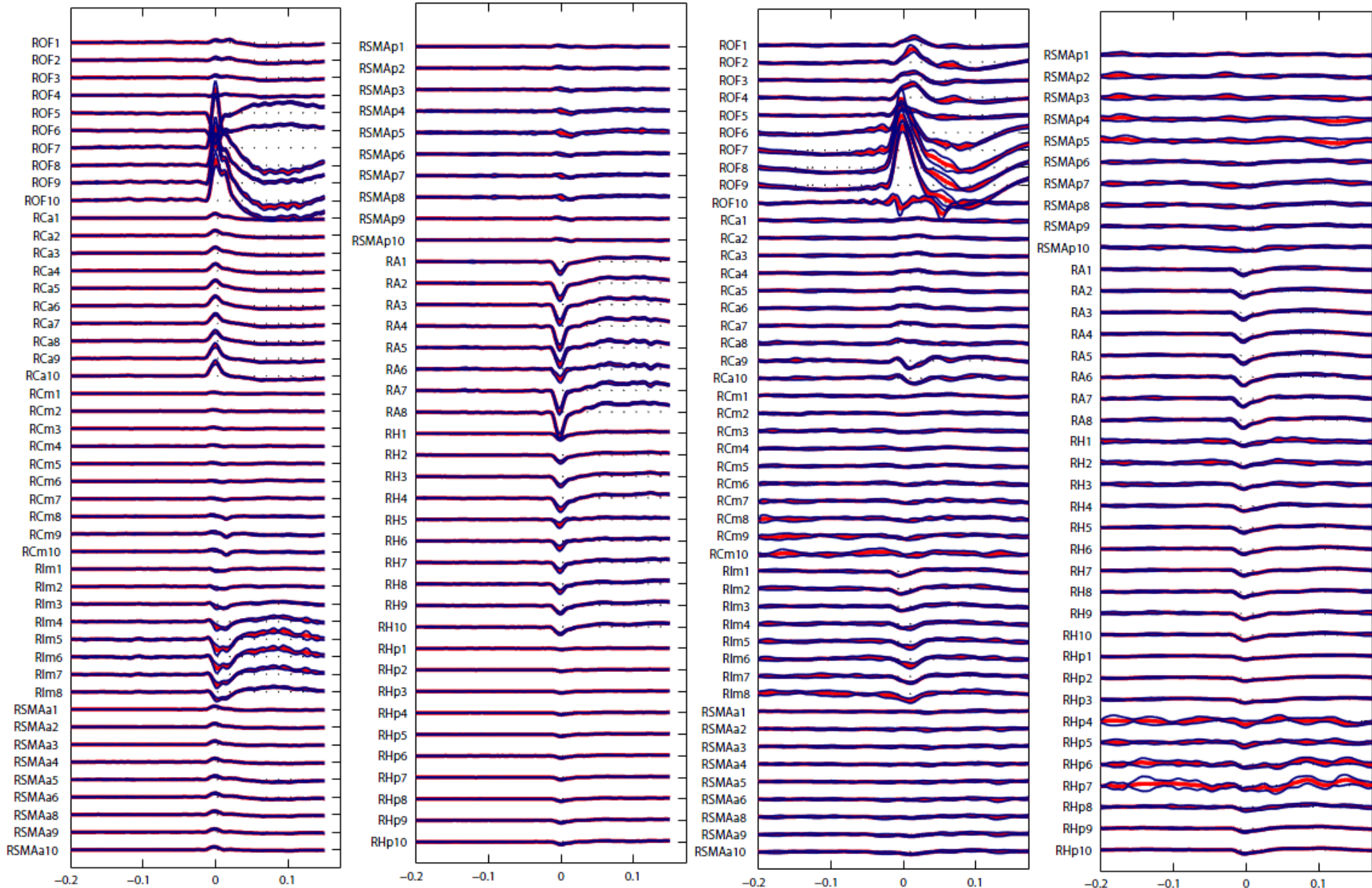
$$V(E_j) = \frac{\vec{n}_i \cdot \vec{u}_r}{4\pi\sigma r^2}$$



Electrical potential created by the i th dipolar source of the cortical surface on the j th iEEG electrode contact, located at a distance r from the source

Key parameters

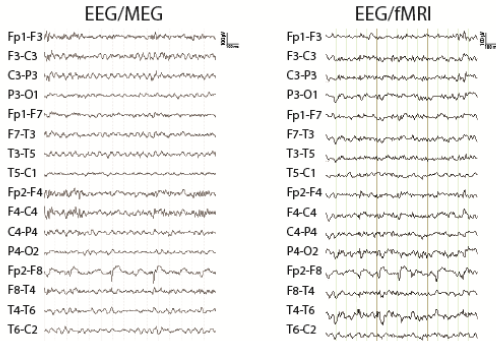
Distance and source orientation

(v) Simulated iEEG potentials from MEG sources V_{MEG} (vi) Recorded iEEG potentials V_{iEEG}

Multimodal comparison involving EEG/MEG fusion, EEG/fMRI and intracranial EEG

A. Spike selection

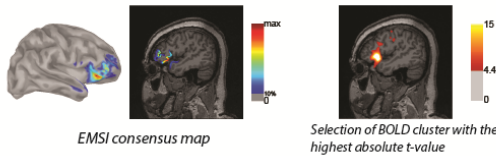
Spikes with same EEG spatial distribution



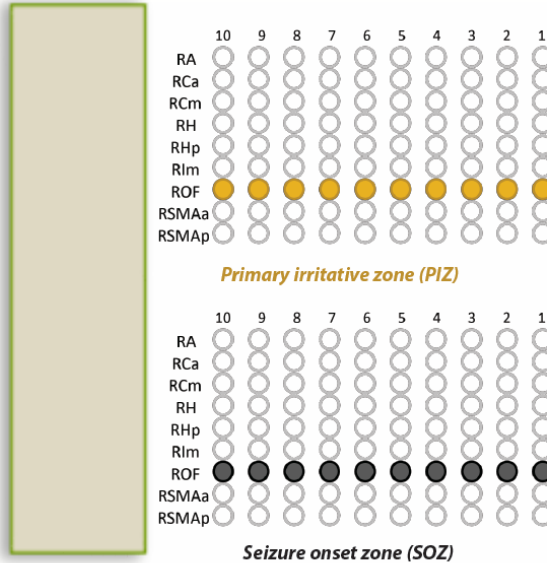
B. Functional imaging

EEG/MEG source localization

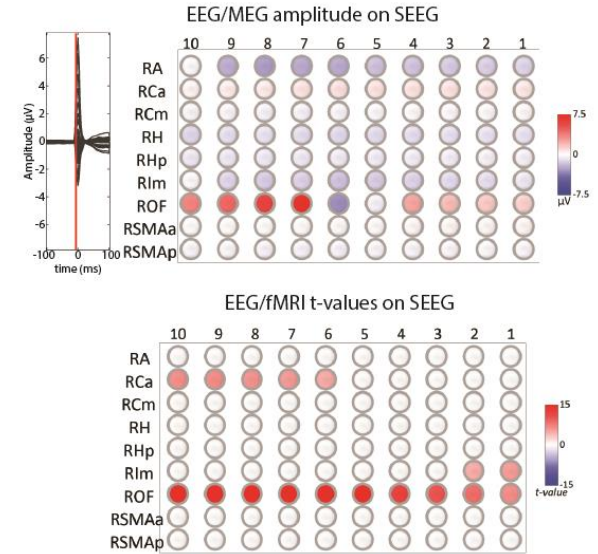
fMRI BOLD analysis



C. Reference selection (SEEG)



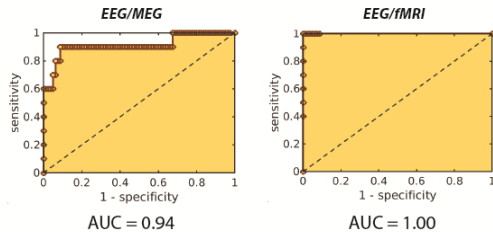
D. Projection of functional Imaging results on SEEG channels



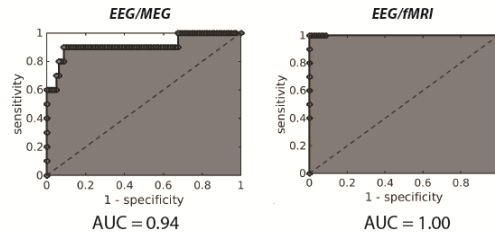
E. Comparison with SEEG findings

1. Area under the ROC curve (AUC)

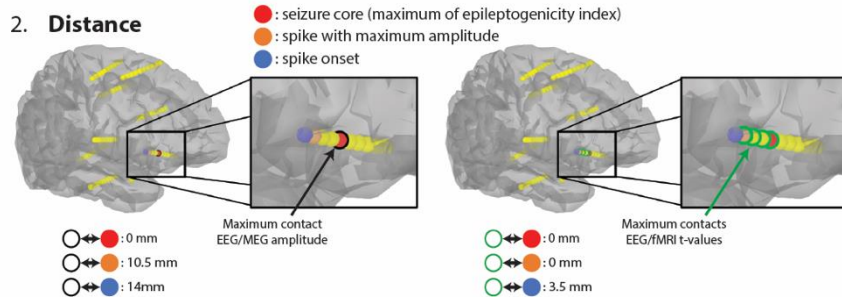
Primary irritative zone (PIZ)



Seizure onset zone (SOZ)



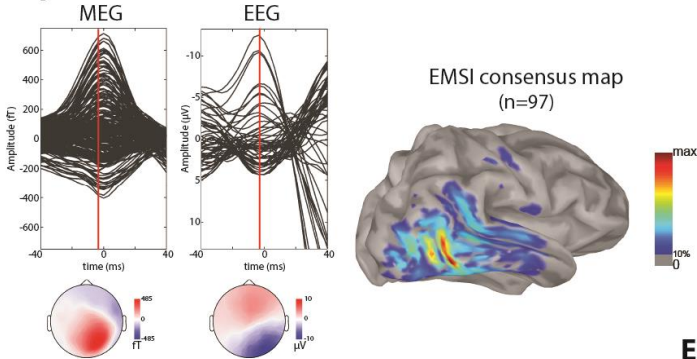
2. Distance



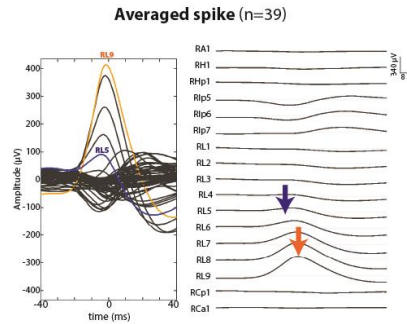
Multimodal comparison involving EEG/MEG fusion, EEG/fMRI and intracranial EEG

PATIENT 9

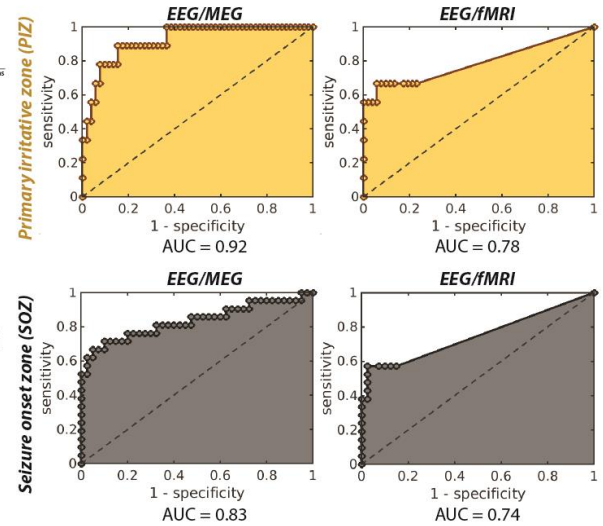
A. Spike source localization



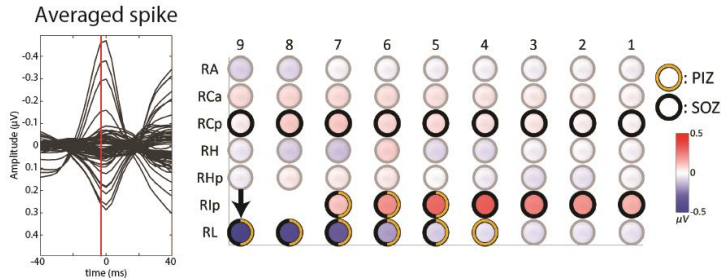
D. SEEG spike signal



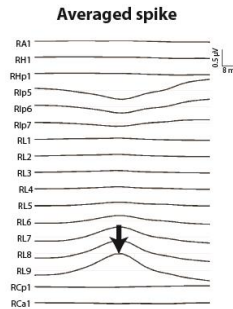
G. Area under the ROC curve (AUC)



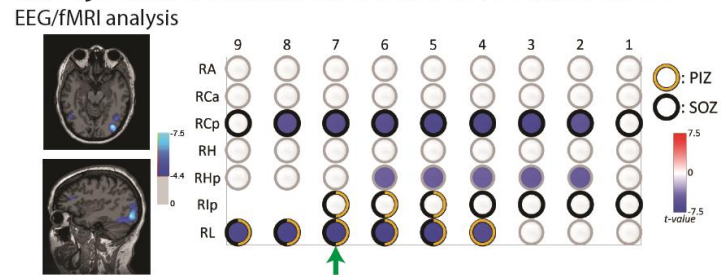
B. SEEG estimated from EEG/MEG + SEEG references



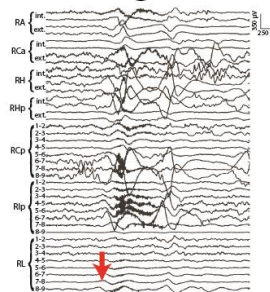
E. SEEG estimated from EEG/MEG



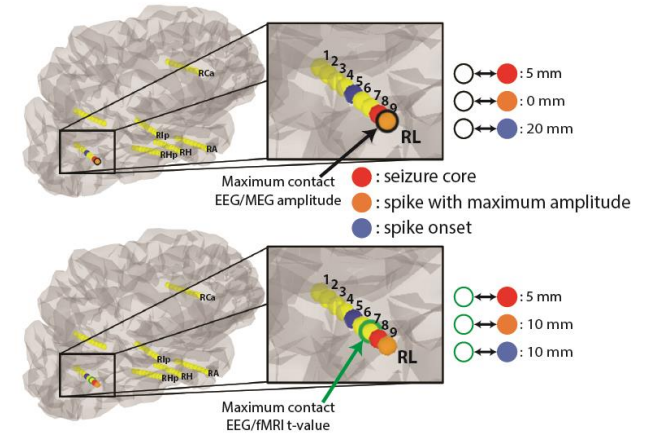
C. Projected EEG/fMRI on SEEG + SEEG references



F. SEEG seizure signal



H. Distance

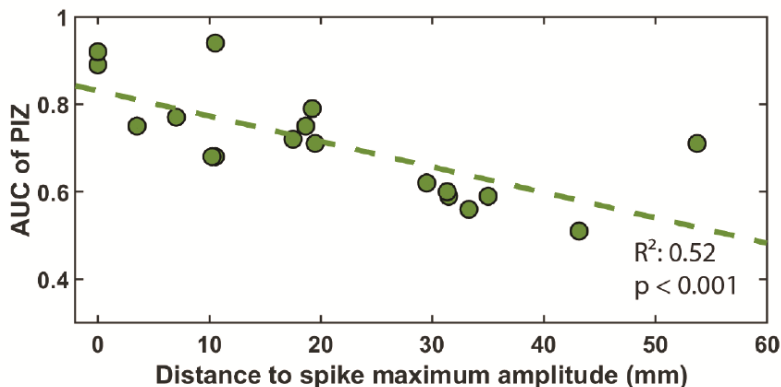


Multimodal comparison involving EEG/MEG fusion, EEG/fMRI and intracranial EEG

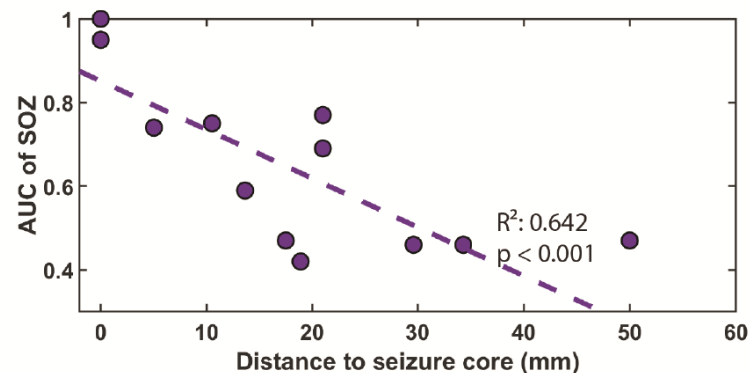


Chifaou Abdallah

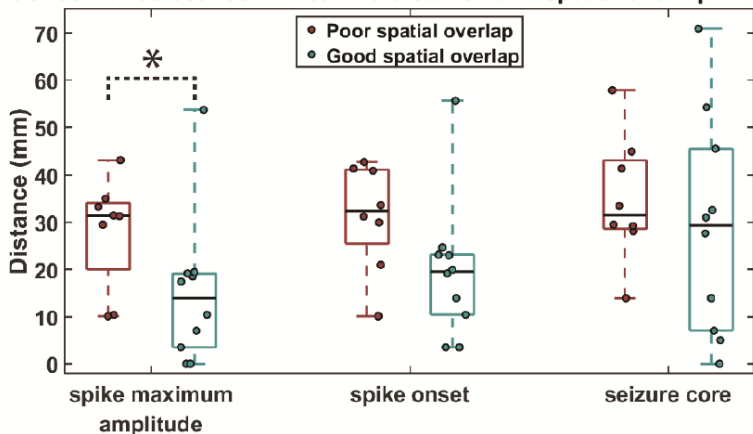
EEG/MEG source imaging vs PIZ



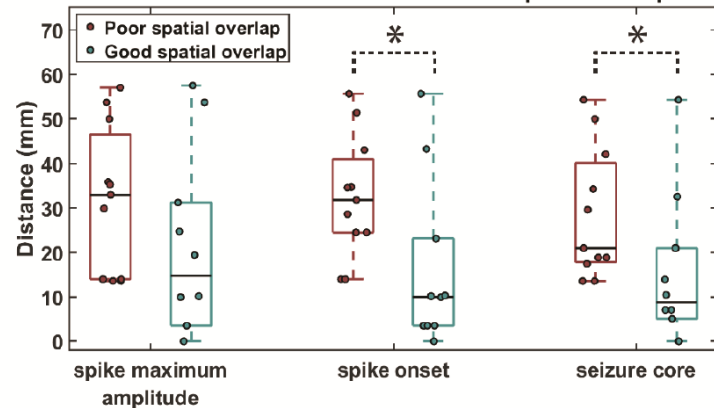
EEG/fMRI response vs SOZ



Concordance between EEG/MEG distance and spatial overlap with PIZ



Concordance between EEG/fMRI distance and spatial overlap with SOZ



Importance of considering spatial overlap in quantitative evaluation

EEG/MEG localized accurately the Primary Irritative Zone (PIZ)

whereas fMRI response to similar spikes well localized the Seizure Onset Zone (SOZ)

*EEG/MEG Source
localization using
Maximum Entropy on the
Mean (MEM)*

*Recover the spatial extent
of the source with good
accuracy*

Brainstorm

<http://neuroimage.uroc.edu/brainstorm>

MEM plugin available in
Brainstorm software

- MEM in the time domain: interesting spatial properties and the ability to recover the **spatial extent of the underlying sources**

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**Co-Developer /
Main Collaborator**

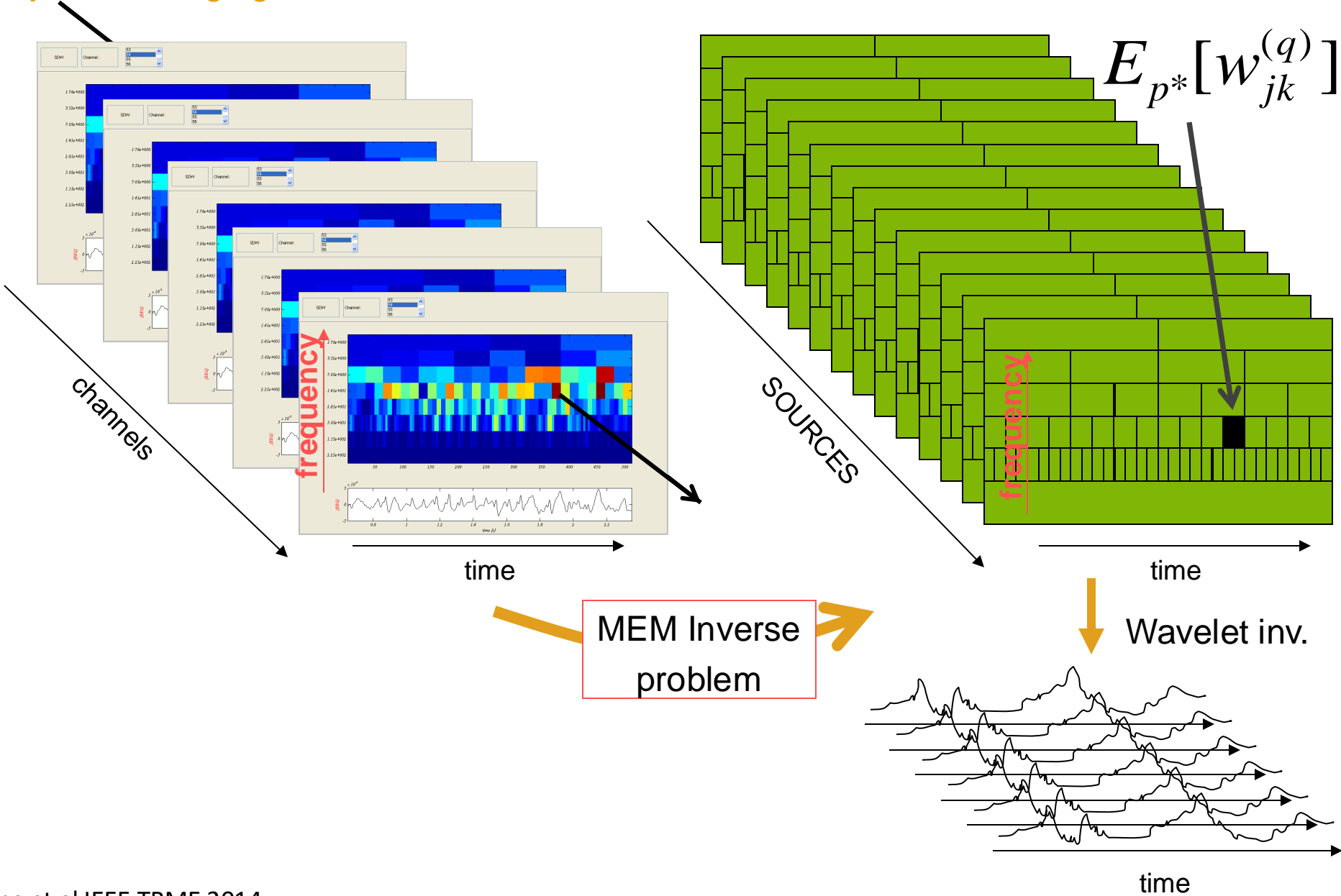
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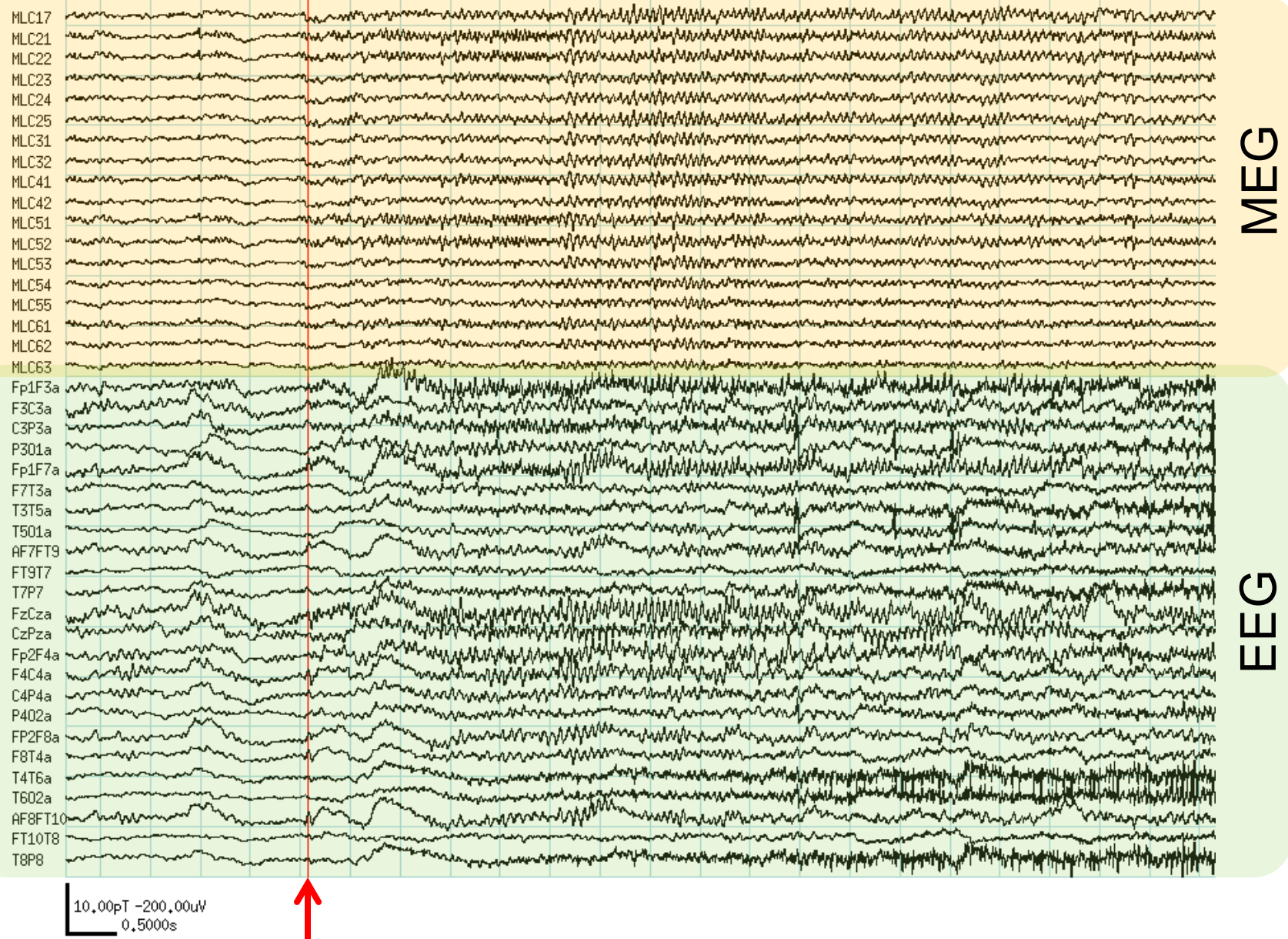
Jean-Marc Lina, PhD

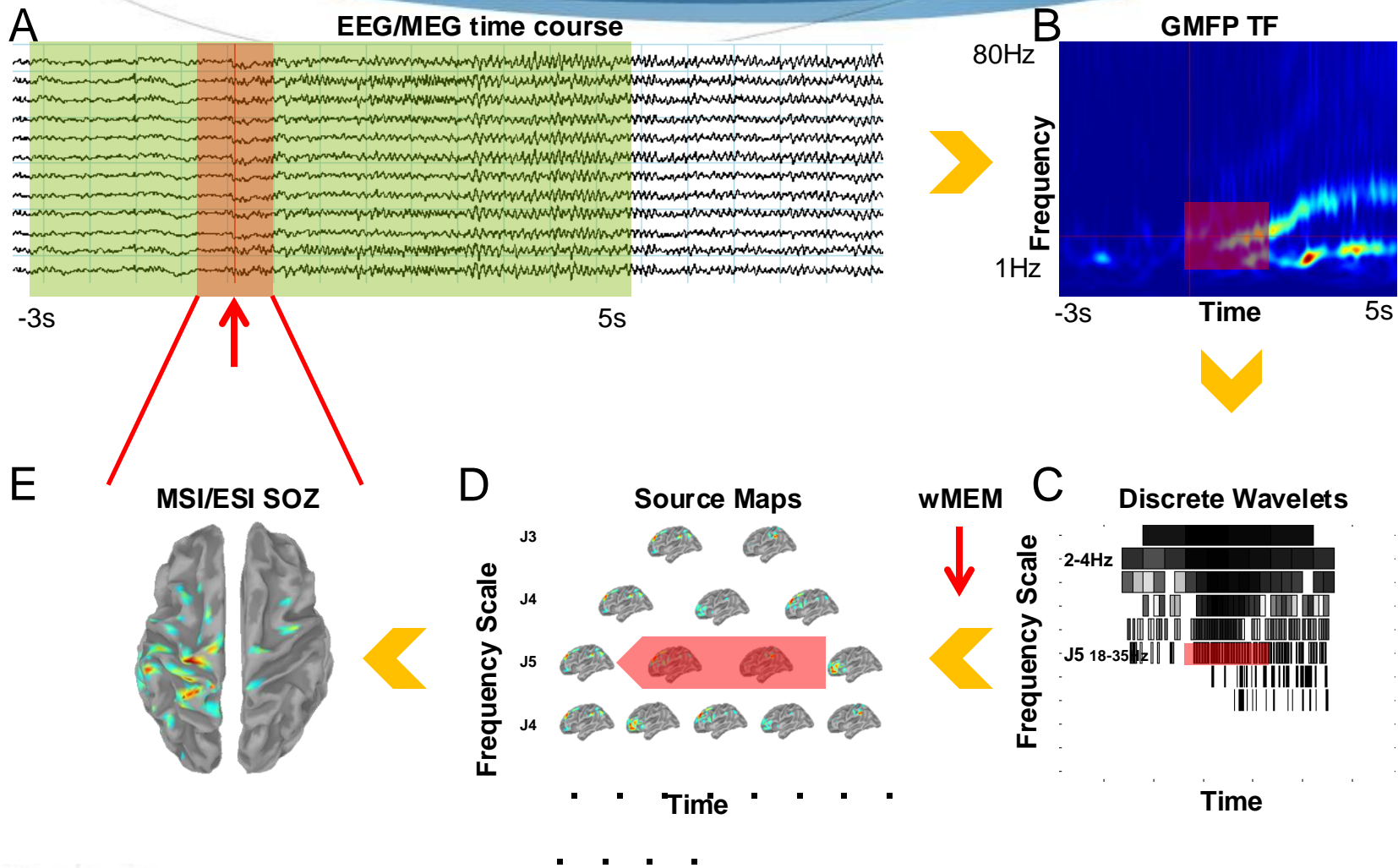
INVERSE PROBLEMS AND SPARSE (WAVELET) REPRESENTATIONS OF SIGNALS

Objective: imaging the local oscillations from MEG/EEGs

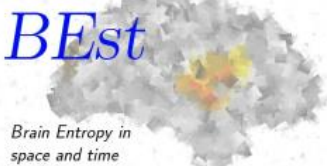


Localization of the Seizure Onset Zone (SOZ) from ictal EEG/MEG data





Wavelet-based Maximal Entropy on the Mean (wMEM): distributed inverse solution approach sensitive to the spatial extent of the epileptic generator (Lina et al., IEEE TBME 2014).



Seizure:

2

3

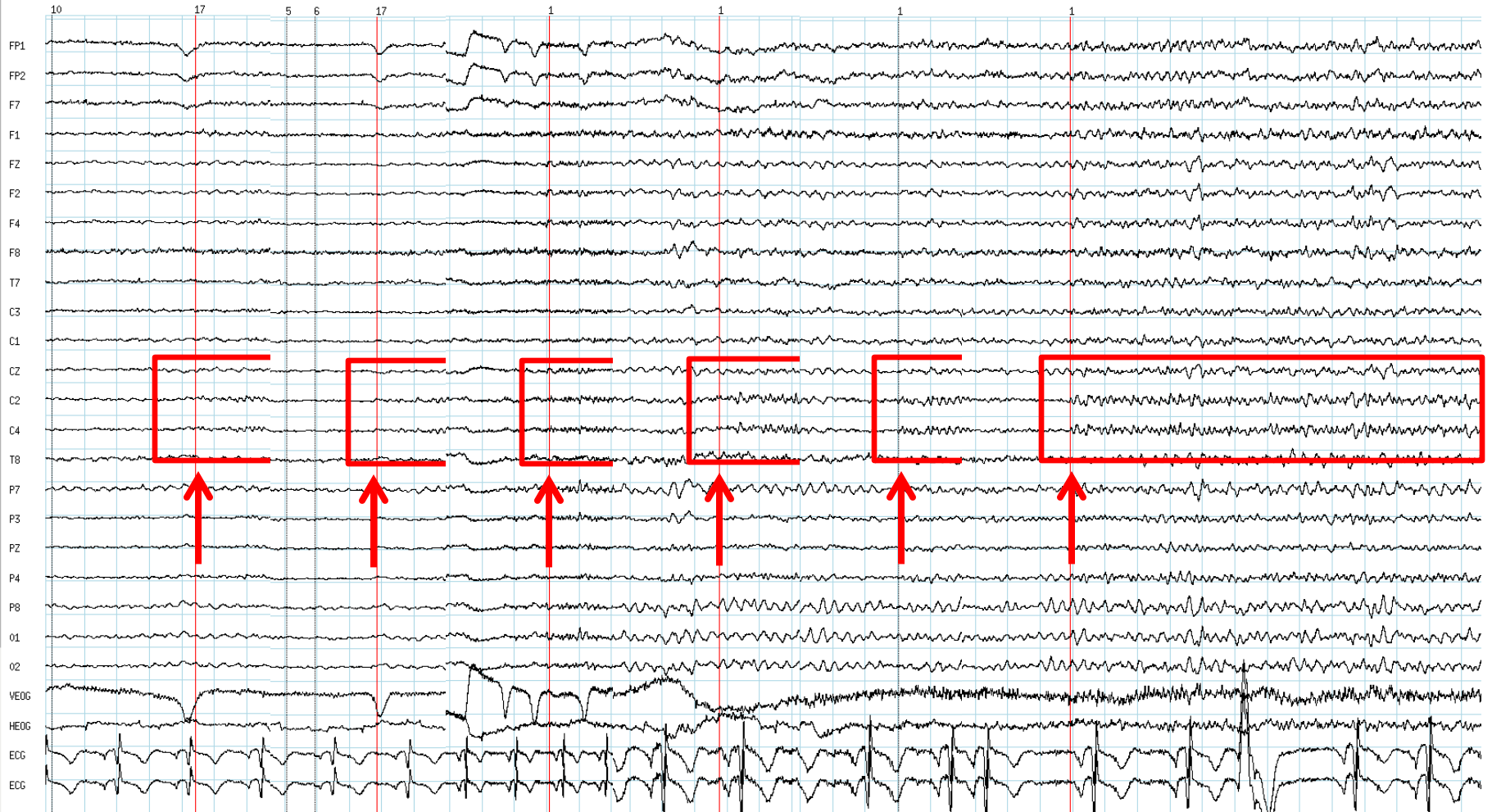
4

5

6

...

1

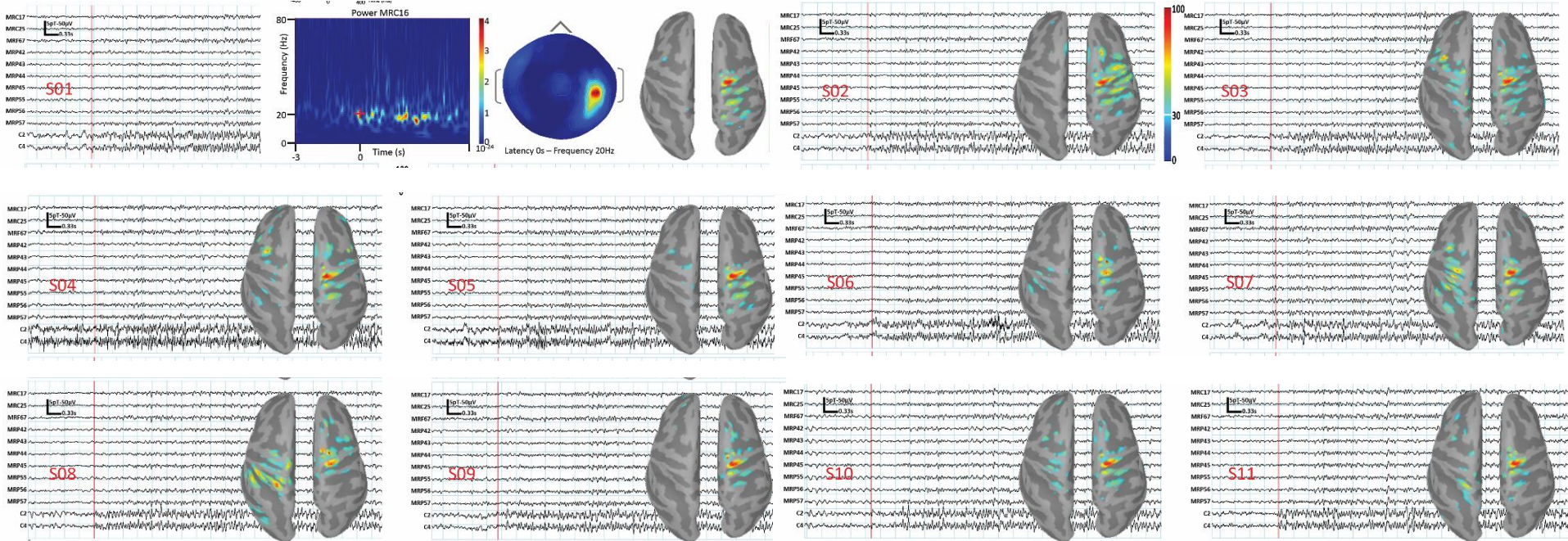
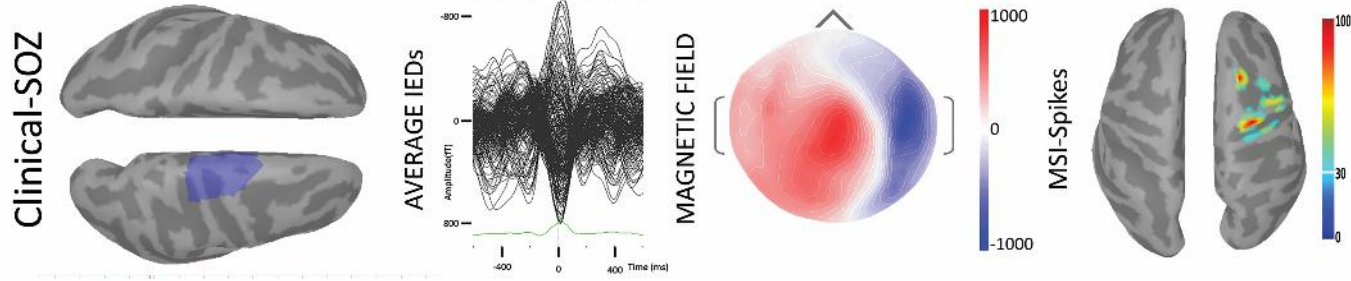


-200.00uV
0.3333s

Localization of the Seizure Onset Zone (SOZ) from ictal EEG/MEG data, using MEM



Giovanni Pellegrino



MEG/EEG Localization of the SOZ versus Clinical-SOZ



Giovanni Pellegrino

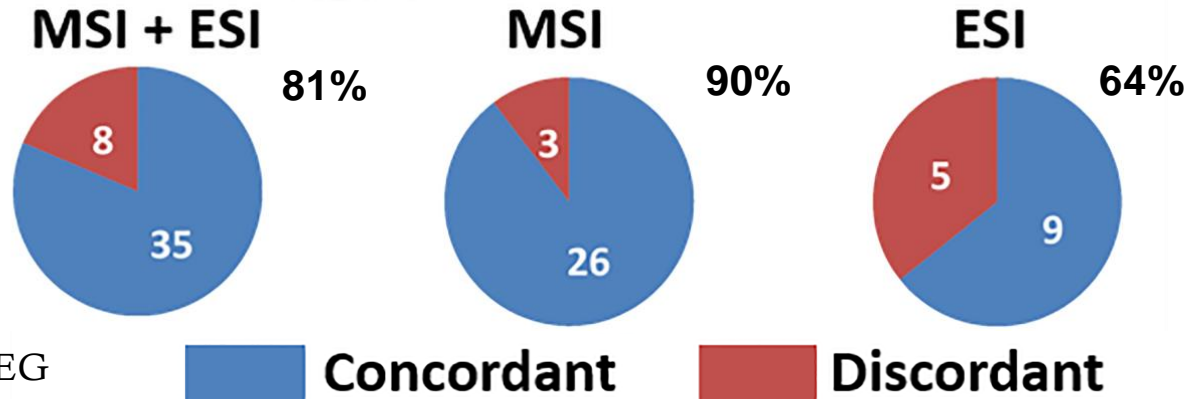
Qualitative analysis

13 Patients

31 seizures:

15 simultaneous EEG/MEG

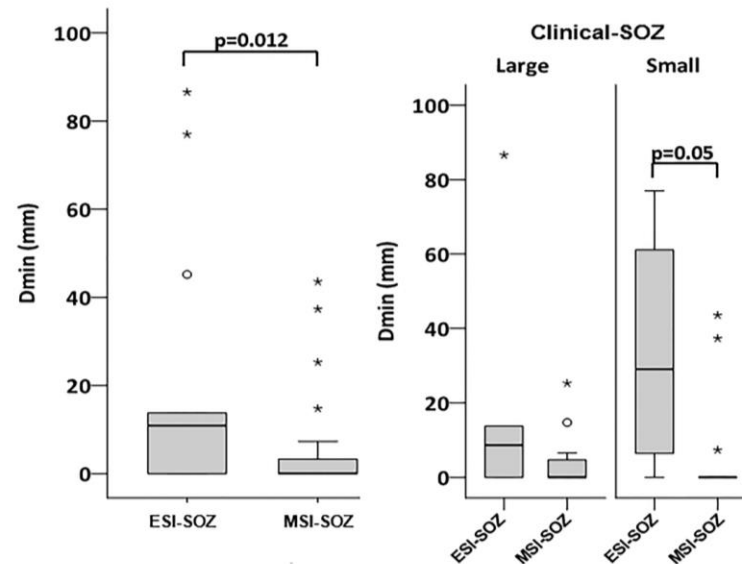
16 MEG only



Quantitative analysis

ESI: EEG Source Imaging

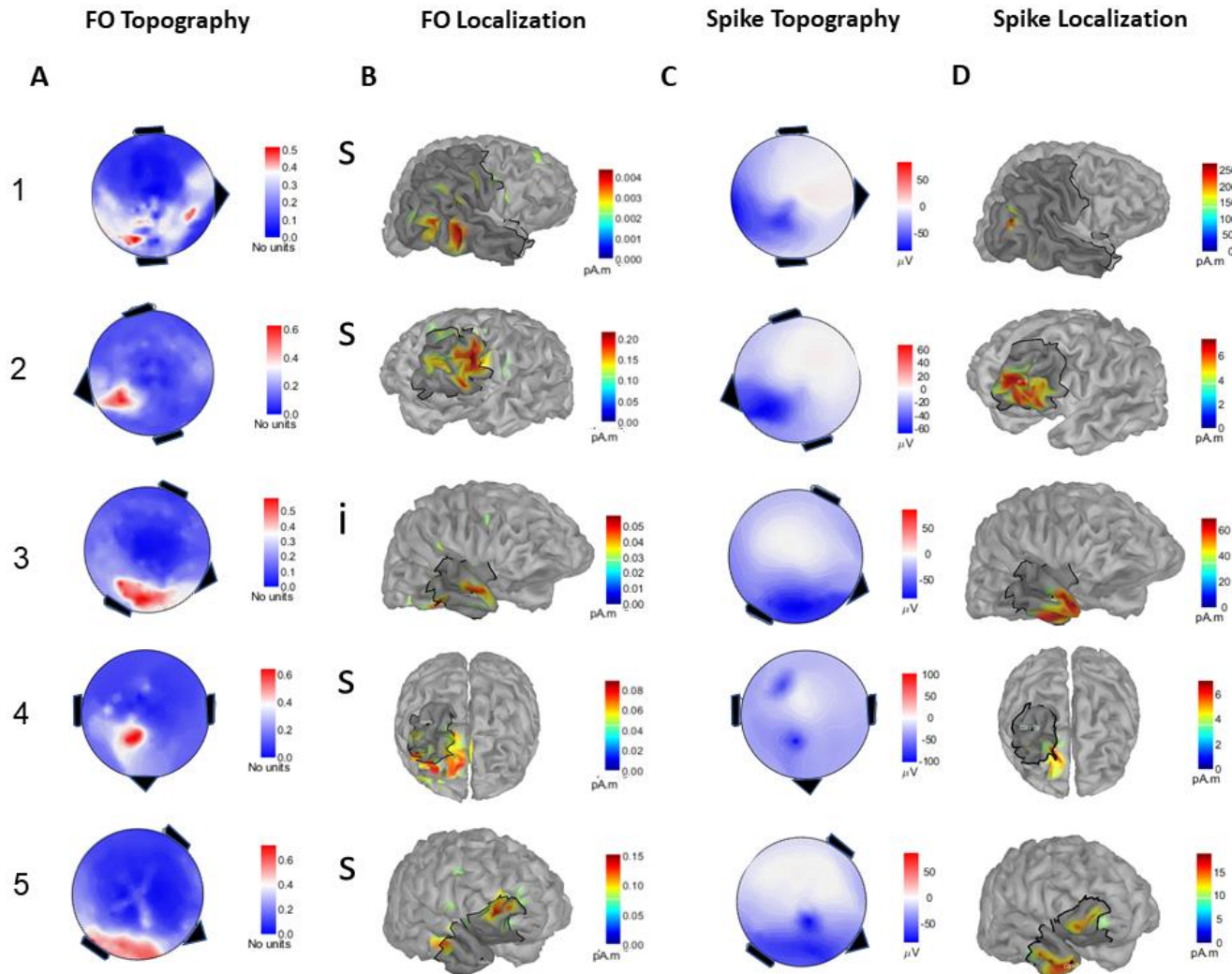
MSI: MEG Source Imaging



Localization of Fast Oscillations (FO 40-160 Hz) detected from high-density EEG



Tamir Avigdor



Birgit Frauscher

Outline

- ◆ Basic principle of source localization and imaging in EEG/MEG
- ◆ Validation of EEG/MEG source imaging with intracranial EEG
- ◆ EEG/MEG source imaging of oscillatory patterns
- ◆ EEG/MEG source imaging of deep activity
- ◆ EEG/MEG source imaging of resting state**

MEG localization of resting state oscillations

Validation with the iEEG atlas as ground truth



Jawata Afnan

1. MEG source imaging of resting state oscillatory patterns in healthy subjects to be validated at the group level with the iEEG atlas
2. Evaluate the ability of wavelet-based MEM, to localize MEG resting state oscillatory sources in different frequency bands in healthy subjects

Ground truth: the iEEG atlas of normal resting state oscillations



Birgit Frauscher

- ◆ Frauscher et al (2018) proposed the first atlas of normal iEEG data
- ◆ Pulling together iEEG data from different patients, from different epilepsy centres, in healthy regions, eyes closed, during wakefulness, dense coverage of most brain regions
- ◆ Provides unique opportunity to study the spectral characteristics of normal brain oscillatory patterns at a group level

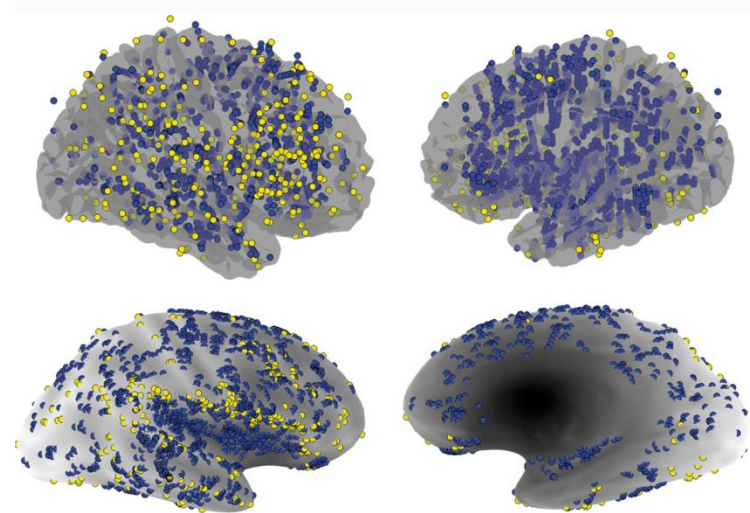
doi:10.1093/brain/awy035

BRAIN 2018; 141; 1130–1144 | 1130

BRAIN
A JOURNAL OF NEUROLOGY

Atlas of the normal intracranial electroencephalogram: neurophysiological awake activity in different cortical areas

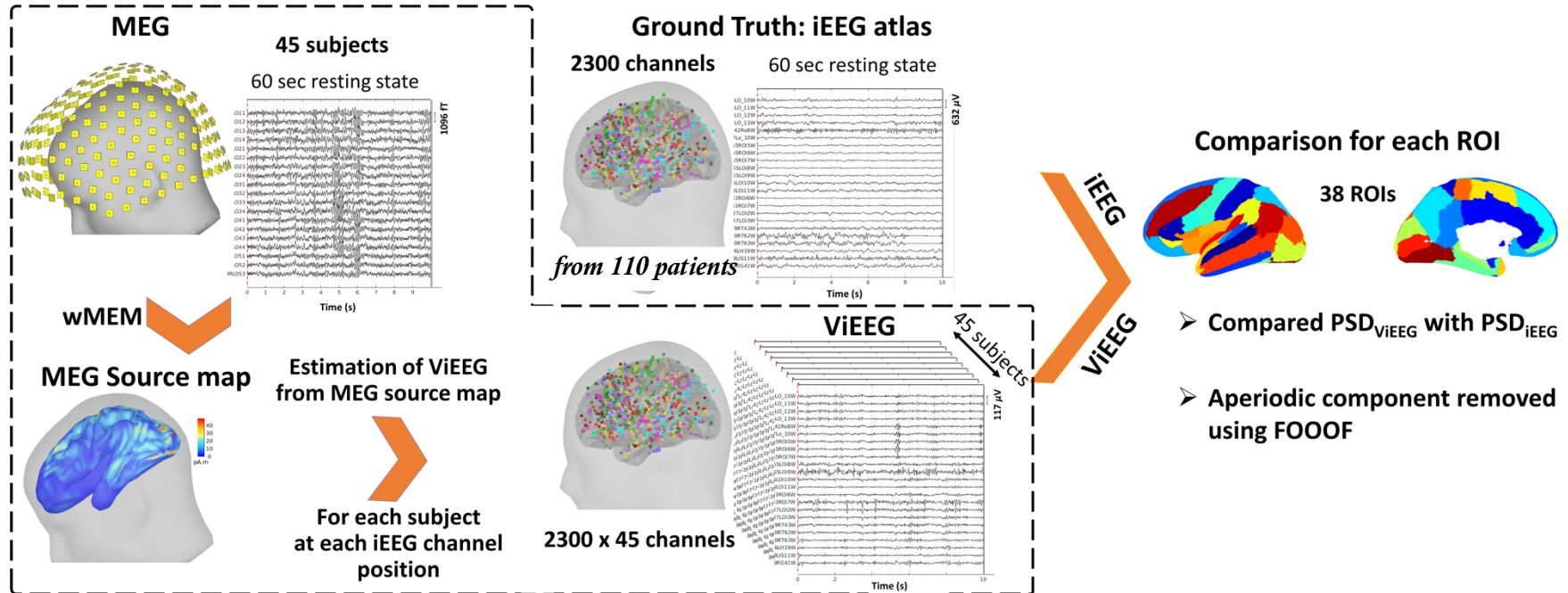
Birgit Frauscher,^{1,2} Nicolas von Ellenrieder,¹ Rina Zelman,^{1,3} Irena Doležalová,⁴ Lorella Minotti,⁵ André Olivier,¹ Jeffery Hall,¹ Dominique Hoffmann,⁵ Dang Khoa Nguyen,⁶ Philippe Kahane,⁵ François Dubeau¹ and Jean Gotman¹



MEG localization of resting state oscillations Validation with the iEEG atlas as ground truth



Jawata Afnan

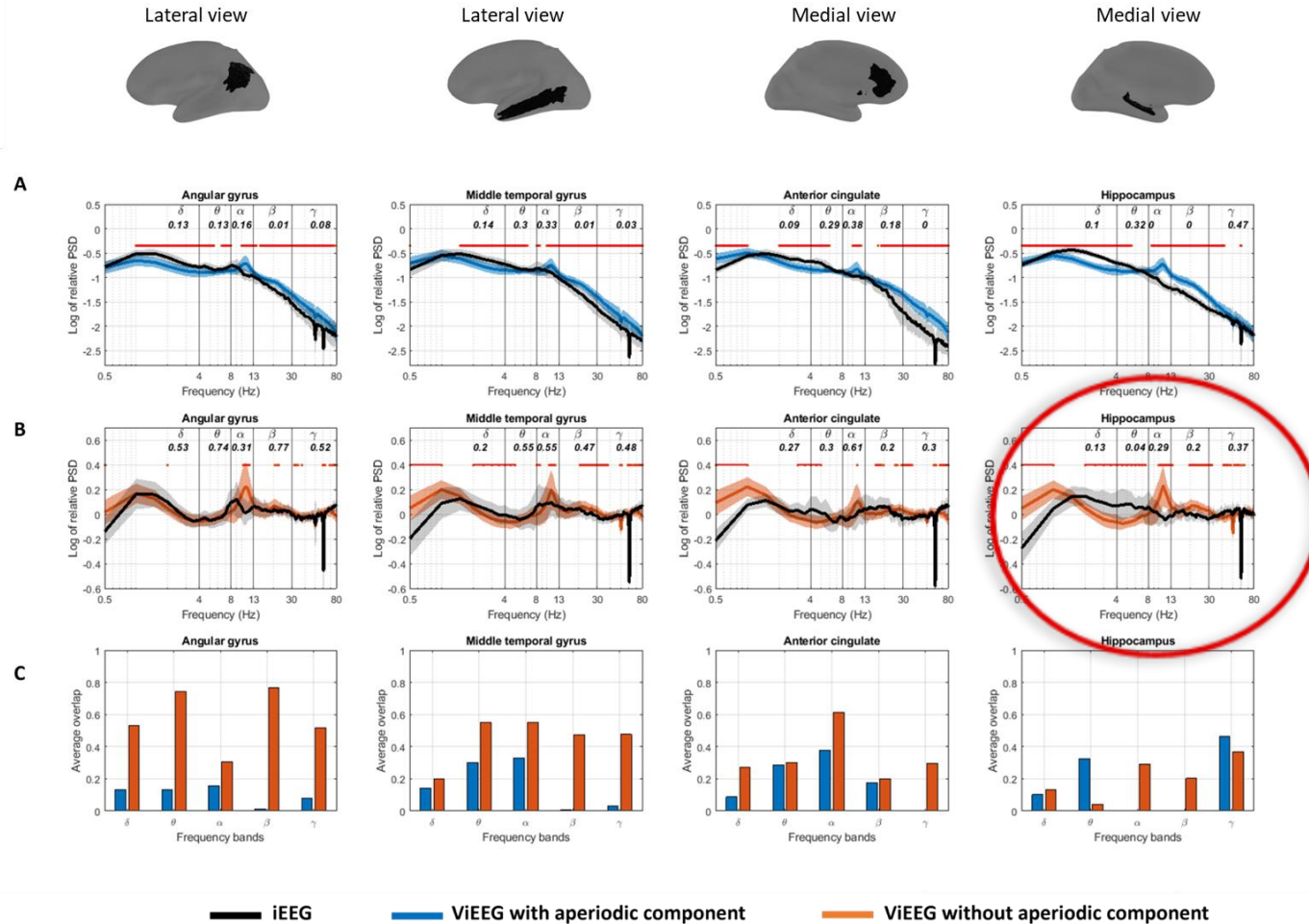


MEG localization of resting state oscillations Validation with the iEEG atlas as ground truth



Jawata Afnan

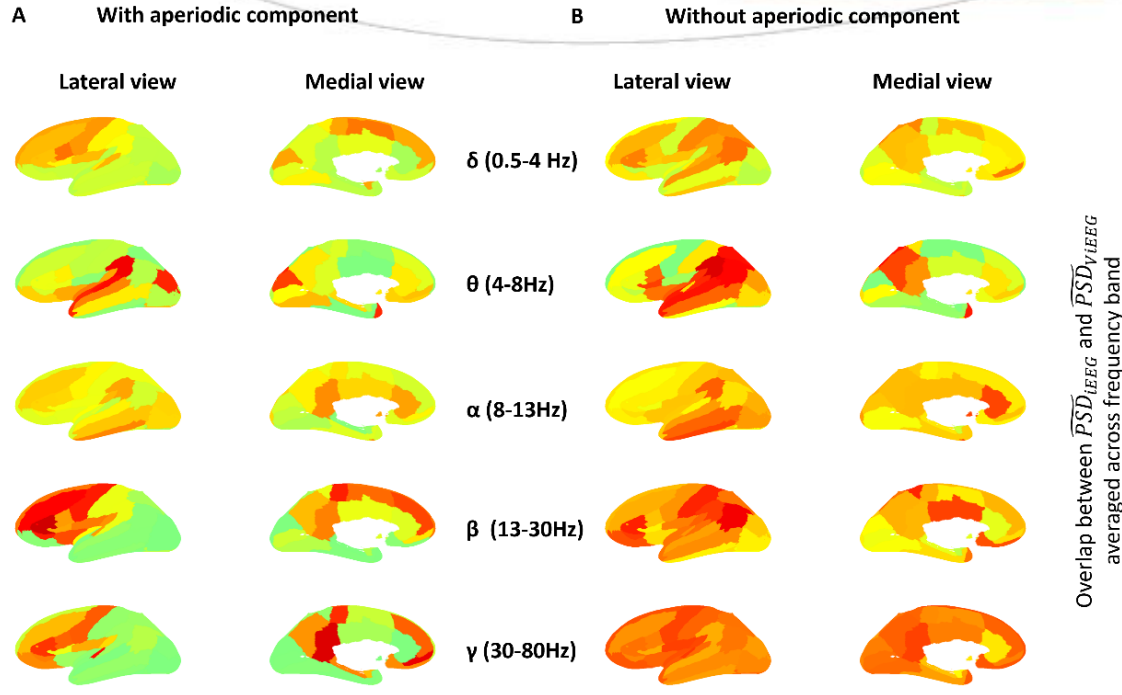
Comparison of MEG estimated spectra using wMEM with ground truth iEEG: selected ROIs



MEG localization of resting state oscillations Validation with the iEEG atlas as ground truth



Jawata Afnan



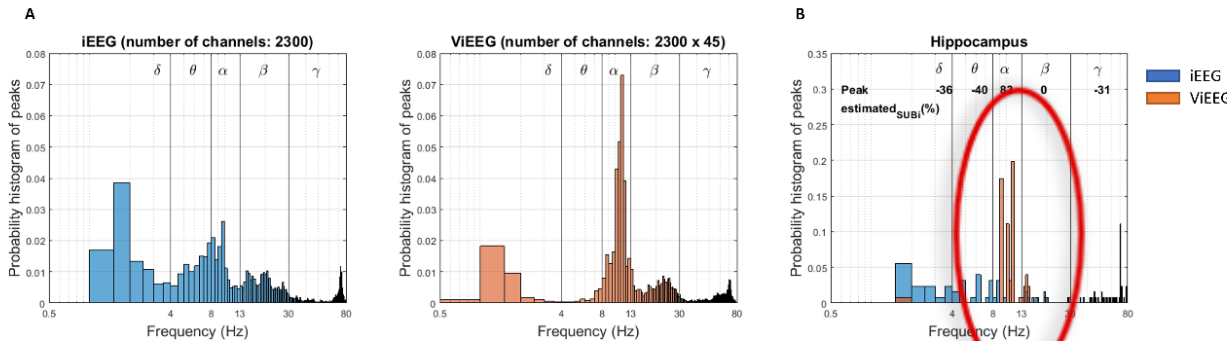
Overall we retrieved accurate MEG resting state oscillations in most cortical regions in different frequency bands

Results were more comparable with the iEEG atlas after removing aperiodic components

Localization in deeper structures was biased by source leakage, cf. widespread large alpha peak

Comparison of oscillatory peaks identified in MEG estimated spectra with MNI

iEEG atlas



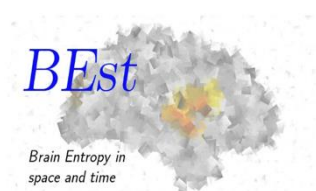
Similar findings when considering wMEM, MNE and Beamformer

Take home messages

- ◆ Several hypotheses associated with each localization method
- ◆ From *dipole fitting* (requires excellent knowledge / expertise in electrophysiology) to *source imaging* (less parameters to tune, but be careful when interpreting)
- ◆ All methods are useful, some might be wrong, always assess compatibility with scalp topography, be aware of the methods' assumption when interpreting the data
- ◆ Comparison between localization methods is always a plus
- ◆ Complementarity between MEG and high-density EEG source imaging
- ◆ Localizing deep activity remains challenging, even more during resting state
- ◆ Estimation of the spatial extent: our plugin using *Maximum Entropy on the Mean* is available in Brainstorm software



MEM is available as a Brainstorm Toolbox



Brainstorm BEst Tutorial

<http://neuroimage.usc.edu/brainstorm/Tutorials/TutBEst>

MEG_SEEG_Chifa

- MEG-RF-spikes EEG+MEG_Cluster_2_80spikes_avg-70_to_50
- MEG-RF-spikes EEG+MEG_Cluster_3_41spikes_avg-70_to_50
- MEG-RF-spikes EEG+MEG_Cluster_1_14spikes_avg-70_to_50
- MEG-RF-spikes EEG+MEG_Cluster_2_31spikes_avg-70_to_50
- MEG-RF-spikes EEG+MEG_Cluster_3_14spikes_avg-70_to_50
- MEG-RF-spikes EEG+MEG_Cluster_1_33spikes_avg-70_to_50
- MEG-RF-spikes EEG+MEG_Cluster_2_54spikes_avg-70_to_50
- MEG-RF-spikes EEG+MEG_Cluster_3_17spikes_avg-70_to_50
- EEG-RF-spikes_fusion EEG+MEG_Cluster_1_63spikes_avg-50_to_30
- EEG-RF-spikes_fusion EEG+MEG_Cluster_2_56spikes_avg-50_to_30
- > Avg: EEG-RF-spikes_for_fusion(119)
- > Avg: EEG-RF-spikes (184)
 - cMEM: : EEG(Full) | timewindow: -0.1 to 0.1s | smooth=0.6 2018
 - cMEM: : MEG(Full) | timewindow: -0.1 to 0.1s | smooth=0.6 2018_02
- > Avg: MEG-RF-spikes (215)
- > Avg: MEG-RF-spikes (163)
- baseline (#1)
 - MEG-RF-spikes - _new Consensus map - Cluster number : 1 is compos
 - MEG-RF-spikes - _new Consensus map - Cluster number : 2 is compos
 - MEG-RF-spikes - _new Consensus map - Cluster number : 3 is compos
 - MEG-RF-spikes - _new Consensus map - Cluster number :
 - MEG-RF-spikes - _new Consensus map - Cluster number :
 - MEG-RF-spikes - _new Consensus map - Cluster number :
 - MEG-RF-spikes - _new Consensus map - Cluster number :
 - MEG-RF-spikes - _new Consensus map - Cluster number :
 - MEG-RF-spikes - _new Consensus map - Cluster number :

Time: [-1000.0, 1000.0] ms
Sampling: 300 Hz 601 samples

<<< < > >>>

Record Filter Surface Scout +

Surface options

Transp.: 0%
Smooth: 43%

Color Sulci Edge

Data options

Amplitude: 0%
Min size: 1
Transp.: 0%

Reset [X,Y,Z]

Left Right Struct Reset

Vertices: 8002 Faces: 15993

Compute sources

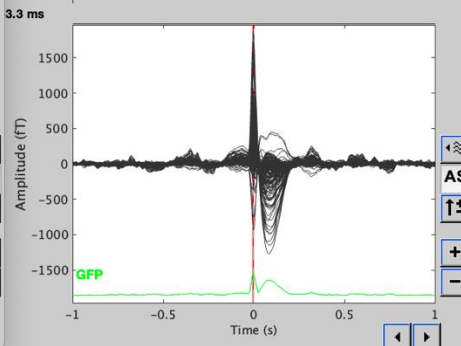
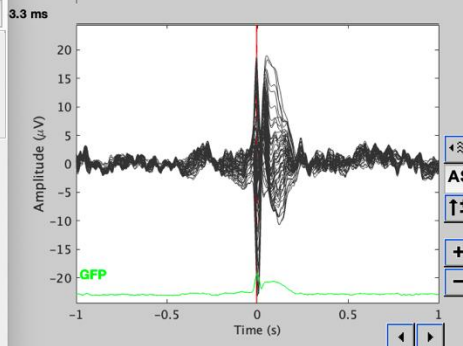
Comment: MEM: : MEG

- Method
- Minimum norm imaging
 - LCMV beamformer
 - Dipole modeling
 - MEM: Max entropy on the mean

MEM
Requires the BrainEntropy plugin.
Options defined in a separate panel.

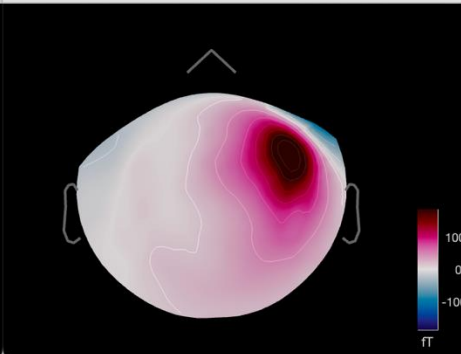
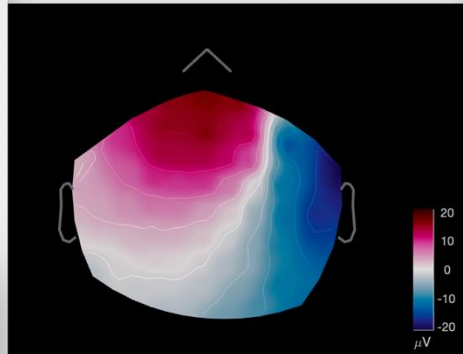
Sensors
 MEG EEG

Hide details Cancel OK



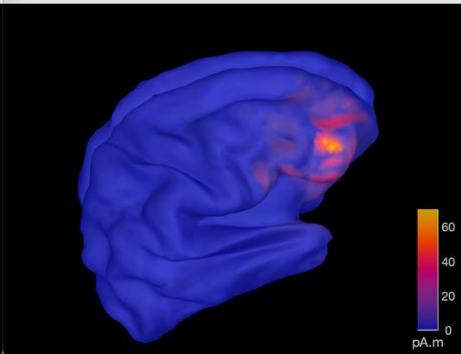
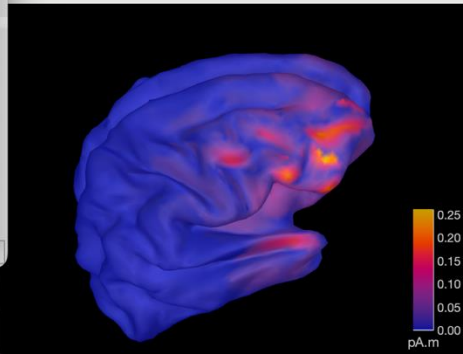
EEG/TP: PA65-P/PA65_EPI-ekobayashi_2...

MEG/TP: PA65-P/PA65_EPI-ekobayashi_2...



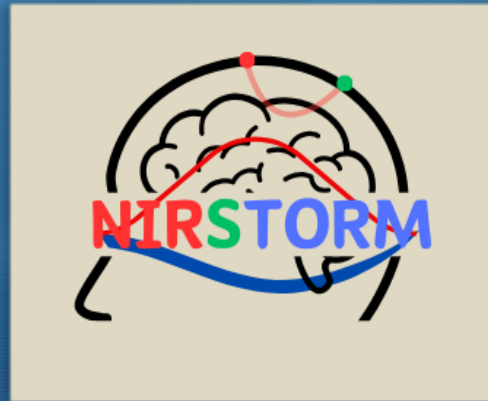
EEG/3D: PA65-P/PA65_EPI-ekobayashi_2...

MEG/3D: PA65-P/PA65_EPI-ekobayashi_2...



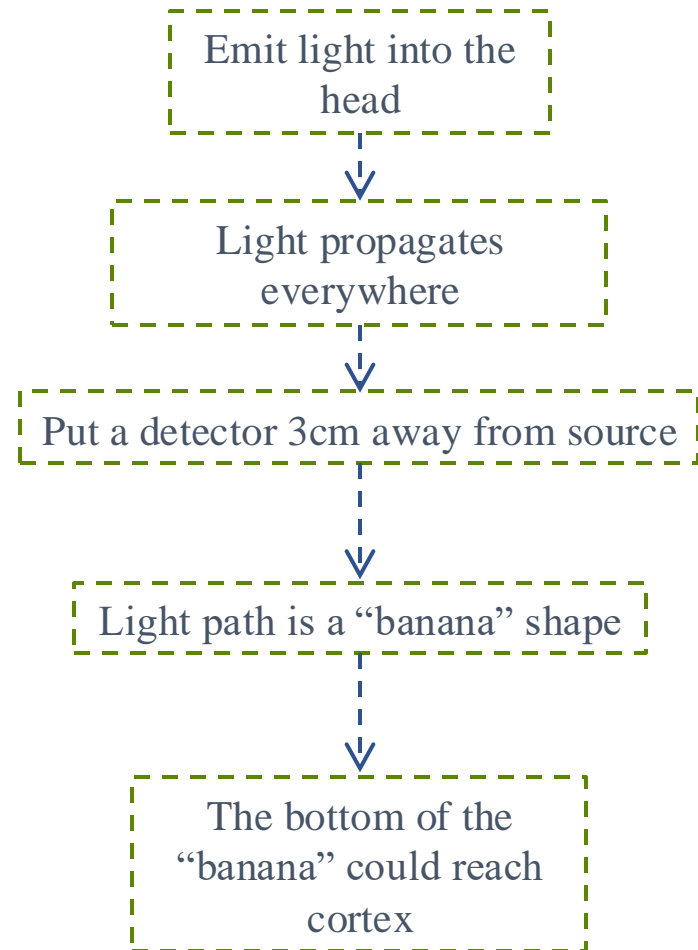
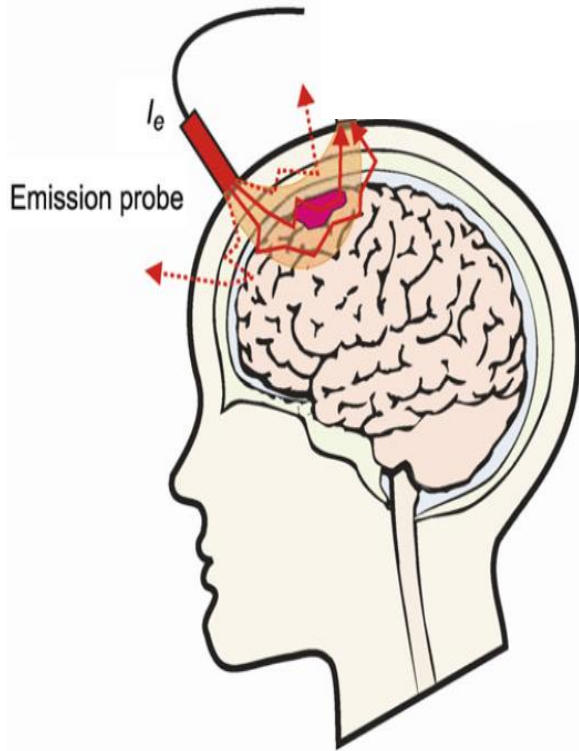
Files to process: Data [0]

Part 2: NIRSTORM analysis of fNIRS data from optimal probe design to 3D reconstruction



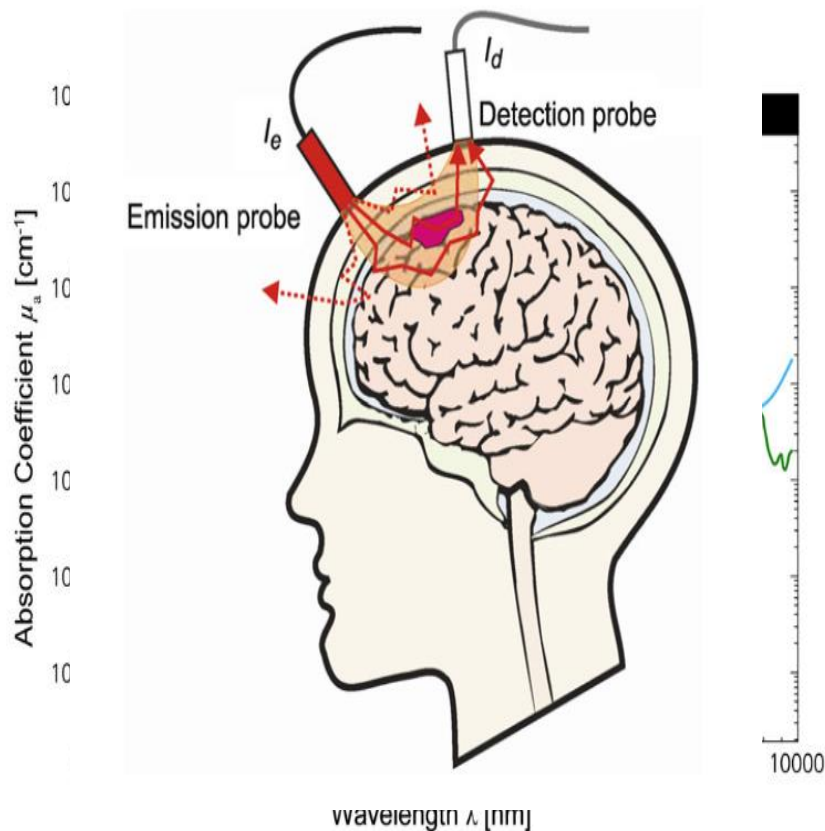
What is functional Near Infra-Red Spectroscopy (fNIRS)?

- fNIRS measures non-invasively fluctuations of both oxygenated and deoxygenated hemoglobin (HbO and HbR) in the brain with high temporal resolution
- How does it work?



What is functional Near Infra-Red Spectroscopy (fNIRS)?

- fNIRS measures non-invasively fluctuations of both oxygenated hemoglobin (HbO) and deoxygenated hemoglobin (HbR) in the brain with high temporal resolution
- How does it work?



Hemoglobin absorbs the light

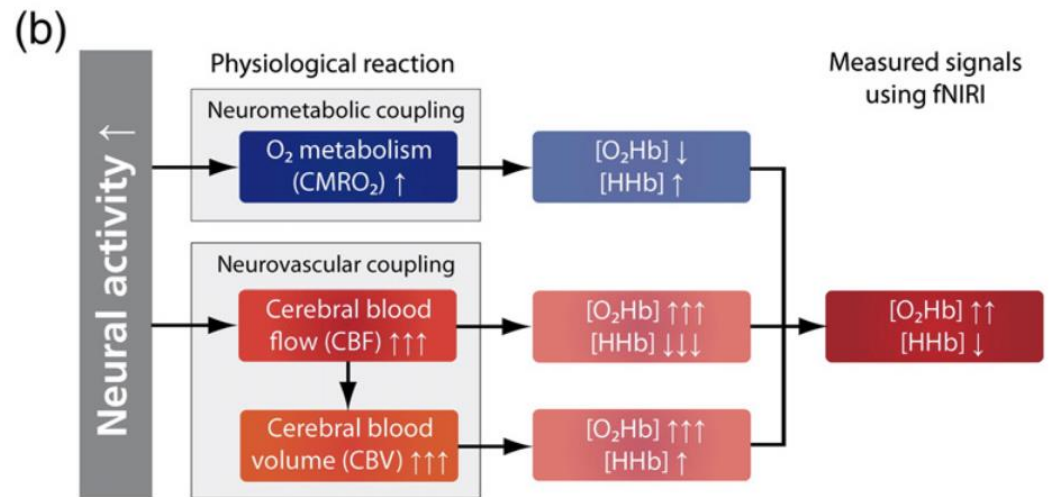
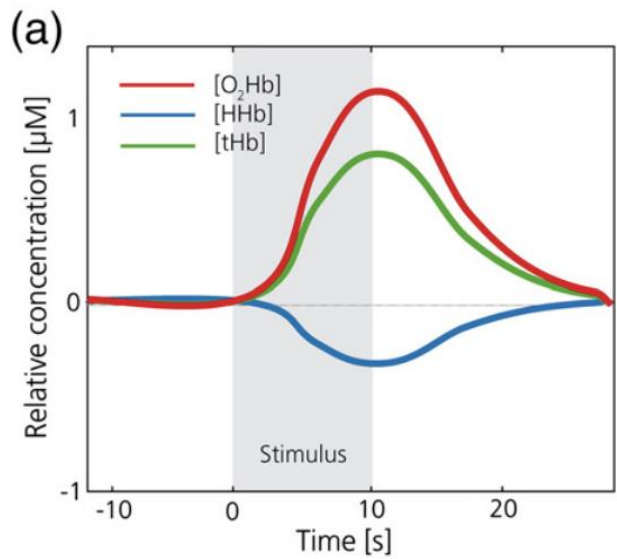
If hemoglobin concentration changes

Light intensity will change

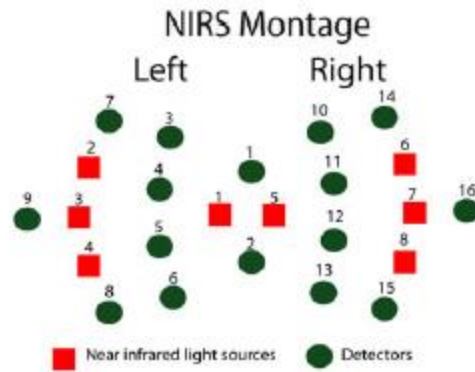
HbO/HbR at least 2 wavelengths

2 equations
modified Beer-Lambert law
with 2 unknowns
problem solved

Origins of fNIRS signals



Finger opposition task in fMRI and NIRS

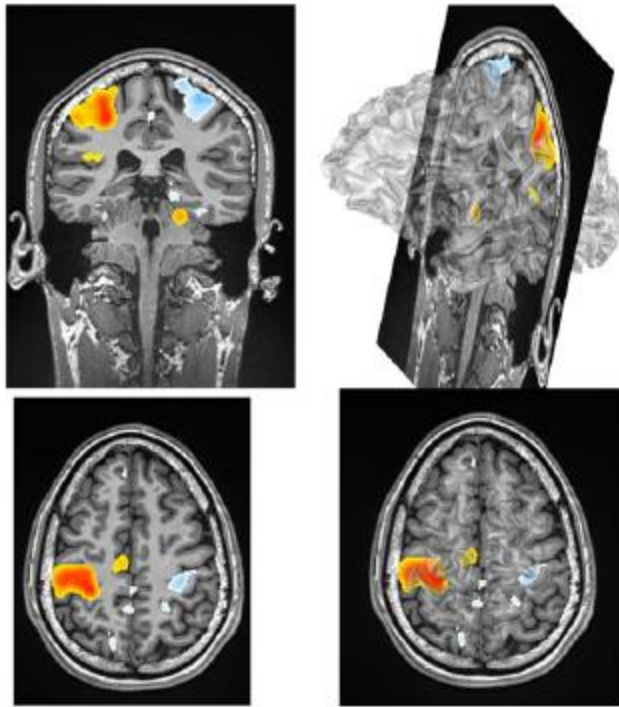


(i) NIRS montage using 8 sources at 690 nm, 8 sources at 830 nm (red squares) and 16 detectors (green circles)

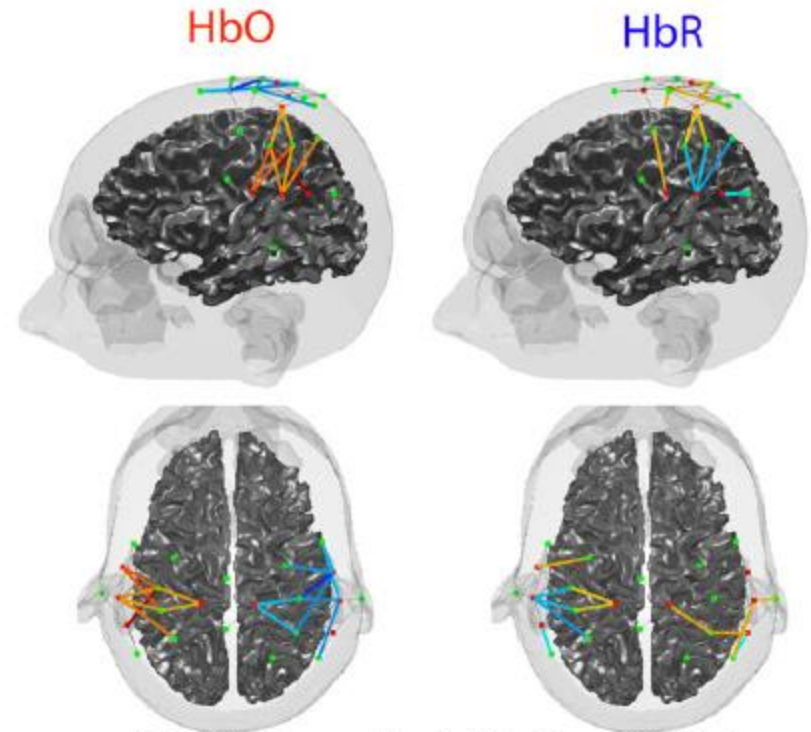


(ii) Installation of Brainsight fibers equipped with low profile prisms on the EEG/NIRS cap

Finger opposition task in fMRI and NIRS

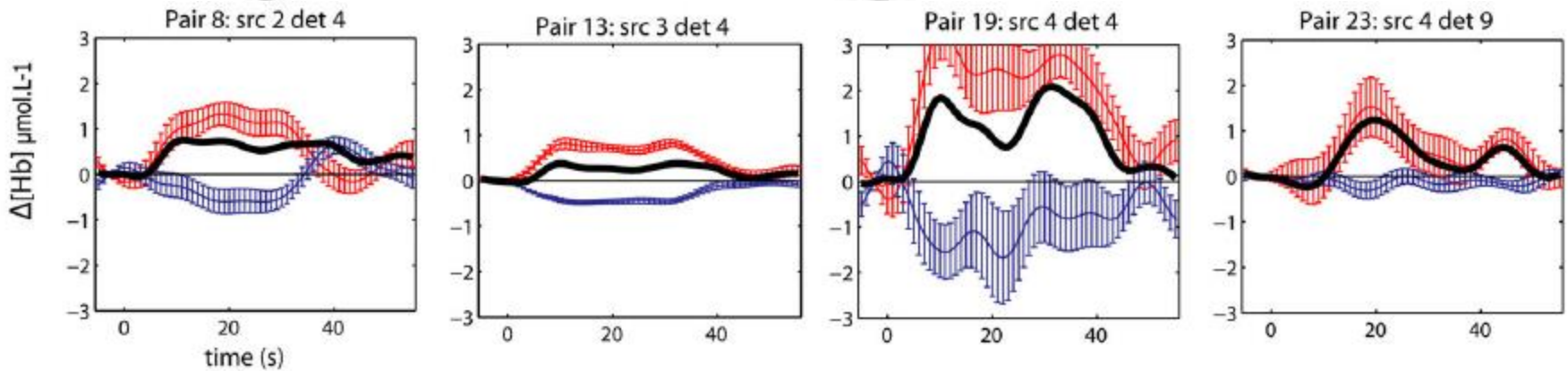


(iii) BOLD response: t-map superimposed on anatomical MRI (cortical surface in transparency)

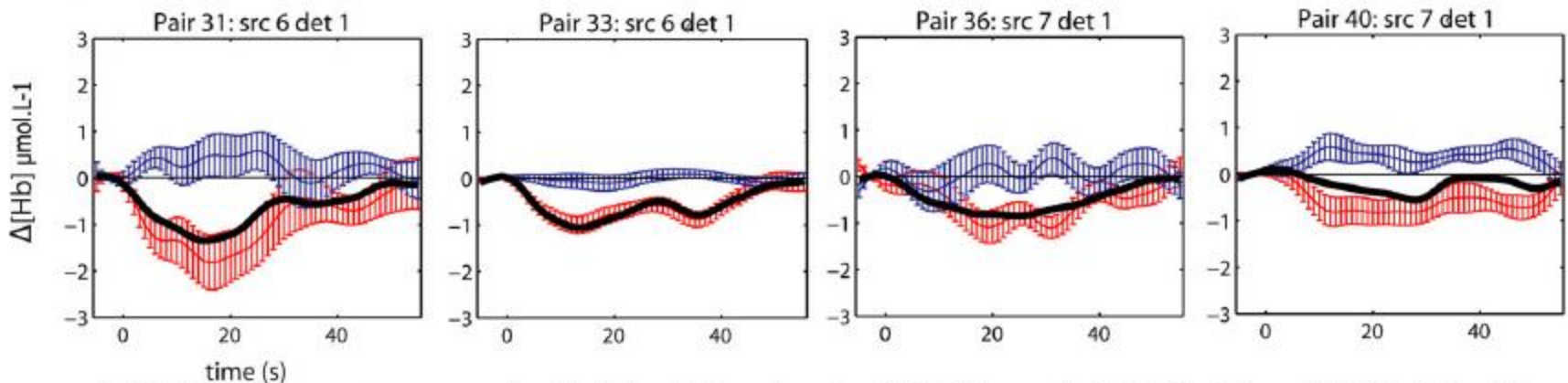


(iv) NIRS results in HbO and HbR over the cortical surface of the subject. For each channel: t-values in color

Finger opposition task in fMRI and NIRS



(v) NIRS response on selected contralateral pairs (HbO in red, HbR in blue, HbT in black)



(vi) NIRS response on selected ipsilateral pairs (HbO in red, HbR in blue, HbT in black)

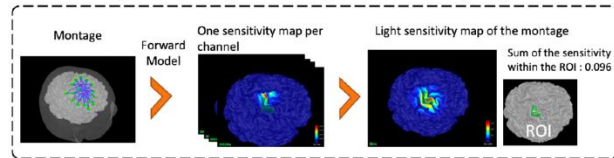
NIRSTORM: a Brainstorm extension dedicated to functional Near Infrared Spectroscopy (fNIRS) data analysis, advanced 3D reconstructions, and optimal probe design



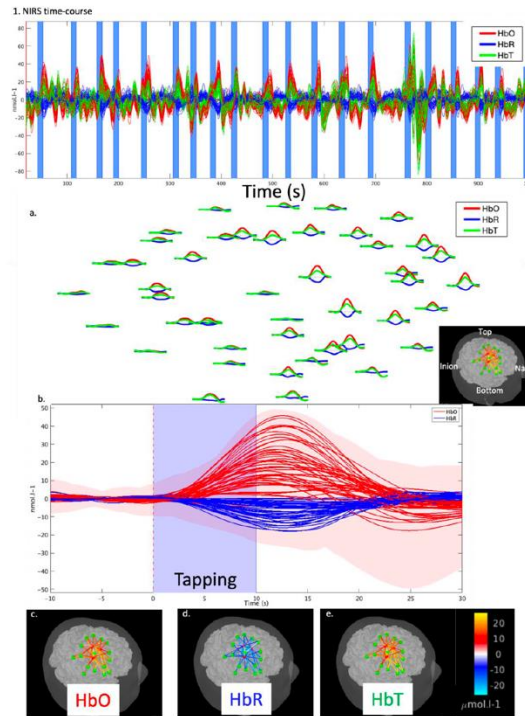
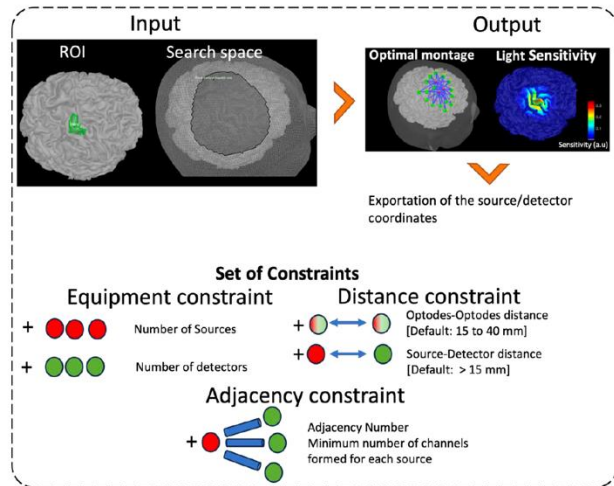
Édouard Delaire, Thomas Vincent, Zhengchen Cai, Alexis Machado, Laurent Hugueville, Denis Schwartz, Francois Tadel, Raymundo Cassani, Louis Bherer, Jean-Marc Lina, Mélanie Pélégriani-Issac, Christophe Grova

doi: <https://doi.org/10.1101/2024.09.05.611463>

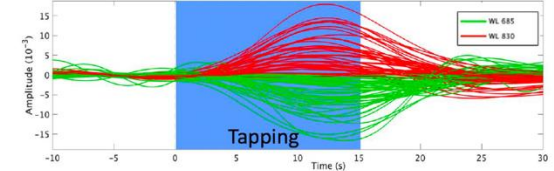
A. Sensitivity of a montage to the region of interest (ROI)



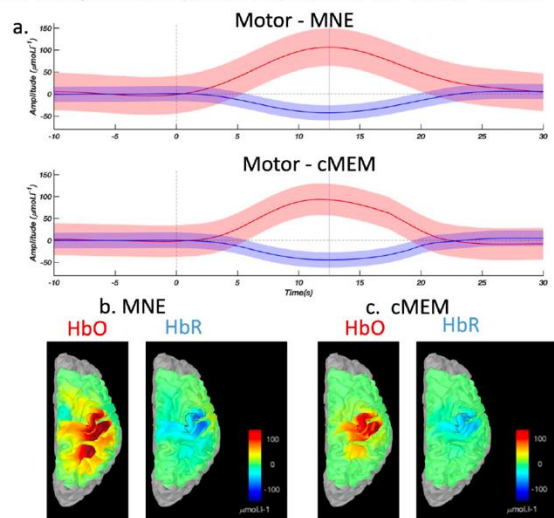
B. Optimization of the montage to maximize the sensitivity to the ROI



1. Averaged optical density response at the sensors levels



2. Averaged hemodynamic response on the cortical surface

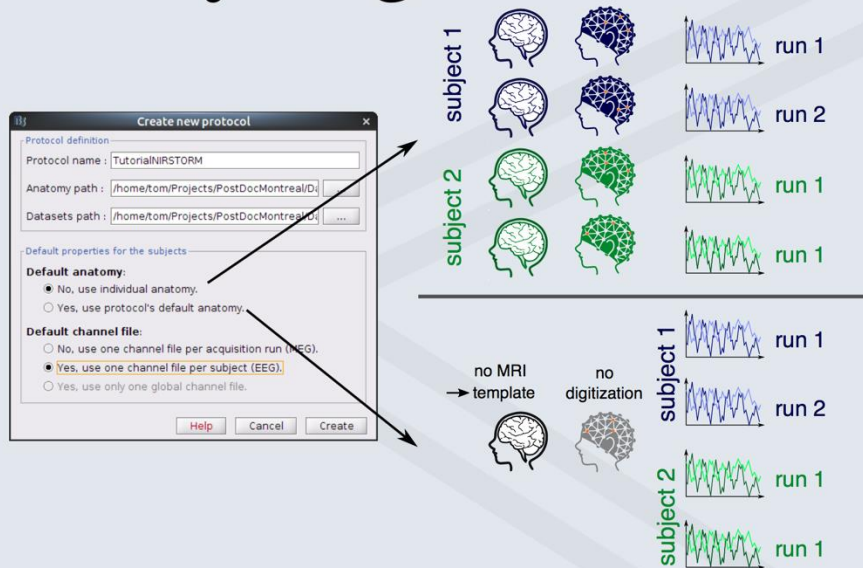


NIRSTORM

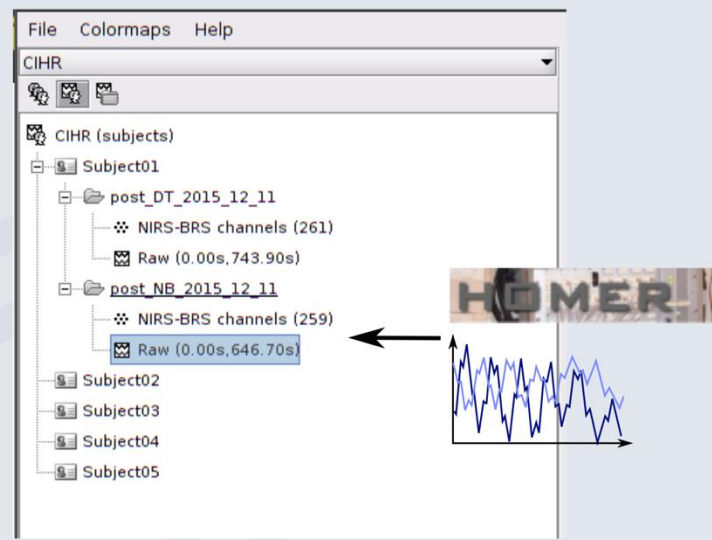


1. fNIRS standard sensor level analysis

Study Organization



NIRS import



Input Data format:

.nirs as in Homer

.snirf file

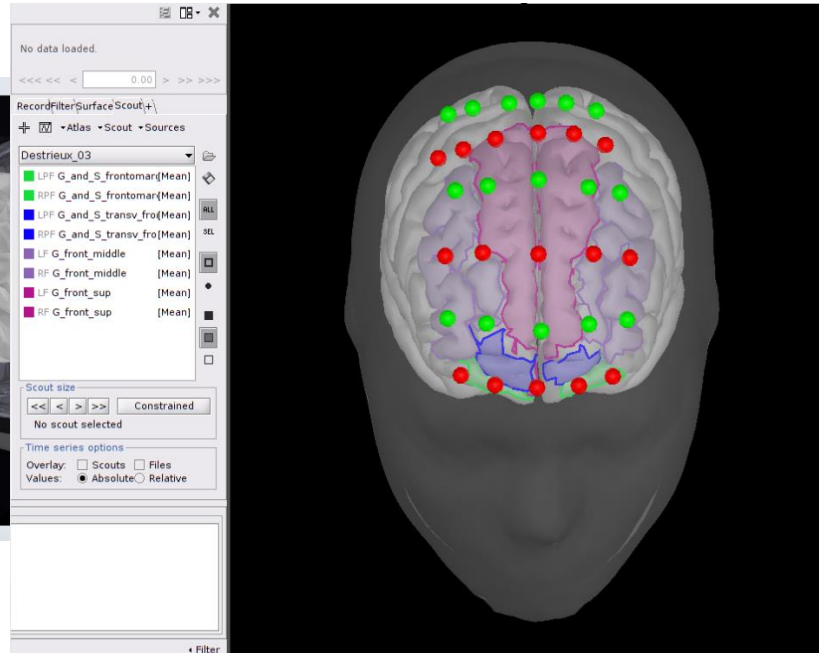
...

Standard NIRS data analysis in the sensor space

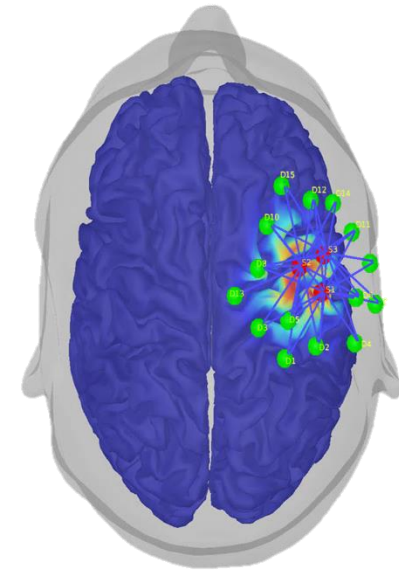
Visualization features

Anatomical Model

subject specific or Template



Overlay on anatomical atlases



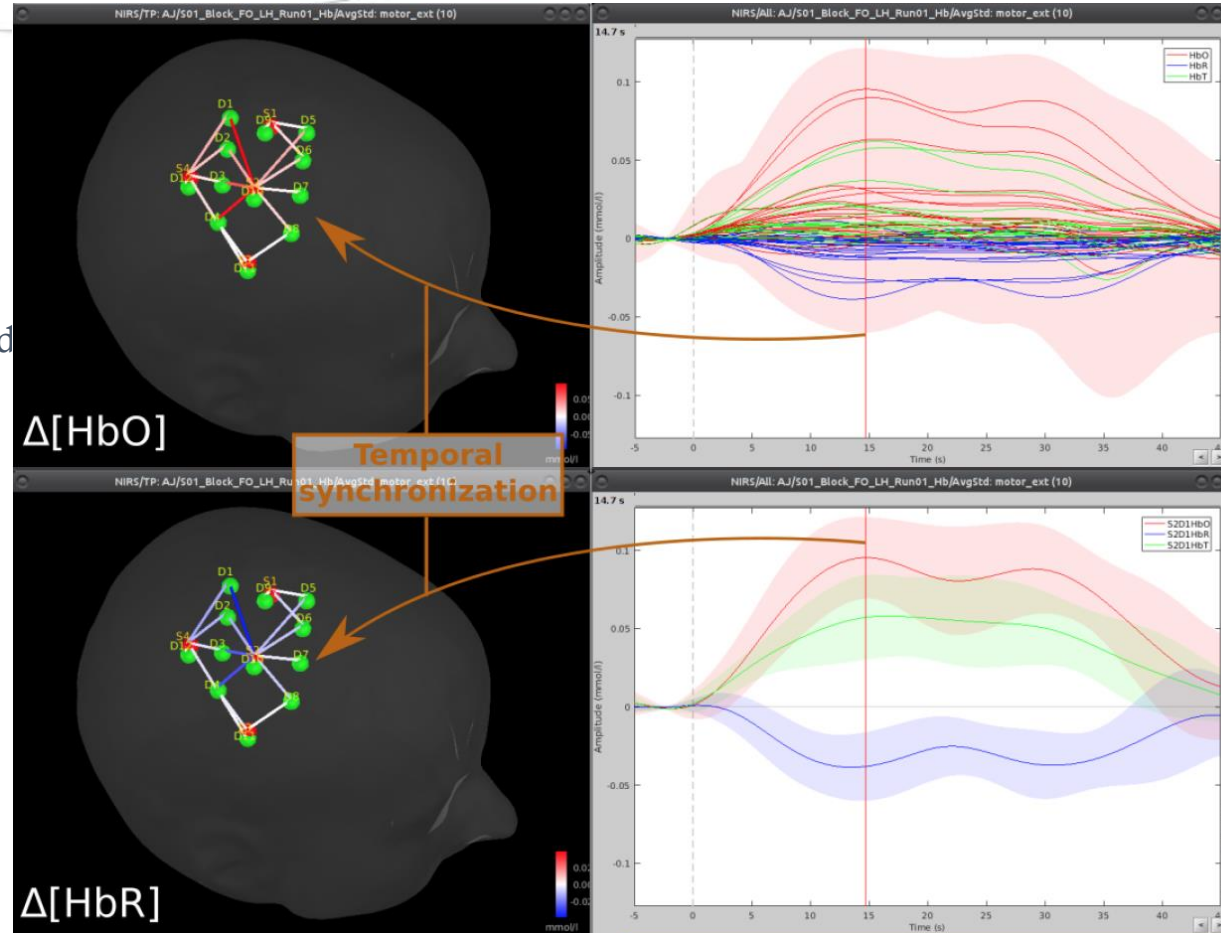
Optimal fNIRS
montage
targeting the right
hand knob

Standard fNIRS data analysis in the sensor space

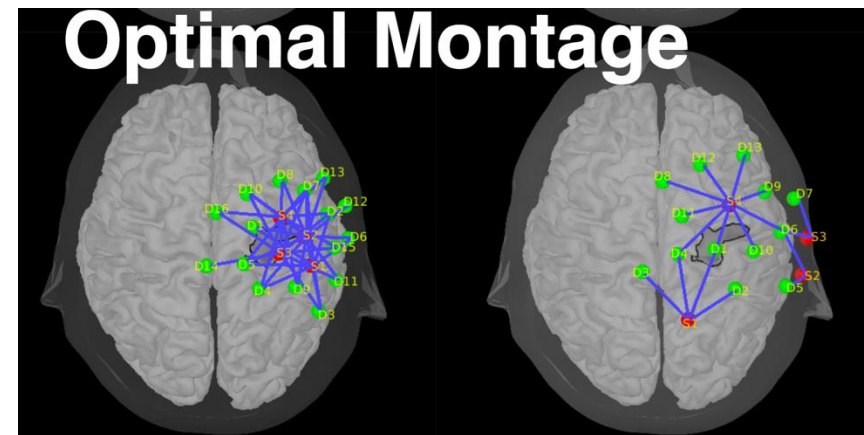
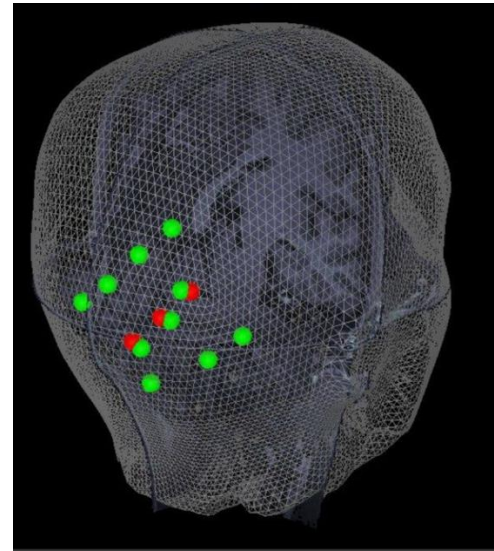
Typical preprocessing pipeline

1. Importing data and trigger exploration, verification, removal of bad channels
2. Motion Detection / Correction
3. Conversion in HbO/HbR Modified Beer Lambert Law
4. Band Pass Filtering (0.005-0.08Hz), short distance channel regression
5. Signal averaging and interaction with the data

Taking benefit from Brainstorm EEG/MEG developments: filtering, PCA, ICA, SSP, Wavelets, connectivity measures ...



Personalized fNIRS: Optimal Montage Design



Optimal Montage Design: motivations

- No standard procedures: Many different probe designs proposed

Velcro patches



Elastic nets

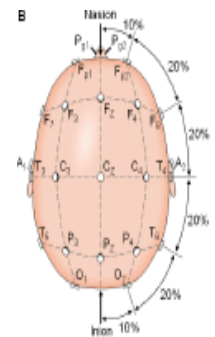


Semi rigid



- Difficulty to assess the cortical area being illuminated
- Difficult to maintain optode contact for long periods
- Difficulty to integrate montages with an EEG positioning system

EEG 10-20
international
system

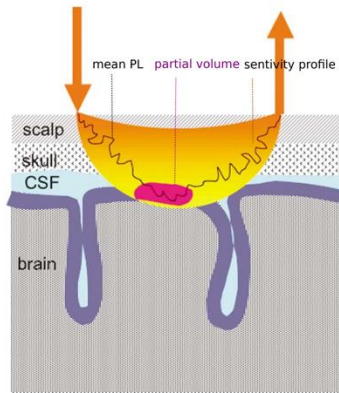


Development of personalized “Optimal NIRS montages”



Alexis
Machado

Light sensitivity profile



$\Delta[\text{HbO}]$ interpolation on the scalp



➤ How to ensure that the target area is well illuminated ?

Methodology to find the best optode positions over target brain regions

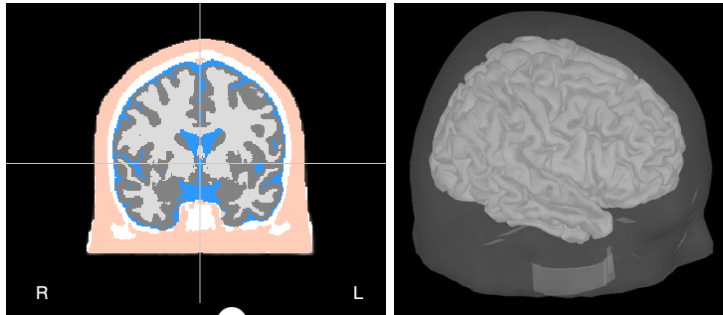
Machado et al. 2014, Journal of Biomedical Optics

Machado et al, 2018, JNS – Methods

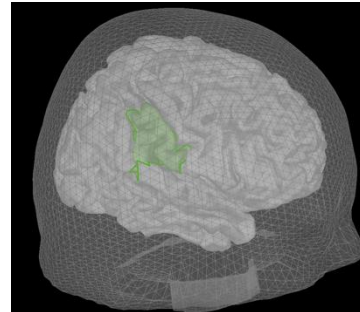
Development of personalized “Optimal fNIRS montages”

Anatomical Information

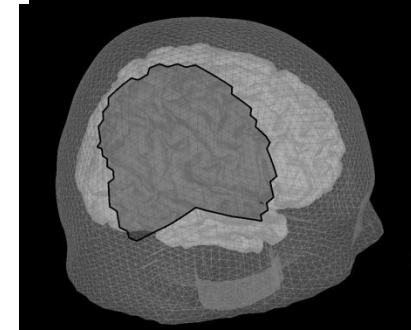
Head model for light propagation modeling



Region of Interest To target



Optodes possible locations on the skin (search space)





Definition of the constraints to search for an Optimal Montage

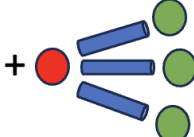
Equipment constraint

- +  Number of Sources
- +  Number of detectors

Distance constraint

- +  Optodes-Optodes distance
[Default: 15 to 40 mm]
- +  Source-Detector distance
[Default: > 15 mm]

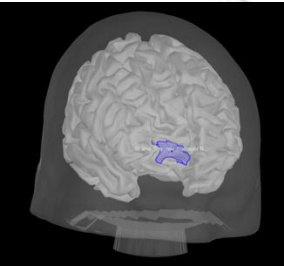
Adjacency constraint

- +  Adjacency Number
Minimum number of channels
formed for each source

Machado et al. 2014, Journal of Biomedical Optics

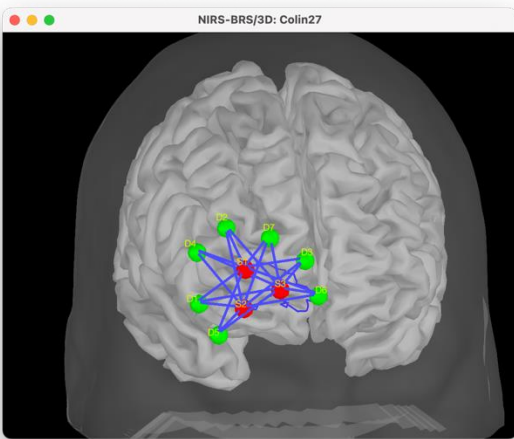
Machado et al, 2018, JNS – Methods

Development of personalized “Optimal fNIRS montages”

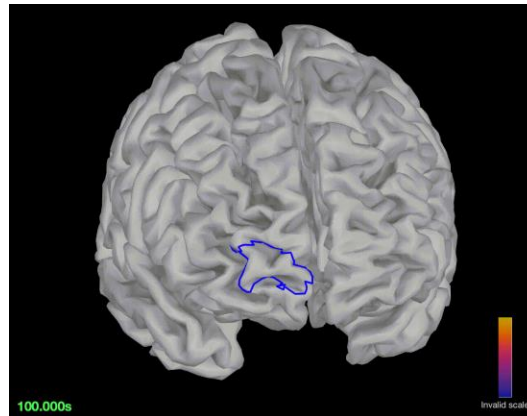


Targeted right
Fronto polar region

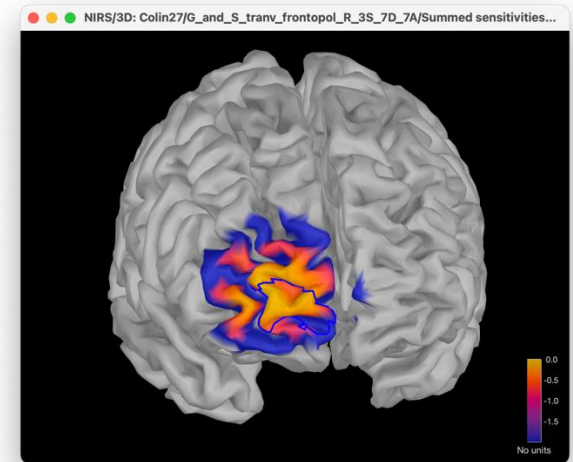
fNIRS montage



Light sensitivity map



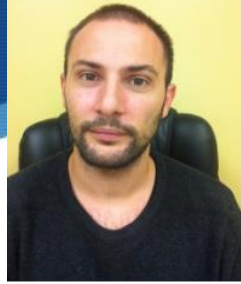
Summed Light sensitivity map



Machado et al. 2014, Journal of Biomedical Optics

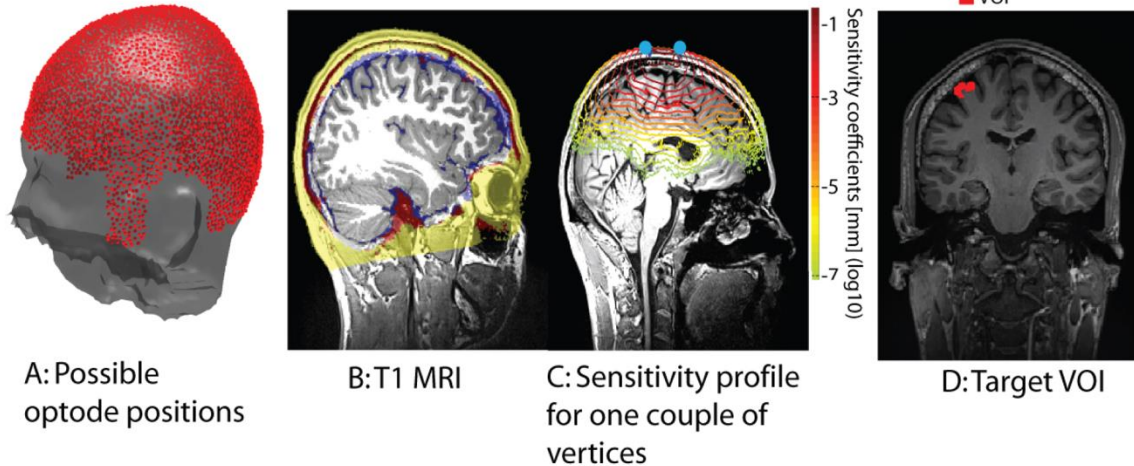
Machado et al, 2018, JNS – Methods

Personalized NIRS using “Optimal NIRS montages”



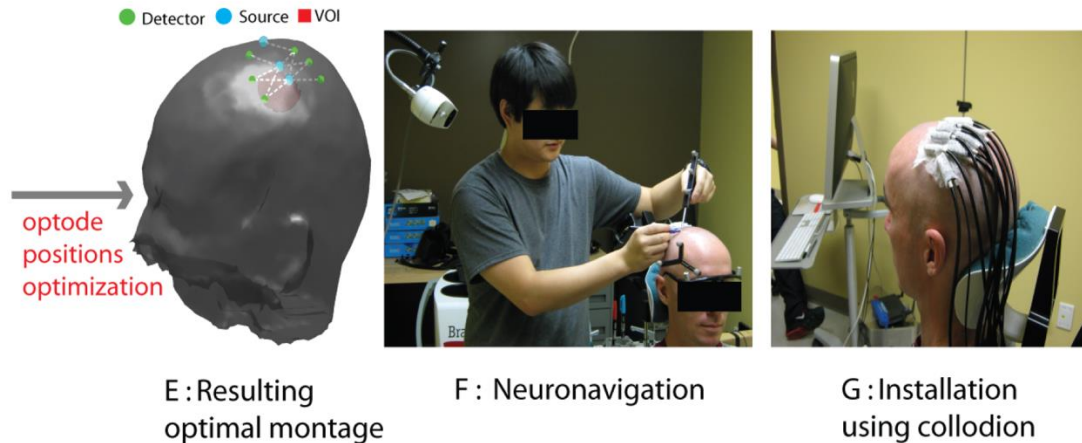
Alexis
Machado

Definition of a target Volume of Interest to be explored using fNIRS

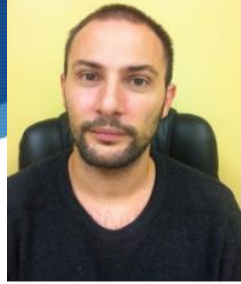


Maximizing a priori light sensitivity to the target and spatial overlap between channels

Mixed integer linear programming problem (CPLEX, IBM)

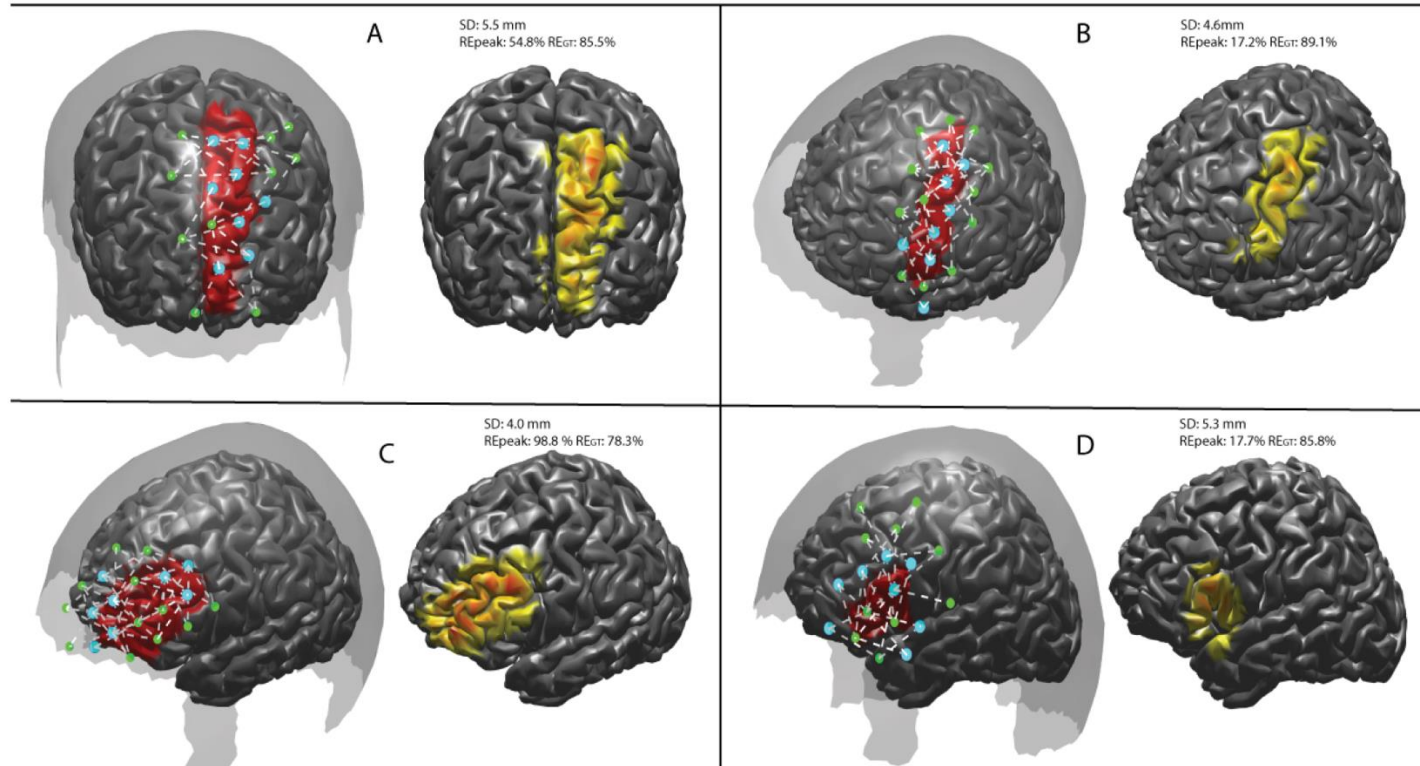


Personalized NIRS using “Optimal NIRS montages”



Alexis
Machado

HD-OM



Personalized fNIRS using optimal montage: dataset considered for NIRSTORM webinar

Personalized fNIRS channel layout design using anatomical head MRI

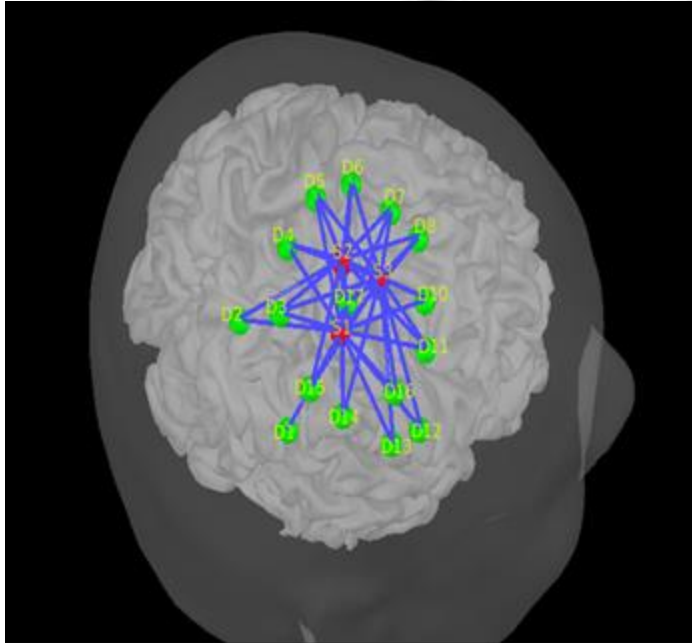
- Optical head model using a Monte Carlo photon simulator (Fang and Boas, 2009)
- Personalized optimal montage targeting the right hand knob (Machado et al., 2018)



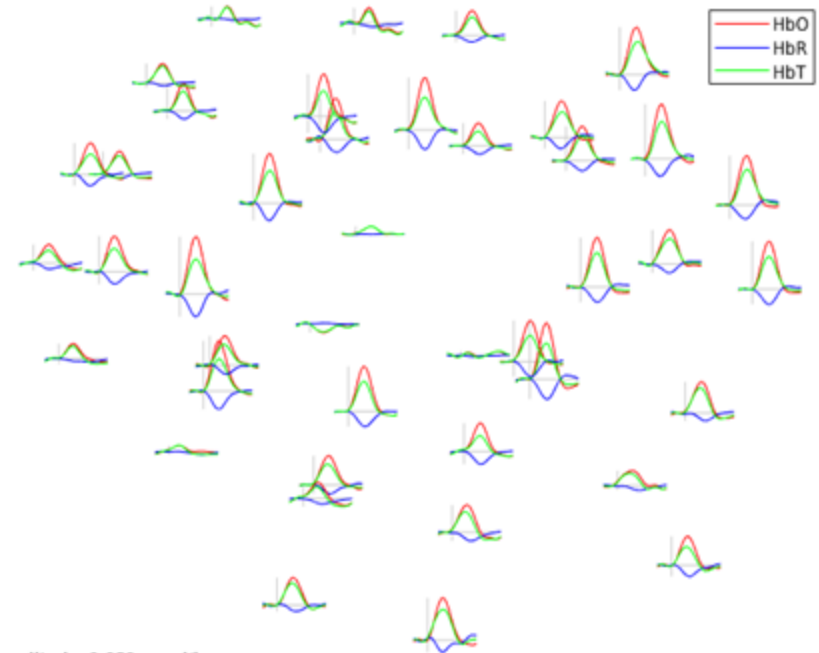
What is optimal montage?

- Maximization of spatial sensitivity of fNIRS measurements targeting a specific brain region, and maximizing spatial overlap between sensors
 - Hand knob 16.7 cm² (black profile)
- Pre-set # of sources, detectors and the density of channels
 - 3 Sources, 15 Detectors, at least 13 Detectors seeing each source , source-detector separation 1.5~4cm
- Use of collodion to glue optodes on the scalp, ensuring good optical contact for prolonged investigations (Yücel et al., Neuroimage, 2014; Pellegrino et al., Frontiers Neurosc, 2016)
- Finger opposition task at 2Hz, 20 Blocks of 10s with an inter-stimulus period ranging from 30 to 60s, Brainsight fNIRS device (Rogue-Research Inc, Montreal)

Standard NIRS data analysis on data measured using the optimal montage



Optimal Montage targeting
the right hand knob region
+ 1 additional detector
between the three sources
To obtain three short distance
channels

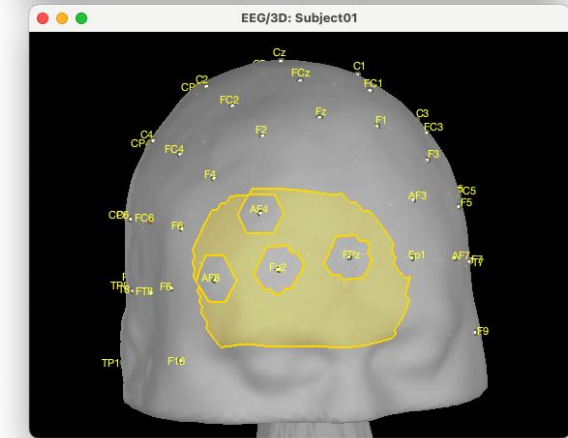
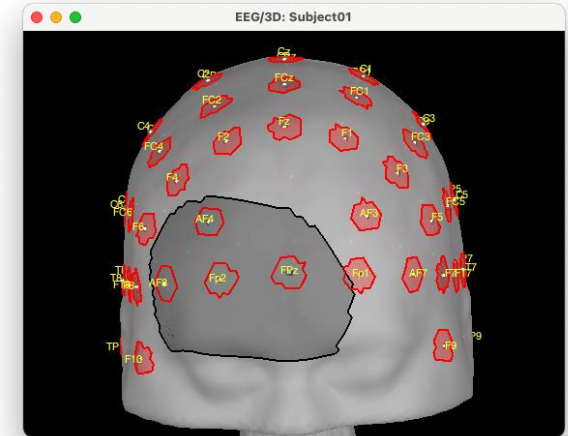
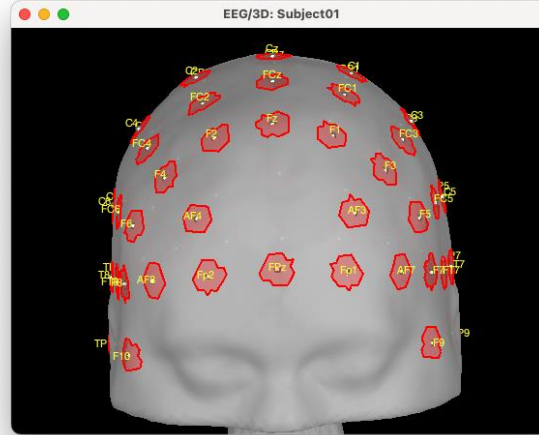
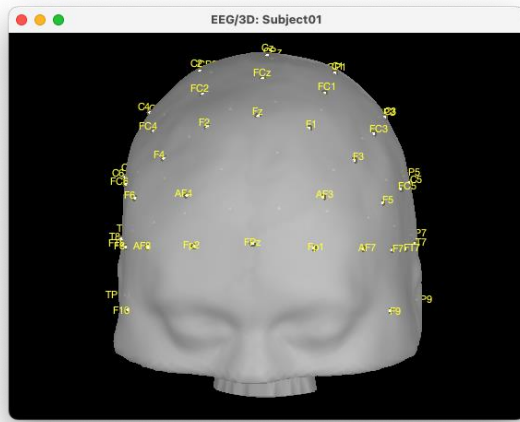


Max amplitude: 0.039 mmol/l
Time window: [-10000, 35000] ms



Average response
Band pass filter 0.005 – 0.08Hz
+ Short distance channel regression

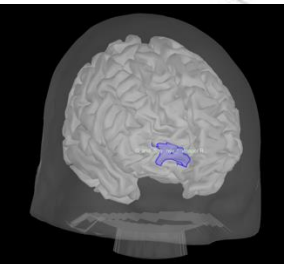
Optimal fNIRS montage, taking into account EEG position constraints



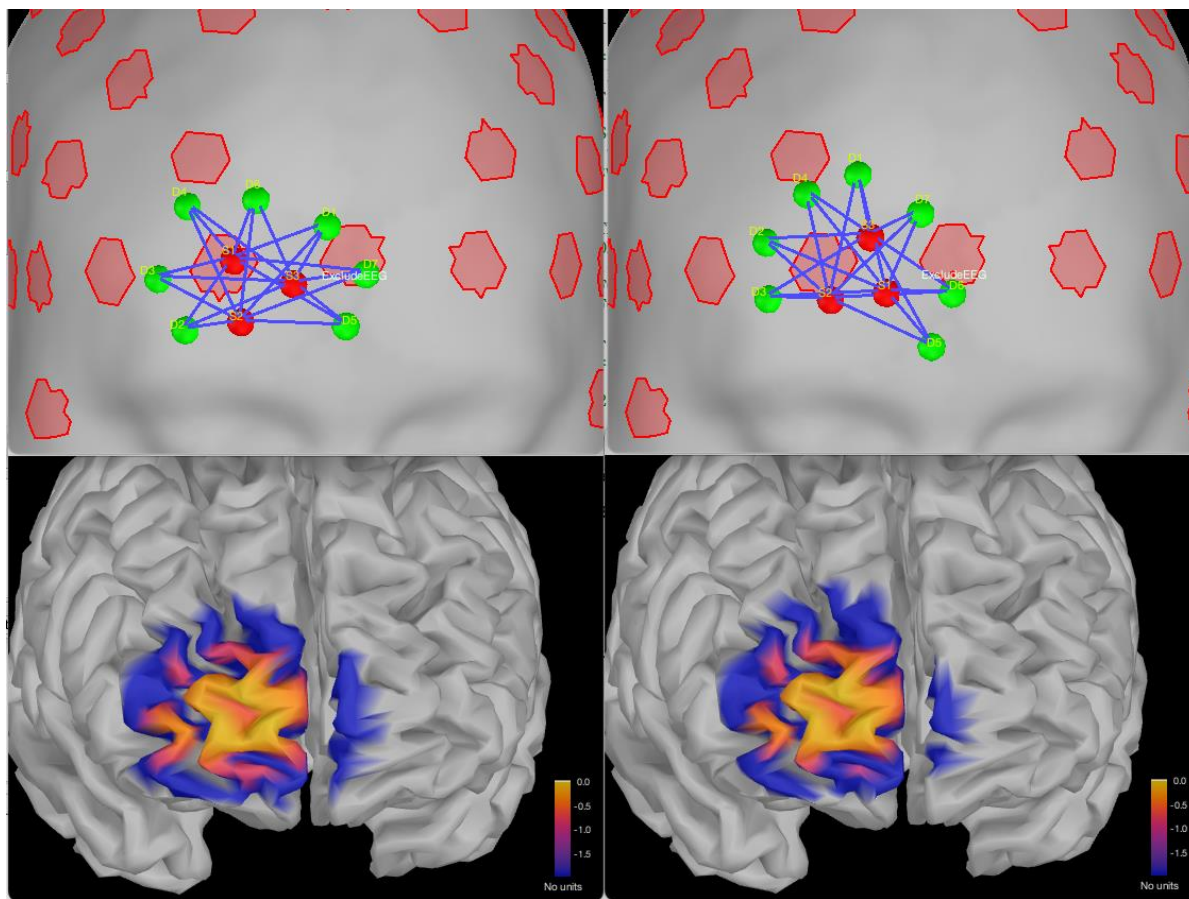
Avoiding the positions of an EEG cap

Updating the search space

Optimal fNIRS montage, taking into account EEG position constraints

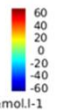
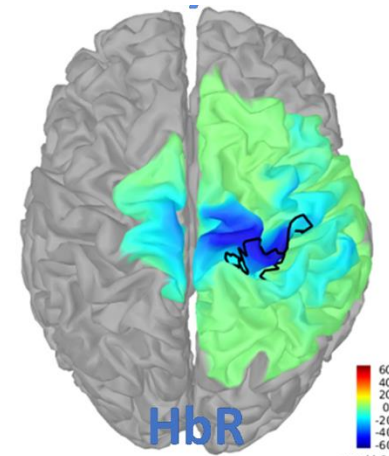
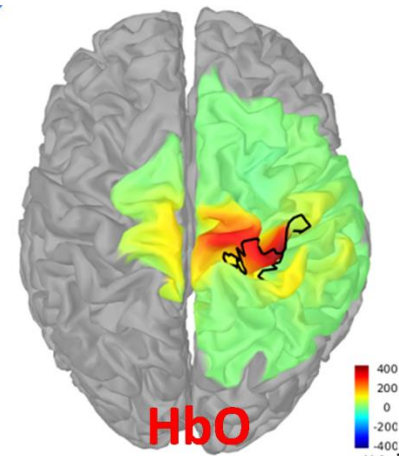
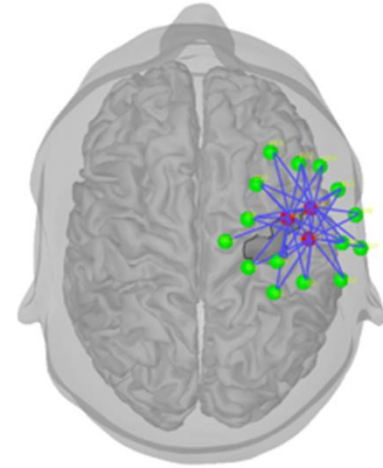


Targeted right
Fronto polar region



fNIRS 3D Reconstructions

Diffuse Optical Tomography (DOT)

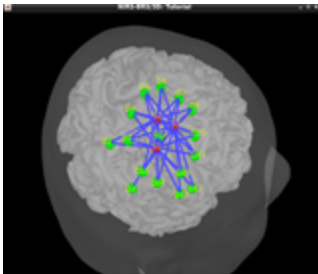
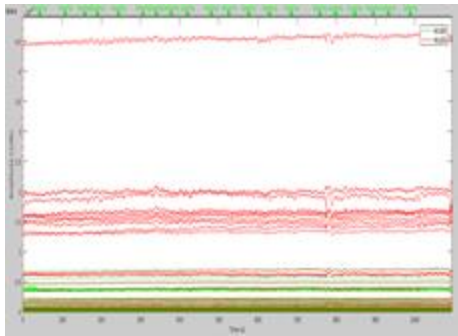


fNIRS 3D reconstruction

Solving an ill-posed inverse problem

$$Y = AX + e \leftarrow \text{Noise}$$

Optical Density data at specific wavelengths
(685, 830 nm)

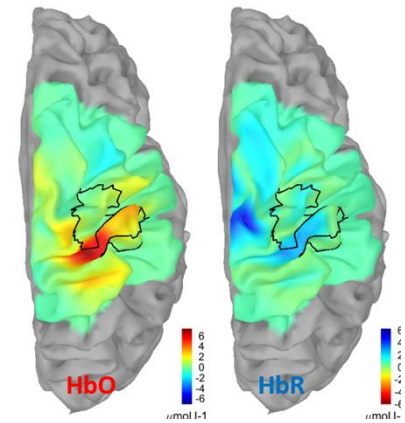
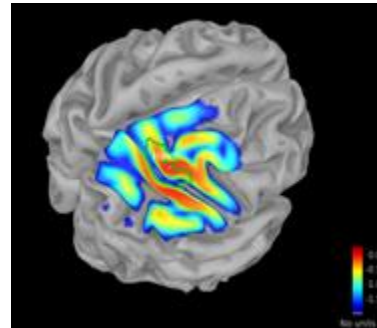


fNIRS forward model
Light sensitivity maps
estimated using Monte Carlo
simulations
MCXLab
(Fang and Boas 2009)

fNIRS 3D reconstruction
along the cortical surface

1. Minimum Norm Estimate (MNE)
2. Maximum Entropy on the Mean (MEM)

a



fNIRS 3D reconstruction

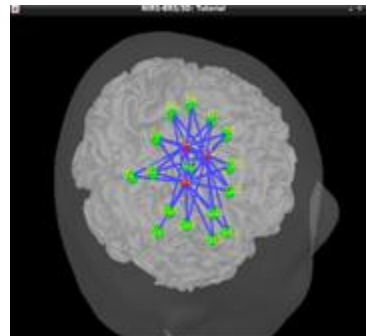
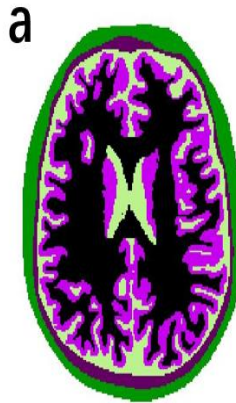
Solving the forward Problem A

$$Y = AX + e$$

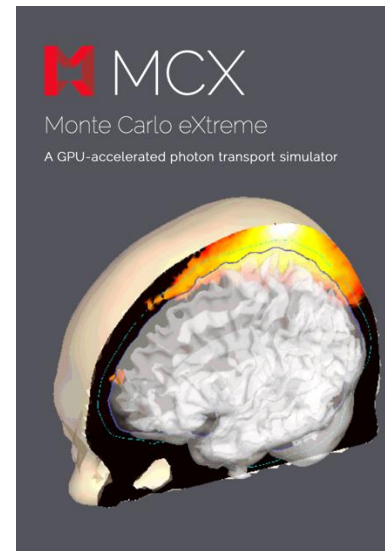


fNIRS forward model
Light sensitivity maps
estimated using Monte
Carlo simulations
MCXLab
(Fang and Boas 2009)

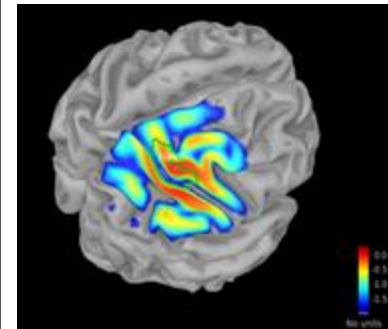
Subject Specific
(or template base)
Head Modeling in 5
tissues
(Freesurfer, SPM)



Integration of MCXLab, Monte
Carlo Simulation of light
transport on GPU
(Fang and Boas 2009)
<http://mcx.space>



Light sensitivity map
on the cortical
surface,



fNIRS 3D reconstruction

Solving the DOT inverse problem



Zhengchen Cai

$$Y = AX + e$$

Minimum Norm Estimate (MNE)

Hamalainen and Ilmoniemi 1994, Zeff et al 2007, Dehghani et al 2009, Eggebrecht et al 2014

$$\hat{X}_{MNE} = \operatorname{argmin} (\|(Y - AX)\|_{\Sigma_d}^2 + \lambda \|X\|_{\Sigma_s}^2)$$

$$= (A^T \Sigma_d A + \lambda \Sigma_s)^{-1} A^T \Sigma_d Y$$

Noise covariance

Hyperparameter of regularization
(L-curve)

Prior on source covariance (Identity)

Depth Weighted MNE

Lin et al 2006, Cai et al Submitted

$$\hat{X}_{dMNE} = \operatorname{argmin} (\|(Y - AX)\|_{\Sigma_d}^2 + \lambda \|X\|_{\Sigma_s}^2)$$

$$= (A^T \Sigma_d A + \lambda (\Lambda \Lambda^t)^{-1})^{-1} A^T \Sigma_d Y$$

$$\operatorname{diag}(\Lambda) = \frac{1}{\operatorname{diag}((A^T \Sigma_d A)^\omega)} \leftarrow \text{Depth weighting parameter}$$

Maximum Entropy on the Mean (MEM)

Amblard et al 2004, Grova et al 2006, Chowdhury et al 2013, Cai et al Sci Rep 2021

Non linear probabilistic approach

Relative entropy with a prior distribution

$$S_v(dp(x)) = - \int_x \log \left(\frac{dp(x)}{d\nu(x)} \right) dp(x)$$

Data Fit term

$$Y - [A|I_q] \begin{bmatrix} E_{dp}[x] \\ e \end{bmatrix} = 0, \quad dp \in C_m$$

Regularization using entropy

$$dp^*(x) = \operatorname{argmax}_{dp(x) \in C_m} (S_v(dp(x)))$$

Flexible framework to define the prior distribution (reference)

Recent implementation of depth weighting within MEM

fNIRS 3D reconstruction using the MEM framework originally developed for EEG/MEG source imaging versus MNE

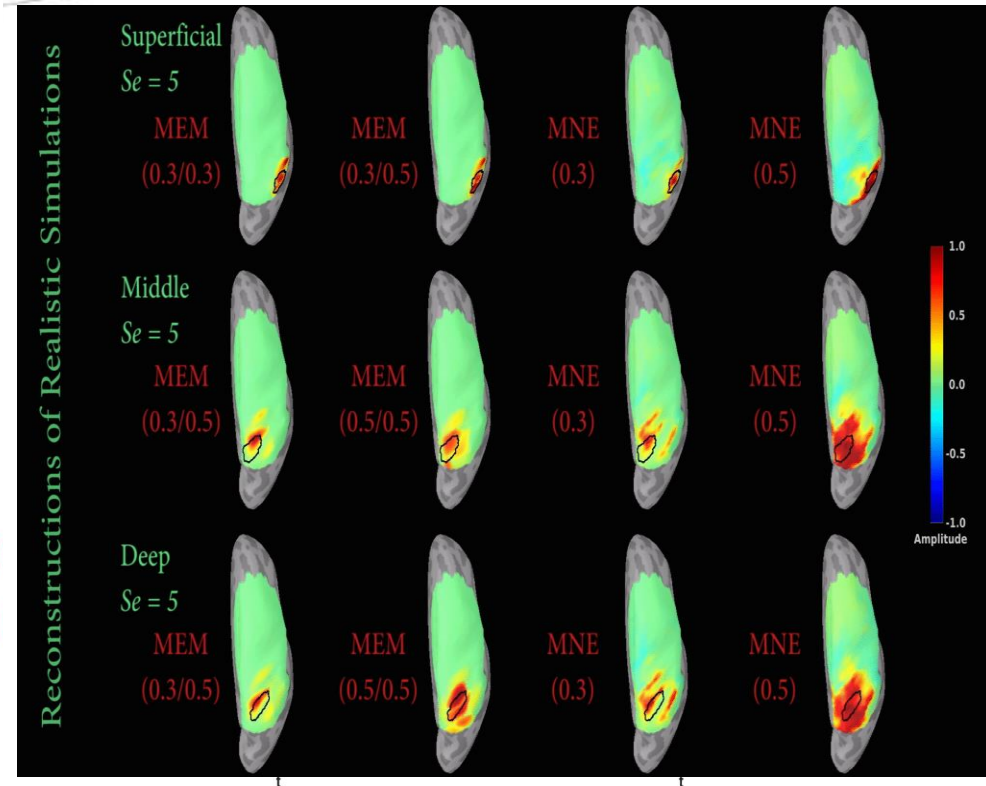
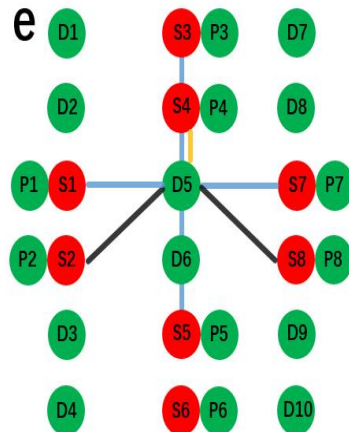
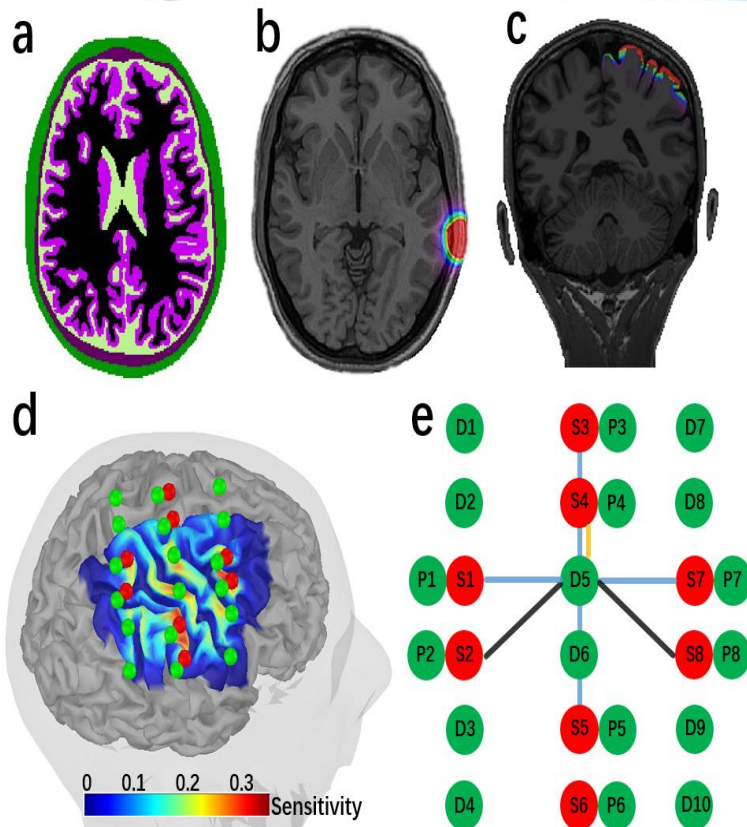


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1. Evaluation using realistic simulations

fNIRS probe and forward model
(Monte Carlo simulations)

fNIRS realistic simulations
at different SNR



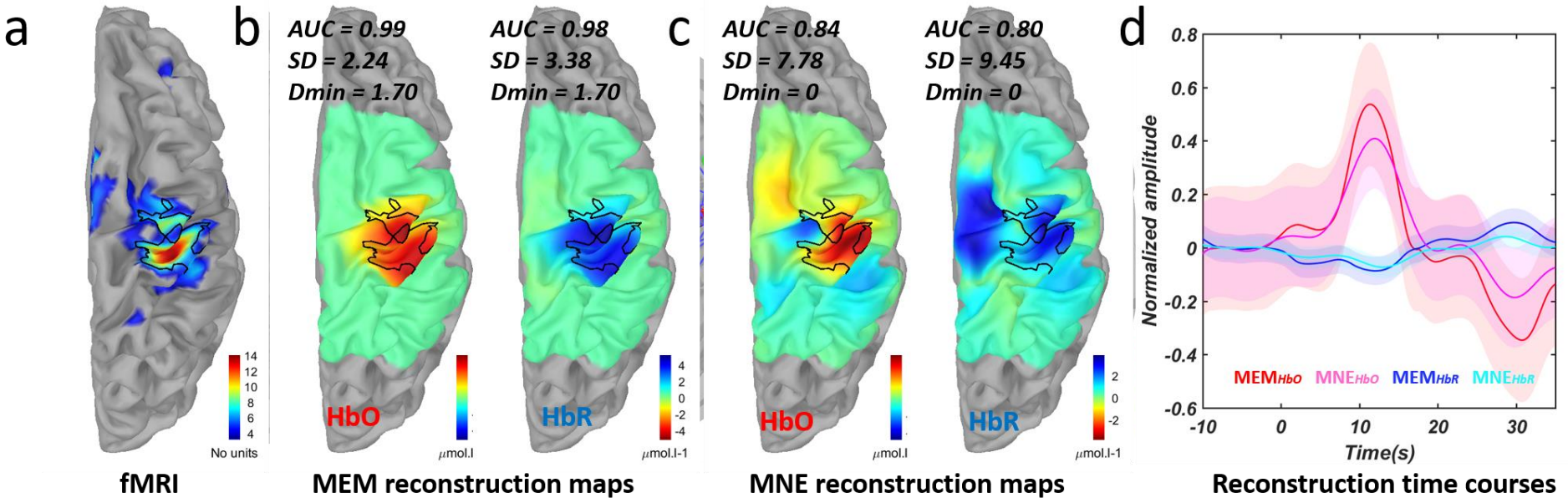
fNIRS 3D reconstruction using the MEM framework originally developed for EEG/MEG source imaging versus MNE

2. Comparison with finger tapping fMRI in 10 healthy controls

Personalized fNIRS: optimal montage targeting the right hand knob



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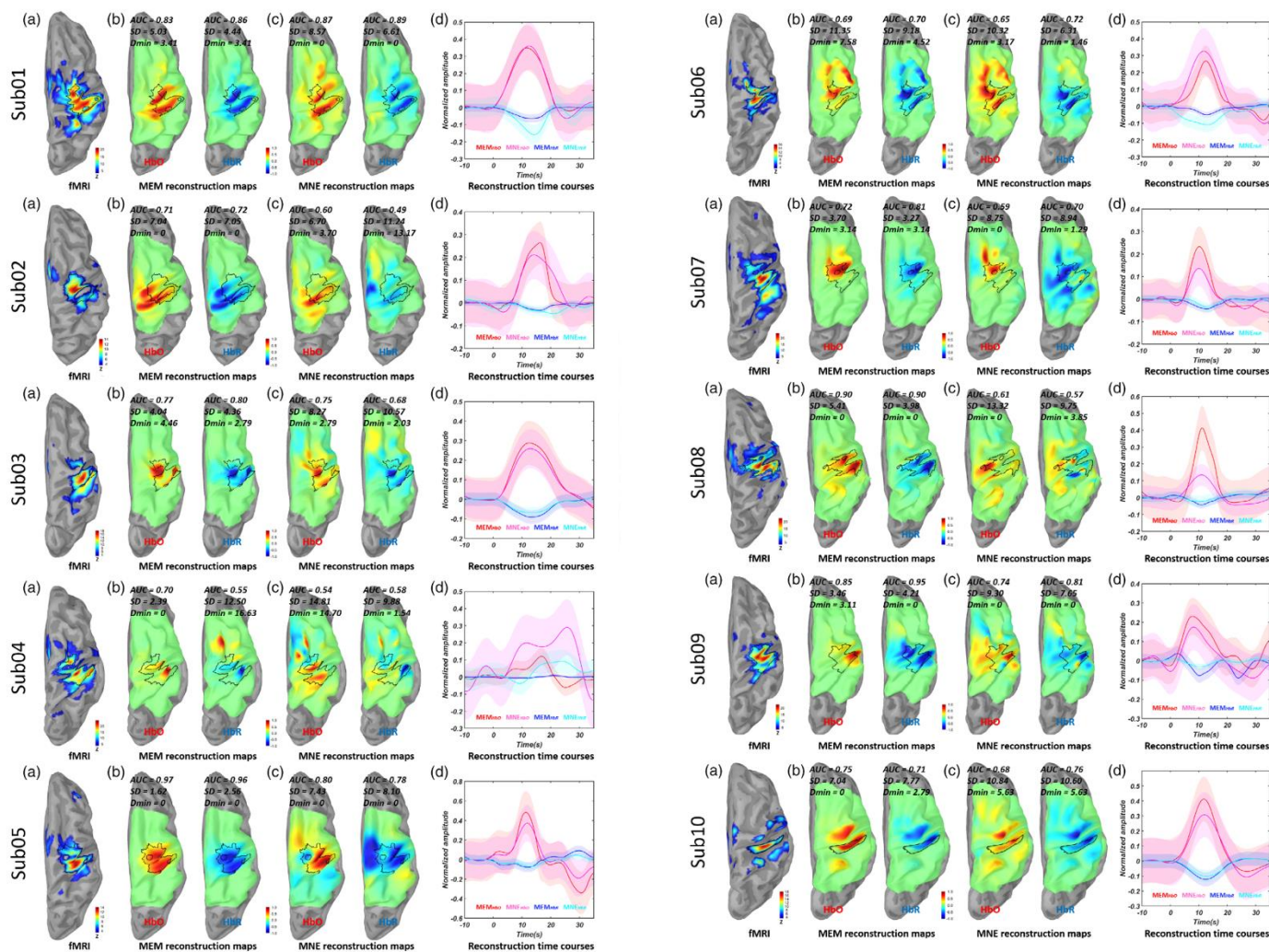
Evaluation of a personalized functional near infra-red optical tomography workflow using maximum entropy on the mean

Zhengchen Cai , Makoto Uji, Ümit Aydın, Giovanni Pellegrino, Amanda Spilkin, Édouard Delaire, Chifaou Abdallah, Jean-Marc Lina, Christophe Grova

First published: 03 August 2021 | <https://doi.org/10.1002/hbm.25566> | Citations: 4



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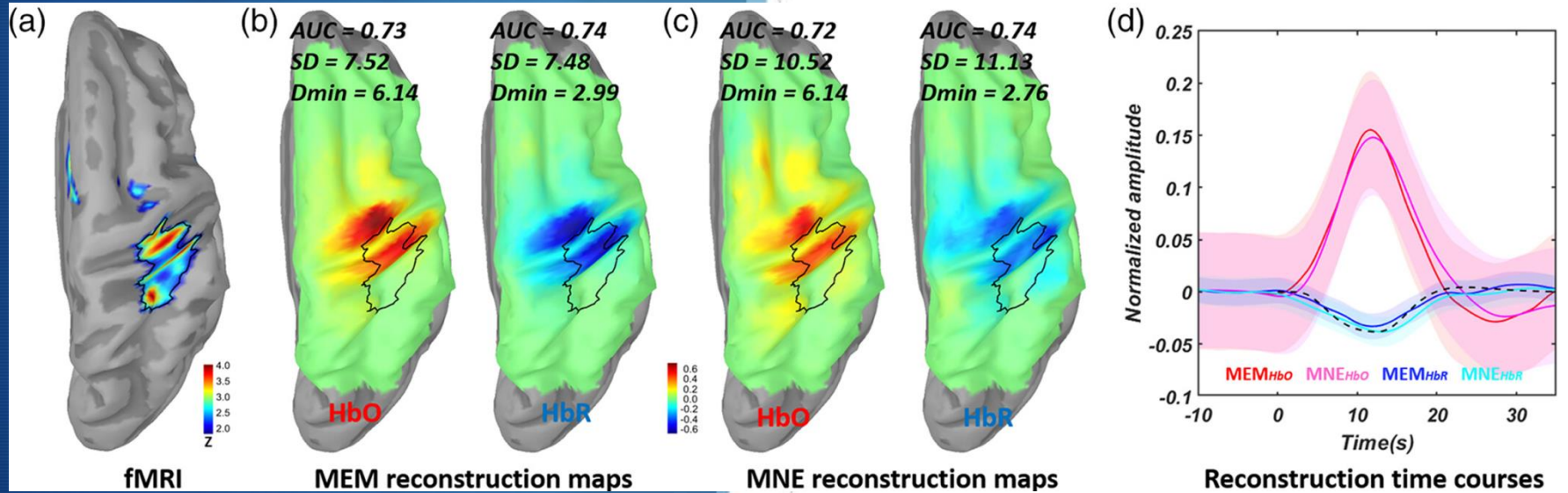
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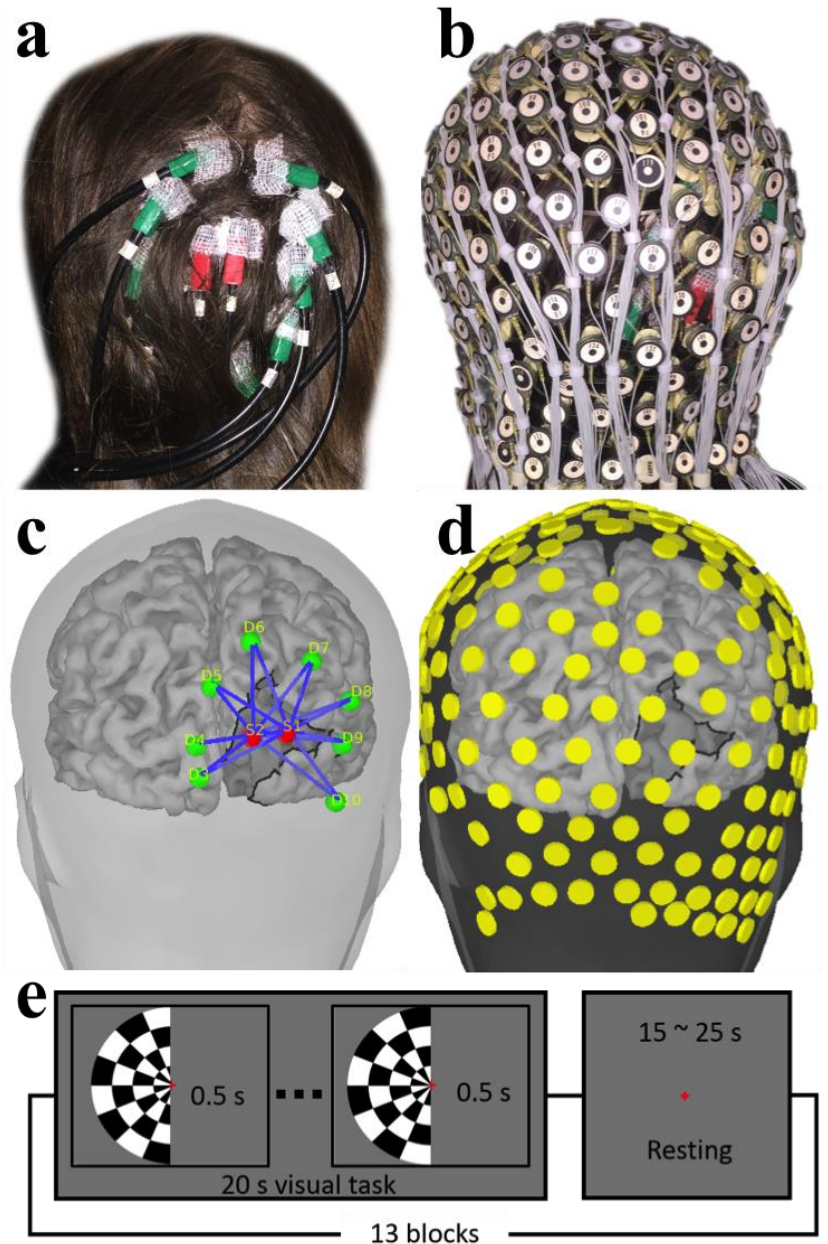
First published: 03 August 2021 | <https://doi.org/10.1002/hbm.25566> | Citations: 4



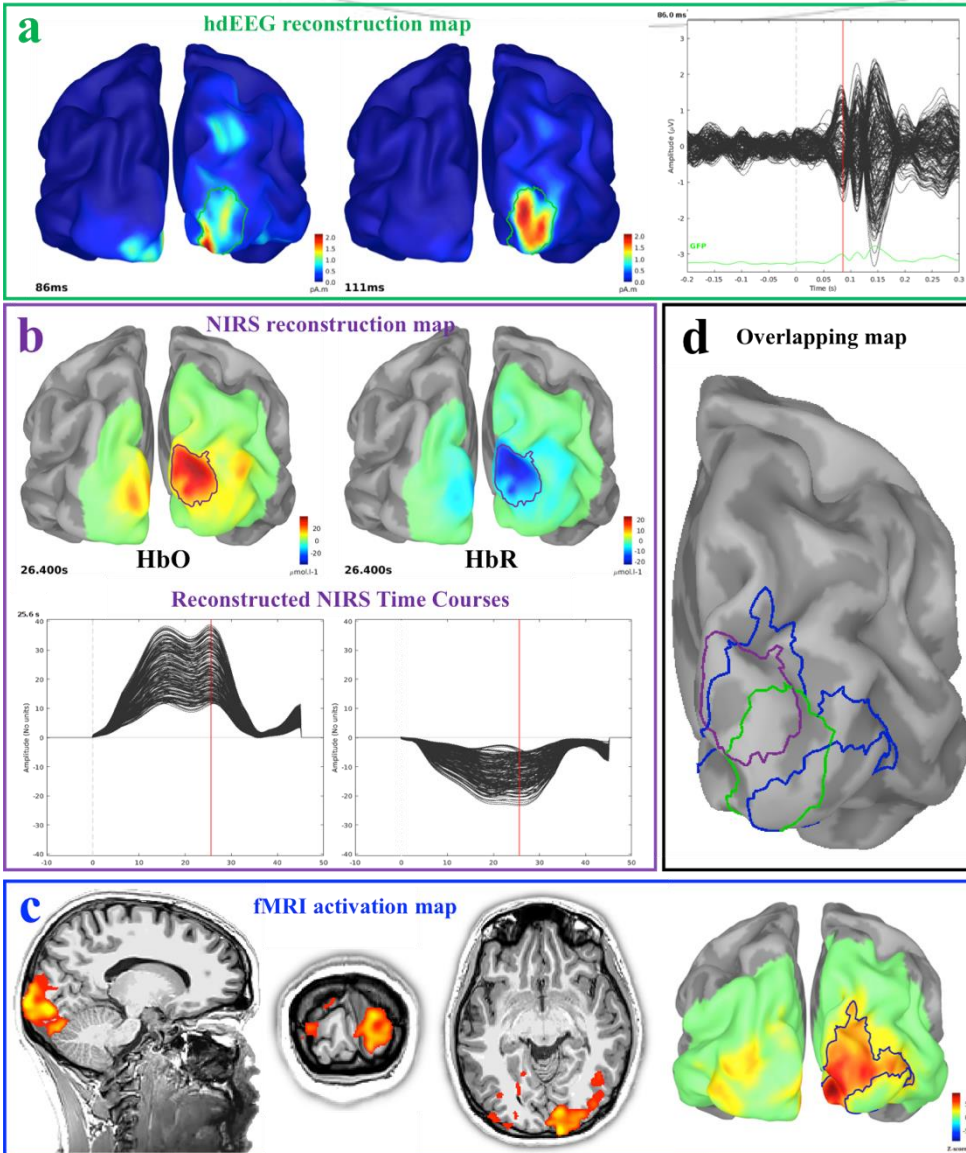
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An example of complete multimodal investigation using: fMRI, high density EEG and NIRS



Full multimodal investigation (hdEEG, fMRI, NIRS) during a visual stimulation task



EEG and NIRS 3D Reconstruction using Maximum Entropy on the Mean (MEM)
Amblard et al IEEE TBME 2004
Pellegrino et al HBM 2018, 2020
Abdallah et al Neurology 2022
Afnan et al HBM 2024

NIRSTORM



MEM in fNIRS:
Cai et al, HBM 2021
Cai et al Sci. Report 2021
Cai et al HBM 2023
Delaire et al Bioarxiv 2024



Brainstorm BEst Tutorial
<http://neuroimage.usf.edu/brainstorm/Tutorials/TutBEst>



NIRSTORM
<https://github.com/Nirstorm/nirstorm>

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Multimodal functional Imaging Lab (Concordia and McGill)



Multimodal Functional Imaging Laboratory



Centre PERFORM Centre



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Eliane Kobayashi



Jean-Marc Lina

